



UNIVERSITY OF  
GLOUCESTERSHIRE

This is a peer-reviewed, final published version of the following document, This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit <http://creativecommons.org/licenses/by/4.0/>. and is licensed under Creative Commons: Attribution 4.0 license:

**Mayfield, Dean L., Cronin, Neil ORCID: 0000-0002-5332-1188 and Lichtwark, Glen A. (2023) Understanding altered contractile properties in advanced age: insights from a systematic muscle modelling approach. *Biomechanics and Modeling in Mechanobiology*, 22. pp. 309-337. doi:10.1007/s10237-022-01651-9**

Official URL: <http://doi.org/10.1007/s10237-022-01651-9>

DOI: <http://dx.doi.org/10.1007/s10237-022-01651-9>

EPrint URI: <https://eprints.glos.ac.uk/id/eprint/11873>

#### **Disclaimer**

The University of Gloucestershire has obtained warranties from all depositors as to their title in the material deposited and as to their right to deposit such material.

The University of Gloucestershire makes no representation or warranties of commercial utility, title, or fitness for a particular purpose or any other warranty, express or implied in respect of any material deposited.

The University of Gloucestershire makes no representation that the use of the materials will not infringe any patent, copyright, trademark or other property or proprietary rights.

The University of Gloucestershire accepts no liability for any infringement of intellectual property rights in any material deposited but will remove such material from public view pending investigation in the event of an allegation of any such infringement.

PLEASE SCROLL DOWN FOR TEXT.



# Understanding altered contractile properties in advanced age: insights from a systematic muscle modelling approach

Dean L. Mayfield<sup>1</sup> · Neil J. Cronin<sup>2,3</sup> · Glen A. Lichtwark<sup>4</sup>

Received: 8 April 2022 / Accepted: 14 October 2022  
© The Author(s) 2022

## Abstract

Age-related alterations of skeletal muscle are numerous and present inconsistently, and the effect of their interaction on contractile performance can be nonintuitive. Hill-type muscle models predict muscle force according to well-characterised contractile phenomena. Coupled with simple, yet reasonably realistic activation dynamics, such models consist of parameters that are meaningfully linked to fundamental aspects of muscle excitation and contraction. We aimed to illustrate the utility of a muscle model for elucidating relevant mechanisms and predicting changes in output by simulating the individual and combined effects on isometric force of several known ageing-related adaptations. Simulating literature-informed reductions in free  $\text{Ca}^{2+}$  concentration and  $\text{Ca}^{2+}$  sensitivity generated predictions at odds qualitatively with the characteristic slowing of contraction speed. Conversely, incorporating slower  $\text{Ca}^{2+}$  removal or a fractional increase in type I fibre area emulated expected changes; the former was required to simulate slowing of the twitch measured experimentally. Slower  $\text{Ca}^{2+}$  removal more than compensated for force loss arising from a large reduction in  $\text{Ca}^{2+}$  sensitivity or moderate reduction in  $\text{Ca}^{2+}$  release, producing realistic age-related shifts in the force-frequency relationship. Consistent with empirical data, reductions in free  $\text{Ca}^{2+}$  concentration and  $\text{Ca}^{2+}$  sensitivity reduced maximum tetanic force only slightly, even when acting in concert, suggesting a modest contribution to lower specific force. Lower tendon stiffness and slower intrinsic shortening speed slowed and prolonged force development in a compliance-dependent manner without affecting force decay. This work demonstrates the advantages of muscle modelling for exploring sources of variation and identifying mechanisms underpinning the altered contractile properties of aged muscle.

**Keywords** Ageing · Twitch · Force-frequency relationship · Calcium sensitivity · Specific force · Calcium uptake and release

## 1 Introduction

Evidence has mounted in favour of the view that the intrinsic contractile properties of skeletal muscle are altered in advanced age. Age-related deficits in single fibre specific tension and maximum velocity of shortening have been

found for type I and type II fibres from aged muscles of both rodents (Degens et al. 1998; Thompson et al. 1998; González et al. 2000, 2003; Zhong et al. 2006; Kim and Thompson 2013) and humans (Larsson et al. 1997; Frontera et al. 2000; Krivickas et al. 2001; D'Antona et al. 2003; Ochoala et al. 2007; Yu et al. 2007; Lambole et al. 2015; Power et al. 2016; Brocca et al. 2017) and can manifest despite long-term training (Korhonen et al. 2006; Power et al. 2016). Such findings imply that the broad decline in contractile performance with ageing isn't the sole product of reductions in muscle fibre number and size. Reinforcing this notion are a more limited number of studies demonstrating that fundamental processes involved in activation and contraction are prone to impairment in old muscle, including the kinetics of cross-bridge cycling (Höök et al. 2001; D'Antona et al. 2003; Miller et al. 2013), mechanics of myosin (Lowe et al. 2001) and  $\text{Ca}^{2+}$  sensitivity of force (Brooks and Faulkner

✉ Dean L. Mayfield  
deanm@ucr.edu

<sup>1</sup> Department of Evolution, Ecology, and Organismal Biology, University of California, Riverside, Riverside, USA

<sup>2</sup> Neuromuscular Research Centre, Faculty of Sport and Health Sciences, University of Jyväskylä, Jyväskylä, Finland

<sup>3</sup> School of Sport and Exercise, University of Gloucestershire, Cheltenham, UK

<sup>4</sup> School of Human Movement and Nutrition Sciences, University of Queensland, Brisbane, Australia

1994; Lowe et al. 2002; Lamboley et al. 2015; Straight et al. 2018; Mazara et al. 2021), and handling of  $\text{Ca}^{2+}$  by the sarcoplasmic reticulum [SR (Larsson and Salvati 1989; Delbono et al. 1995; Narayanan et al. 1996; Wang et al. 2000; Jiménez-Moreno et al. 2008; Andersson et al. 2011; Uman-skaya et al. 2014)].

Impaired intrinsic contractile performance, however, is not universally observed for old muscle (Trappe et al. 2003; Hvid et al. 2011; Sundberg et al. 2018; Teigen et al. 2020; Mazara et al. 2021). The same is true of disturbances to cellular level contractile processes, such as  $\text{Ca}^{2+}$  sensitivity of force (Eddinger et al. 1986; Plant and Lynch 2001; Lamboley et al. 2015; Teigen et al. 2020) and SR  $\text{Ca}^{2+}$  uptake (Fitts et al. 1984; Narayanan et al. 1996; Thomas et al. 2010). When human single fibre data published within the last decade are considered (Claffin et al. 2011; Hvid et al. 2011, 2017; Miller et al. 2013; Sundberg et al. 2018; Straight et al. 2018; Gries et al. 2019; Teigen et al. 2020; Grosicki et al. 2021; Mazara et al. 2021), a compelling argument could be made that neither type I nor type II fibres show an appreciable decline in specific force or shortening speed. Yet, age-related deficits in joint-level contraction speed and mass-specific mechanical power arise in the absence of impaired single fibre function (Reid et al. 2012; Sundberg et al. 2018). Prolonged or slowed force rise and decay and elevated force generation at submaximal stimulation frequencies (i.e. leftward-shifted force-frequency relationship) are also among the most commonly observed features of whole muscle in advanced age (Fitts et al. 1984; Davies et al. 1986; Larsson and Edström 1986; Vandervoort and McComas 1986; Brooks and Faulkner 1988; Alway 1995; Roos et al. 1999; Dow et al. 2005; McNeil et al. 2007; Tevald et al. 2009). A plausible explanation may be that an age-related elevation of the fractional area occupied by type I fibres or of the myosin heavy chain (MHC) I fibre content (Larsson et al. 1978; Coggan et al. 1992; Hunter et al. 1999; Short et al. 2005; Cui et al. 2008; Nilwik et al. 2013; Sonjak et al. 2019) is sufficient to produce a slower contractile phenotype (Ranatunga and Thomas 1990; Harridge et al. 1996).

Predicting altered mechanical output and identifying the underlying determinants remains challenging because contractile properties present inconsistently in advanced age, which may be reconciled with the myriad alterations that aged muscle can exhibit. Reports of the effect of age on single fibre or whole muscle contractile performance can be conflicting or show variation across taxa (Ballak et al. 2014), rodent strains (Rice et al. 2005), muscles (Brooks and Faulkner 1988; Brown and Hasser 1996; Narayanan et al. 1996; Hill et al. 2020), and as a function of activity level or training status (Fitts et al. 1984; Klitgaard et al. 1989; D'Antona et al. 2007), sex (Degens et al. 1998; Krivickas et al. 2001; Hill et al. 2020) and fibre type (Yu et al. 2007; Kim and Thompson 2013; Lamboley et al. 2015). Even for

a given muscle of a model organism, the effect of ageing on contractile behaviour can vary (Brooks and Faulkner 1988; Moran et al. 2005). In addition to the aforementioned adaptations of cellular level function (e.g. slower cross-bridge kinetics), and a relative increase in type I fibre content, aged muscle may exhibit structural adaptations, such as altered intramuscular and extramuscular connective tissue properties (Gao et al. 2008; Wood et al. 2011; Stenroth et al. 2012; Danos et al. 2016; Holt et al. 2016). Compared to a loss of muscle mass, it is less clear how these adaptations (and others) impact contractile performance, especially when acting in concert, and to what extent these adaptations must present to be meaningful.

Determining the impact of age-related changes in muscle structure and function on mechanical output isn't always feasible. For example, experimental approaches to quantifying excitation-SR  $\text{Ca}^{2+}$  release coupling and SR  $\text{Ca}^{2+}$  uptake dynamics may preclude myosin-actin interaction or be performed without simultaneous measurement of contractile force (Larsson and Salvati 1989; Delbono et al. 1995; Narayanan et al. 1996; Wang et al. 2000). In this context, it is also worth noting that crude homogenates of muscle frequently used to study  $\text{Ca}^{2+}$  release and  $\text{Ca}^{2+}$  uptake in advanced age (Fitts et al. 1984; Hunter et al. 1999; Thomas et al. 2010; Russ et al. 2011) may also be sensitive to an age-related increase in type I fibre content. The multifaceted and diverse nature of muscle deterioration and remodelling in response to ageing places importance on the interaction of adaptations. Interaction effects may be nonintuitive and may not always result in obvious impairment. Whereas an age-related reduction in the  $\text{Ca}^{2+}$  sensitivity of force may compound a reduction in SR  $\text{Ca}^{2+}$  release, an age-related slowing of SR  $\text{Ca}^{2+}$  uptake may offer a buffering effect. Linking any single adaptation to impaired contractile performance may be difficult when the scope of the study from an explanatory point of view is narrow and the broader extent of senescence is uncertain.

Establishing the likelihood that an altered property would appreciably impair contractile performance, in isolation and when acting in concert, might aid our understanding of altered contractile performance in advanced age from mechanistic and predictive perspectives. Muscle models are useful tools for exploring the effects of muscle design and adaptation on contractile performance (Wisdom et al. 2015). Several common traits of aged muscle contractile performance have been accurately simulated by adjusting model parameters to reflect known changes in activation and contraction dynamics and muscle-tendon morphology (Thelen 2003; Hasson and Caldwell 2012). Hill-type models simulate contractile behaviour according to well-established intrinsic mechanical phenomena (Curtin et al. 1998; Williams et al. 1998; Wakeling and Johnston 1999) and can be integrated with relatively simple, yet

physiologically-grounded activation dynamics (Lichtwark and Wilson 2005a). Because many of the parameters used in Hill-type models can be related to muscle–tendon structure and intrinsic muscle properties, such models have the potential to elucidate the predominant mechanisms of altered force output and help explain unexpected observations and variance reported in the literature.

In this study, we implement a three-element Hill-type muscle model to examine how known changes in muscle function and structure in advanced age affect the contractile properties of muscle during fixed-end contractions. Drawing upon published literature, we simulate the individual and combined effects of impaired  $\text{Ca}^{2+}$  release, slower  $\text{Ca}^{2+}$  uptake, lower  $\text{Ca}^{2+}$  sensitivity of force, slowed intrinsic shortening speed, altered series elastic compliance, and a greater fractional content of type I fibres. Specifically, we evaluate the effects of these adaptations on isometric force during a twitch, brief tetanic contraction, and sustained contractions at submaximal and maximal stimulation frequencies. We then discuss the use of the model to explain how these known adaptations might affect muscle force, consider the adaptations most consistent with the contractile properties of aged muscle observed experimentally and reported by others in the literature, and identify certain conditions that may result in non-intuitive outcomes.

## 2 Methods

### 2.1 Experimental twitch data

Plantar flexion twitch torque was measured in 10 young (mean  $\pm$  SD; age:  $28 \pm 3$  years; body mass:  $78 \pm 11$  kg; height:  $179 \pm 6$  cm) and 18 older (age:  $72 \pm 5$  years; body mass:  $76 \pm 10$  kg; height:  $174 \pm 5$  cm) healthy human adult males. An analysis of the experimental data obtained from young adults and a detailed description of the experimental protocol used for both young and older adults have been published previously (Mayfield et al. 2015). In brief, participants sat with their knee extended and right foot securely fixed to a non-compliant rotational footplate. The ankle was set to a neutral position (foot  $90^\circ$  relative to tibia). Two custom-built strain gauges positioned directly under the footplate measured isometric plantar flexion force evoked by percutaneous electrical stimulation of the tibial nerve. Single supramaximal square-wave pulses were delivered to elicit unpotentiated twitches, which were evaluated for peak torque, contraction time and half-relaxation time. Unpaired Student's *t*-tests or Welch's *t*-tests (unequal variance) were performed to test the effect of age. Statistical significance

was set at  $P < 0.05$  and effect sizes were calculated as eta squared ( $\eta^2$ ).

### 2.2 Hill-type muscle model

We implemented an adapted Hill-type muscle model previously shown to successfully predict the time course of muscle force during contractions involving either ramp shortening or lengthening, or sinusoidal length changes (Curtin et al. 1998; Lichtwark and Wilson 2005a). The model (Mayfield and Lichtwark 2022), developed in Simulink (MathWorks, Natick, MA), consists of a contractile element (CE) and parallel elastic element (PEE) arranged in-series with an elastic element (SEE). The active force output of the CE depends on the interaction of CE activation, length, and velocity dynamics.

#### 2.2.1 Activation

Activation of the CE is regulated by the concentration of an activator, which we consider to be calcium, in a single compartment. Calcium ions ( $\text{Ca}^{2+}$ ) are released transiently at a constant rate in response to each stimulus and subsequently removed at a rate dependent on the  $\text{Ca}^{2+}$  concentration (Fig. 1a).  $\text{Ca}^{2+}$  release occurs over a defined pulse width according to the following equation:

$$\frac{da}{dt} = \frac{(1-a)}{\tau_1}$$

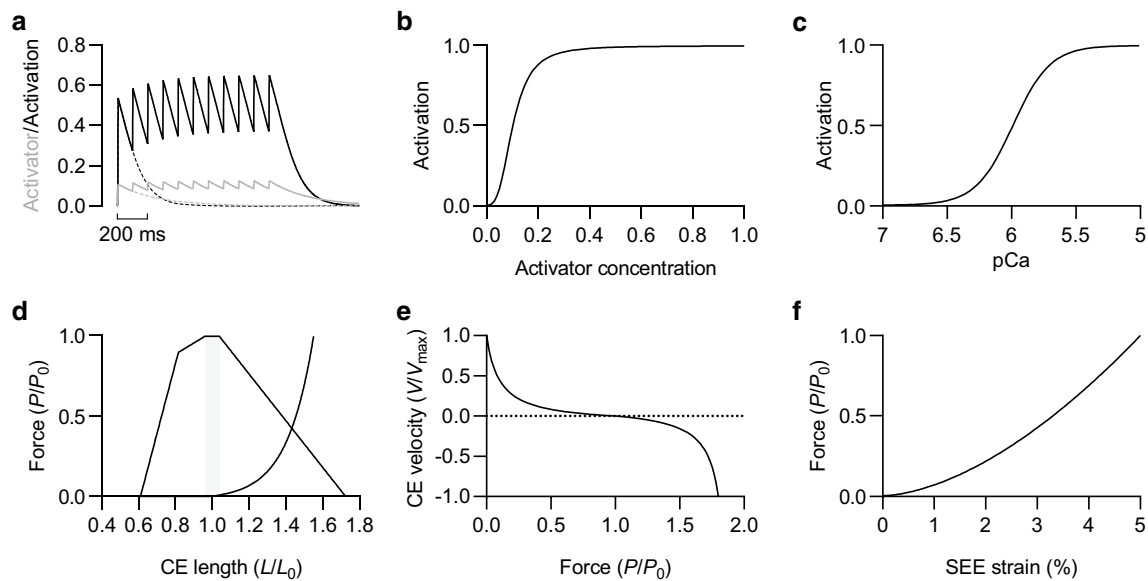
Otherwise,  $\text{Ca}^{2+}$  is removed according to the following equation:

$$= \frac{-a}{\tau_2}$$

where  $a$  is the concentration of activator ( $\text{Ca}^{2+}$ ) and  $\tau_1$  and  $\tau_2$  are the time constants for the rise and fall of  $\text{Ca}^{2+}$ , respectively (Lichtwark and Wilson 2005a).  $\text{Ca}^{2+}$  release for a second stimulus is attenuated relative to the first for brief interstimulus intervals (Caputo et al. 2004; Barclay 2012). Inactivation of  $\text{Ca}^{2+}$  release was incorporated into the model by reducing pulse width according to a single exponential equation describing the recovery of  $\text{Ca}^{2+}$  release with respect to interstimulus interval:

$$1 - Ae^{-isi/r}$$

where  $A$  is the minimum relative  $\text{Ca}^{2+}$  release (i.e. maximum inactivation),  $isi$  is the interstimulus interval and  $r$  is the time constant for the recovery of relative  $\text{Ca}^{2+}$  release (Barclay 2012).  $A$  and  $r$  were set at 20% and 350 ms, respectively, such that the force-frequency relationship was comparable to empirical observations for predominantly slow muscle [e.g.



**Fig. 1** Muscle model properties. **a** Activator concentration (lower trace) and activation level during a twitch (dashed) and 1 s stimulation train at 10 Hz. **b** Activation-activator relationship. **c** Activation-

pCa relationship. **d** CE and PEE force-length relationships. Shaded region represents range of optimal CE lengths. **e** CE force-velocity relationship. **f** SEE force-strain relationship

rat soleus (Ranatunga 1982; Larsson and Edström 1986)] or several muscles with varying fibre type compositions crossing the same joint (Marsh et al. 1981; Sale et al. 1982).

The relationship between  $\text{Ca}^{2+}$  and activation (Fig. 1b) is given by a sigmoidal function of the form:

$$Act = \frac{a^{n_H}}{(a^{n_H} + a_{50}^{n_H})}$$

where  $Act$  is thin filament activation and represents the fraction of cross-bridge binding sites available for cycling,  $n_H$  is the Hill coefficient, and  $a_{50}$  is the activator concentration required for half-maximal cross-bridge activation (Curtin et al. 1998).  $n_H$  and  $a_{50}$  (i.e.  $\text{pCa}_{50}$ ) are indices of cooperative activation and the  $\text{Ca}^{2+}$  sensitivity of force, respectively (Walker et al. 2010).

To relate the activation-activator relationship in the model to the force-pCa relationship of permeabilised single fibres (Hellam and Podolsky 1969; Stephenson and Williams 1982), we assumed that the activator concentration achieving saturation was equivalent to a calcium concentration of 10  $\mu\text{M}$  or pCa 5 (Fig. 1c); pCa is the negative log of the theoretical calcium concentration. A form of the Hill equation was then used to describe the relationship between calcium concentration and force:

$$\frac{P}{P_0} = \frac{1}{1 + 10^{n_H \cdot (\text{pCa} - \text{pCa}_{50})}}$$

where pCa is the negative log of the activator concentration, and  $\text{pCa}_{50}$  is the negative log equivalent of  $a_{50}$  (Martyn and Gordon 2001).

## 2.2.2 CE force-length & force-velocity relationships

Active force generated by the CE was modelled according to classic force-length (Gordon et al. 1966) and force-velocity (Hill 1938) relationships (Fig. 1d, e). The speed at which the CE shortens with respect to force, which is scaled by CE activation and length, was modelled according to a normalised form of the Hill equation:

$$\frac{P}{P_0} = \frac{K(1 - V/V_{\max})}{K + V/V_{\max}}$$

where  $P$  is force,  $P_0$  is the maximum isometric force,  $K$  represents  $a/P_0$  and indicates the curvature of the rectangular hyperbola describing the concentric force-velocity relationship,  $V$  is the velocity of CE shortening and  $V_{\max}$  is the maximum velocity of CE shortening (Seow 2013). The speed at which the CE lengthens with respect to an externally applied force (Fig. 1e) was modelled according to the following equation:

$$\frac{P}{P_0} = c - \frac{k(1 + V/V_{\max})}{1 - q(V/V_{\max})}$$

where  $c$  is a constant indicating the maximum eccentric force expressed relative to  $P_0$ ,  $k$  is a constant relating to the  $y$ -intercept, whereby  $c - k = 1$  to meet the condition of  $P/P_0 = 1$  for a lengthening velocity of 0, and  $q$  is a constant describing the curvature of the eccentric force–velocity relationship (Otten 1987; Azizi and Roberts 2014).  $c$ ,  $k$ , and  $q$  were assigned values of 1.8, 0.8 and 7, respectively.

### 2.2.3 PEE force–length relationship

The PEE was assigned an exponential passive force–length relationship (Fig. 1d) according to the following exponential equation:

$$\frac{P}{P_0} = \frac{e^{k_{\text{PEE}}(L_{\text{CE}} - L_{\text{slack}})/\varepsilon_{\text{PEE}}} - 1}{e^{k_{\text{PEE}}} - 1}$$

where  $k_{\text{PEE}}$  is an exponential shape factor,  $L_{\text{CE}}$  is the relative CE length,  $L_{\text{slack}}$  is the slack length of the PEE, and  $\varepsilon_{\text{PEE}}$  is the passive strain of the CE when an external load equal to  $P_0$  is applied (Thelen 2003). When  $L_{\text{slack}}$  is not equal to 1.0, the CE length at  $\varepsilon_{\text{PEE}}$  is equal to  $L_{\text{slack}}$  plus  $\varepsilon_{\text{PEE}} \cdot k_{\text{PEE}} \cdot L_{\text{slack}}$ .  $L_{\text{slack}}$  and  $\varepsilon_{\text{PEE}}$  were assigned values of 4, 0.98 and 0.57, respectively. These values are similar to those used previously for human plantar flexors (Thelen 2003) and generate a passive-force length relationship generally consistent with experimental data (Winters et al. 2011; Rubenson et al. 2012; Moo et al. 2020).

### 2.2.4 SEE force–length relationship

The SEE was assigned a non-linear load-deformation relationship consistent with experimental data for tendon and aponeurosis (Lieber et al. 1991; Trestik and Lieber 1993; Zuurbier et al. 1994; Loren and Lieber 1995; Cui et al. 2009). The general relationship was derived from a non-linear least squares fit of force and deformation data reported for mammalian tendon (Bennett et al. 1986) using the following equation:

$$P = ax^b$$

where  $a$  and  $b$  are regression constants and  $x$  is tendon deformation. SEE strain at  $P_0$  ( $\varepsilon_{\text{SEE}}$ , Fig. 1f) was set to 0.05 (Muramatsu et al. 2001; Arampatzis et al. 2005; Karamanidis and Arampatzis 2006). SEE stiffness was defined as the maximum deformation of the SEE normalised to  $P_0$  and the optimum length of the CE ( $L_0$ ), giving a normalised stiffness [ $k_{\text{SEE}}$  (Lichtwark and Wilson 2005b)]. SEE length ( $L_{\text{SEE}}$ ) and  $L_0$  were set at 300 (Arampatzis et al. 2005; Karamanidis and Arampatzis 2005) and 50 mm (see Hessel et al. 2021 main text and supplementary data), respectively, giving a  $k_{\text{SEE}}$  of  $3.33 P_0 \cdot L_0^{-1}$ . The inverse of normalised SEE stiffness—normalised SEE compliance (i.e. 30%)—relates closely to the

fixed-end compliance, which represents CE strain against the stretch of the SEE during a maximum tetanic contraction (Roberts 2002). We have instead defined fixed-end compliance as CE shortening expressed relative to  $L_0$ , as to allow normalised SEE compliance and fixed-end compliance to be equal. Because there is considerable passive tension at the optimal MTU length in the model (initial CE length of  $\sim 1.23 L_0$ ), consistent with experimental observations for the human plantar flexors (see Hessel et al. 2021 supplementary data), SEE deformation and CE shortening during maximum force development are  $\sim 23\%$ , rather than 30% of  $L_0$ . This value generally agrees with experimental data for the human plantar flexors (see Hessel et al. 2021 supplementary data) after considering the overestimation of fascicle shortening against the stretch of tendon and aponeurosis owing to inevitable ankle rotation (Karamanidis et al. 2005).

## 2.3 Model optimisation to simulate plantar flexion twitch of young men

Model parameters for the initial state or control condition were optimised to minimise the combined error in contraction time and half-relaxation time between simulated and experimental twitches. An additional requirement was that the relative amplitude of the simulated twitch be  $\sim 0.2 P_0$ . The simulated twitch was for an initial CE length of  $1.0 L_0$ . The experimental twitch represented the waveform average for young men determined from twitches recorded with the ankle at  $0^\circ$  and the knee extended. Initially,  $\tau_1$ ,  $\tau_2$ ,  $[a]_{50}$ ,  $n_H$  and  $V_{\text{max}}$  parameters were included in the optimization process. Where appropriate, physiological upper and lower limits were imposed. Subsequently,  $n_H$  and  $V_{\text{max}}$  were constrained at values of 3 and 6, respectively, and the optimization process was repeated.

Although reported values of  $n_H$  are wide-ranging, a value of 3 is generally intermediate between values reported for type I and II fibres or similar to values reported for the former (Stephenson and Williams 1981; Fink et al. 1986, 1990; Lynch et al. 1991; Hvid et al. 2011, 2013). The  $V_{\text{max}}$  value of  $6 L_0 \cdot \text{s}^{-1}$  agrees closely with the value of  $6.2 \text{ FL} \cdot \text{s}^{-1}$  (fibre lengths per second) measured for human medial gastrocnemius fascicles in vivo (Hauraix et al. 2015), and is comparable to values reported for rat soleus [ $6\text{--}7.3 \text{ FL} \cdot \text{s}^{-1}$  (Ranatunga and Thomas 1990; Ranatunga 1998)] and mouse soleus [ $4.5$  and  $8.6 \text{ FL} \cdot \text{s}^{-1}$  (Luff 1981; Lichtwark and Barclay 2010)] muscles at physiological temperatures; the type I fibre composition of these muscles is approximately 73 and 67%, respectively (Asmussen and Maréchal 1989). We arrived at a slightly lower estimate of 60% for the MHC I fibre content for the triceps surae [see section ‘2.3.10 Type I fibre fractional area (i.e., MHC I fibre content)’].

## 2.4 Simulating ageing-related adaptations

### 2.4.1 Free $\text{Ca}^{2+}$ concentration

There is evidence that both SR  $\text{Ca}^{2+}$  release and SR  $\text{Ca}^{2+}$  uptake are impaired in advanced age (Larsson and Salviati 1989; Delbono et al. 1995; Narayanan et al. 1996; Hunter et al. 1999; Wang et al. 2000; Jiménez-Moreno et al. 2008), and that aged single fibres can exhibit a deficit in peak free  $\text{Ca}^{2+}$  concentration (González et al. 2003; Andersson et al. 2011; Umanskaya et al. 2014). To our knowledge, the effect of slowed SR  $\text{Ca}^{2+}$  uptake on steady-state free  $\text{Ca}^{2+}$  concentration and free  $\text{Ca}^{2+}$  decay in intact fibres has not been studied in advanced age. It is unclear whether both adaptations can coexist (Russ et al. 2011, 2014) and to what extent each alteration influences free  $\text{Ca}^{2+}$  concentration. Accordingly, we simulated the independent and concomitant effects of impaired  $\text{Ca}^{2+}$  release and slowed  $\text{Ca}^{2+}$  uptake. For simplicity, we assume that the reductions in peak free  $\text{Ca}^{2+}$  concentration reported in the literature reflect impaired  $\text{Ca}^{2+}$  release without a concomitant slowing of SR  $\text{Ca}^{2+}$  uptake. This simplification allows experimental values of the deficit in  $\text{Ca}^{2+}$  concentration in intact fibres to be emulated by scaling down the instantaneous  $\text{Ca}^{2+}$  availability in the model, rather than increasing the time constant of  $\text{Ca}^{2+}$  release,  $\tau_1$ . Importantly, the fractional deficit in peak free  $\text{Ca}^{2+}$  concentration in intact fibres associated with ageing appears to be similar for maximal and submaximal contractions (González et al. 2003; Eshima et al. 2020).

To our knowledge, there exists only one study of the effect of age on SR  $\text{Ca}^{2+}$  release in human single fibres (Delbono et al. 1995), whereas several studies have been performed on rodent single fibres. In these studies, intact fibres were isolated exclusively from fast-twitch muscles without fibre type identification (Wang et al. 2000, 2002; González et al. 2003; Jiménez-Moreno et al. 2008; Andersson et al. 2011; Umanskaya et al. 2014; Fodor et al. 2020; Eshima et al. 2020). Each of these studies, including the study on human type II fibres, demonstrated an age-related deficit in SR  $\text{Ca}^{2+}$  release rate or peak intracellular  $\text{Ca}^{2+}$  concentration. Collectively, impairment typically ranged from ~30–50%. Accordingly, we incorporated a 30 or 50% reduction in peak  $\text{Ca}^{2+}$  concentration by applying a scaling factor to the instantaneous  $\text{Ca}^{2+}$  concentration of 0.7 or 0.5, respectively. We described the qualitative and quantitative effect (% change) of lower free  $\text{Ca}^{2+}$  availability on the time course (i.e., contraction time, half-relaxation time) and amplitude of the twitch, submaximal force and the force-frequency relationship, and maximum force.

### 2.4.2 SR $\text{Ca}^{2+}$ uptake ( $\tau_2$ )

The rate of SR  $\text{Ca}^{2+}$  uptake may be lower in advanced age, but it is not a universal observation. The effect of age on SR  $\text{Ca}^{2+}$  uptake rate has been predominantly studied in rodent muscle and using a variety of muscle preparations. To our knowledge, only a single study has been performed on human muscle, specifically, crude homogenates from the vastus lateralis muscle (Hunter et al. 1999). In many regards, the findings are inconsistent. Slowing has been demonstrated for skinned type II fibres but not skinned type I fibres (Larsson and Salviati 1989), SR vesicles isolated from slow-twitch muscle but not fast-twitch muscle (Narayanan et al. 1996; Russ et al. 2014), and muscle homogenates from fast-twitch (Russ et al. 2011), slow-twitch (Narayanan et al. 1996), and mixed-fibre type (Hunter et al. 1999) muscles but not in every instance (Fitts et al. 1984; Narayanan et al. 1996; Thomas et al. 2010); measurements from muscle homogenates may be susceptible to confounding by a shift in MHC isoform composition. For those studies supporting an age-related reduction in  $\text{Ca}^{2+}$  uptake rate, the size of the slowing effect ranged from ~20–52% (Larsson and Salviati 1989; Narayanan et al. 1996; Hunter et al. 1999; Russ et al. 2011). Accordingly, we incorporated a 30 or 50% reduction in the rate constant for  $\text{Ca}^{2+}$  removal. The rate constant for  $\text{Ca}^{2+}$  removal is the reciprocal of the time constant,  $\tau_2$ . Therefore,  $\tau_2$  was increased by 43 and 100%. We described the qualitative and quantitative effect of slower  $\text{Ca}^{2+}$  uptake on the time course and amplitude of the twitch, and submaximal force and the force-frequency relationship.

### 2.4.3 $\text{Ca}^{2+}$ sensitivity ( $\text{pCa}_{50}$ )

Lower  $\text{Ca}^{2+}$  sensitivity of force has been found in advanced age, but it is not a universal observation. Studies showing no effect of age (Plant and Lynch 2001; Hvid et al. 2011, 2013, 2017; Lambole et al. 2015; Teigen et al. 2020; Mazara et al. 2021) are similar in number to those showing an age-related deficit. Reduced  $\text{Ca}^{2+}$  sensitivity in advanced age has been demonstrated by several studies for type II fibres from human (Lambole et al. 2015; Straight et al. 2018; Mazara et al. 2021) and rodent (Brooks and Faulkner 1994; Lowe et al. 2002) muscles. In contrast, only a single study has shown  $\text{Ca}^{2+}$  sensitivity to be lower for type I fibres (Straight et al. 2018). The deficit in  $\text{pCa}_{50}$  reported by these studies ranges from 0.05 to 0.15 pCa units but is typically ~0.10 pCa units. Three studies reported a similar difference between means (0.08–0.10 pCa units) without detecting a significant age effect (Hvid et al. 2011, 2013; Mazara et al. 2021). For two of those studies, which sampled from just 11–15 aged type II fibres, we could deduce that the deficit in  $\text{pCa}_{50}$  was of a moderate effect size (Cohen's  $d=0.38$ – $0.49$ ). Accordingly,

we incorporated a reduction in  $pCa_{50}$  of 0.05 or 0.10 pCa units and described the qualitative and quantitative effect on the time course and amplitude of a twitch, submaximal force and the force-frequency relationship, maximum force, and relative force summation.

#### 2.4.4 Cooperativity of activation ( $n_H$ )

The weight of evidence from human and rodent studies indicates that the slope of the force-pCa relationship (i.e. cooperativity)—represented by the Hill coefficient,  $n_H$ —is unaltered in advanced age (Eddinger et al. 1986; Brooks and Faulkner 1994; Hvid et al. 2011, 2013; Lambolely et al. 2015; Straight et al. 2018; Teigen et al. 2020). Challenging this view is one study on human muscle that found  $n_H$  to be elevated for type II fibres in advanced age (Straight et al. 2018) and one study on rat muscle that found  $n_H$  ( $> 0.5 P_0$ ) to be lower for type II fibres (Lowe et al. 2002). Because there are generally pronounced differences in  $n_H$  between fibre types (Fink et al. 1986, 1990; Gardetto et al. 1989; Danieli-Betto et al. 1990; Gregorevic et al. 2004; Hvid et al. 2011, 2013), and stronger evidence that  $n_H$  is affected by disuse (Gardetto et al. 1989; Widrick et al. 1998; Hvid et al. 2011, 2013; Monti et al. 2021), we thought it was important to illustrate the effect of this parameter on force generation. We performed simulations in which the reference value of  $n_H$  was increased and decreased by 1.0. We described the qualitative and quantitative effect on the time course and amplitude of a twitch, submaximal force and the force-frequency relationship, and relative force summation.

#### 2.4.5 Lower free $Ca^{2+}$ concentration & lower $Ca^{2+}$ sensitivity ( $pCa_{50}$ ) in concert

Because the force-pCa relationship is sigmoidal in form, force at near-maximal  $Ca^{2+}$  concentrations is practically insensitive to shifts in  $Ca^{2+}$  sensitivity. A deficit in maximum force generation may only arise when  $Ca^{2+}$  concentration and  $Ca^{2+}$  sensitivity decrease concomitantly. Accordingly, we reduced the instantaneous  $Ca^{2+}$  concentration by 30 or 50% whilst lowering  $pCa_{50}$  by 0.05 or 0.10 pCa units, consistent with our previous manipulations of  $Ca^{2+}$  concentration and  $Ca^{2+}$  sensitivity. We described the qualitative effect of concurrent reductions in  $Ca^{2+}$  concentration and  $Ca^{2+}$  sensitivity on submaximal force and the force-frequency relationship, and quantified the effect on maximal force.

#### 2.4.6 Lower $Ca^{2+}$ release & slower $Ca^{2+}$ uptake ( $\tau_2$ ) in concert

It is unclear from recordings of intracellular  $Ca^{2+}$  transients whether impaired  $Ca^{2+}$  release and slowed  $Ca^{2+}$  uptake occur in parallel and the extent to which they may offset one another (González et al. 2003; Andersson et al. 2011; Eshima et al. 2020). Accordingly, we reduced  $Ca^{2+}$  release by 30% and the rate constant of  $Ca^{2+}$  uptake by 40 (67% increase in  $\tau_2$ ) in concert. Reductions of equal amount would not alter steady-state  $Ca^{2+}$  in the model relative to the control condition. We described the qualitative effect of lower  $Ca^{2+}$  release and slower  $Ca^{2+}$  uptake on submaximal force and the force-frequency relationship.

#### 2.4.7 Lower $Ca^{2+}$ sensitivity ( $pCa_{50}$ ) and slower $Ca^{2+}$ uptake ( $\tau_2$ ) in concert

On the basis that slower  $Ca^{2+}$  uptake will increase free  $Ca^{2+}$  concentration, thereby increasing force, whereas lower  $Ca^{2+}$  sensitivity will act to decrease force, we examined the effect of these two adaptations acting concomitantly. Specifically, we incorporated both a 30% reduction in the rate constant for  $Ca^{2+}$  removal (43% increase in  $\tau_2$ ) and a 0.1 pCa unit reduction in  $Ca^{2+}$  sensitivity ( $pCa_{50}$ ) and described the qualitative effect on the force-frequency relationship.

#### 2.4.8 Maximum velocity of shortening ( $V_{max}$ )

Comparatively, the intrinsic speed of shortening has been extensively studied in young and old muscle fibres from humans and rodents. For both groups, and for both fibre types, the effect of age is inconsistent. Several studies have demonstrated slowing of either or both type I and type II human fibres (Krivickas et al. 2001; D'Antona et al. 2003; Ochala et al. 2007; Yu et al. 2007; Power et al. 2016; Brocca et al. 2017), but just as many studies have found no age effect (Trappe et al. 2003; Claffin et al. 2011; Sundberg et al. 2018; Teigen et al. 2020; Grosicki et al. 2021; Mazara et al. 2021). Similarly, a lower maximal shortening velocity has been demonstrated for aged type I and type II fibres from rodents (Degens et al. 1998; Thompson and Brown 1999; Kim and Thompson 2013), but not in every instance (Eddinger et al. 1986; Brooks and Faulkner 1994; Zhong et al. 2006; Kim and Thompson 2013). Muscle inactivity in advanced age may minimize or negate the effect of age on  $V_{max}$  (Thompson et al. 1998; D'Antona et al. 2003; Kim and Thompson 2013), although there is evidence to the contrary (Grosicki et al. 2021). The deficit in maximal shortening velocity reported for human muscle fibres ranges from ~7–46% (Larsson et al. 1997; Krivickas et al. 2001; Claffin et al. 2011; Power et al. 2016) but is most often ~15–25% (Larsson et al. 1997; Krivickas et al. 2001; D'Antona et al. 2003; Ochala et al.



2007; Yu et al. 2007; Brocca et al. 2017). The slowing of intrinsic shortening speed tends to be more pronounced for rodent muscle fibres; three of the four identified instances of slowing represent a deficit of 32–50% (Degens et al. 1998; Thompson and Brown 1999; Kim and Thompson 2013). Accordingly, we incorporated reductions in intrinsic shortening speed of 30 or 50% and described the qualitative and quantitative effect on the time course and amplitude of a twitch and brief tetanic contraction.

The curvature of the force–velocity relationship (i.e.  $a/P_0$ ) does not appear to be altered in aged fibres that do not exhibit a reduction in  $V_{\max}$  (Brooks and Faulkner 1994; Trappe et al. 2003). To our knowledge,  $a/P_0$  has not been quantified for aged fibres exhibiting a reduction in  $V_{\max}$ . However, because  $a/P_0$  differs markedly between fibre types—human type IIa fibres compared to type I fibres exhibit a two-fold greater value of  $a/P_0$ —(Bottinelli et al. 1996; Widrick et al. 1996; Gilliver et al. 2009)—we deemed it important to illustrate the effect of this parameter on force development. We performed simulations in which the reference value of  $a/P_0$  was increased by 0.05 (50%). We described the qualitative effect on the time course and amplitude of a twitch and brief tetanic contraction. We did not incorporate reductions in  $a/P_0$  because the model was unable to simulate the twitch measured experimentally with a more realistic value for muscle at physiological temperatures [model: 0.10; mouse soleus: 0.18 (Luff 1981); rat soleus: 0.22–0.26 (Ranatunga and Thomas 1990; Ranatunga 1998)].

#### 2.4.9 SEE stiffness

The general effect of age on tendon stiffness appears to be distinct for humans compared to certain animal models of ageing. The weight of evidence from in vivo human studies favours an age-associated reduction in tendon stiffness and elastic modulus (see McCrum et al., 2018). Though some studies have found tendon loading behaviour to be unchanged (Carroll et al. 2008; Couppe et al. 2012), no human studies appear to have reported an age-related increase in tendon stiffness. A recent review reported median reductions in stiffness and elastic modulus of 20% and 28%, respectively (McCrum et al. 2018). However, age-related deficits may be as high as 30–55% (Karamanidis and Arampatzis 2006; Onambele et al. 2006; Stenroth et al. 2012; Csapo et al. 2014). Moreover, relative to old adults (> 65 years), very old adults (> 83 years) can exhibit marked reductions (35–40%) in tendon stiffness and elastic modulus (Eriksen et al. 2018).

In contrast to humans, hindlimb tendons of rodents in advanced age regularly exhibit higher stiffness or elastic modulus (Wood et al. 2011; Danos et al. 2016; Wood and Brooks 2016; Leahy et al. 2022). The magnitude of the increase is typically close to 50%. A number of studies have also reported no ageing effect (Nakagawa et al. 1996; Pardes et al. 2017); fewer have reported an age-related reduction (LaCroix et al. 2013). The variable nature of tendon mechanics in advanced age may be partially explained by methodological approach, age at measurement, ageing-associated inactivity, species, and muscle function (Svensson et al. 2016; McCrum et al. 2018).

We incorporated both a reduction in normalised SEE stiffness of 30% and an increase in normalised stiffness of 50%. We described the qualitative and quantitative effect of SEE stiffness on the time course and amplitude of a twitch and brief tetanic contraction.

#### 2.4.10 Type I fibre fractional area (i.e., MHC I fibre content)

Several human and rodent studies have reported an ageing-related increase of 0.10–0.20, or greater (Brocca et al. 2017), for fractional MHC I content or fractional area occupied by type I fibres (Larsson et al. 1978; Klitgaard et al. 1990b; Kadhiresan et al. 1996; Short et al. 2005; Cui et al. 2008; Nilwik et al. 2013; Sonjak et al. 2019; Soendenbroe et al. 2022). Smaller shifts have also been reported (Sullivan et al. 1995; Hunter et al. 1999). We approximated the effect of this adaptation by considering fibre type-related differences in  $\text{Ca}^{2+}$  removal rate,  $\text{Ca}^{2+}$  sensitivity and cooperativity, and  $V_{\max}$ , and by adjusting composite parameter values according to an increase in type I fibre fractional area. Fibre type-specific values and composite relationships were derived from the whole muscle control values by assigning weightings based on the fractional cross-sectional area of type I and II fibres and assigning fibre type-related differences in each property (Wakeling et al. 2012). Fibre type-specific and composite parameter values were determined according to the following expression:

$$(x_{\text{slow}} \times p_{\text{slow}}) + (x_{\text{fast}} \times p_{\text{fast}}) = x_{\text{whole}} \times \frac{x_{\text{slow}}}{x_{\text{fast}}} = y$$

where  $x$  is the fibre type-specific parameter value,  $p$  is relative fibre content,  $x_{\text{whole}}$  is the whole muscle parameter value, and  $y$  is the fibre type-related difference or offset. Some empirical observations support this approach. Single fast and slow fibres arranged in parallel exhibit an intermediate force–pCa relationship generally consistent with a theoretical composite relationship based on fractional fibre

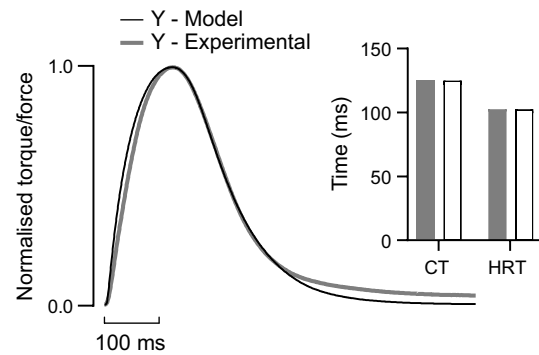
type content (Lynch et al. 1995). In contrast to some methods (Zajac 1989; Clafin and Faulkner 1989; Ranatunga and Thomas 1990), our approach assumes some degree of attenuation of shortening speed at loads where whole muscle velocity exceeds the  $V_{\max}$  assigned to type I fibres, which is generally consistent with observations that inactive muscle depresses the speed of shortening (Hatcher and Luff 1987; Holt et al. 2014).

The total MHC isoform content or fractional area occupied by type I fibres is approximately 50 and 65% for the gastrocnemius and soleus muscles, respectively (Edström and Nyström 1969; Green et al. 1981; Coggan et al. 1992; Harridge et al. 1996, 1998). Thus, given that the combined physiological cross-sectional area (PCSA) of the lateral and medial gastrocnemius muscles represents ~38% of the total PCSA of the triceps surae (Morse et al. 2005; Albracht et al. 2008; Crouzier et al. 2018), it is estimated that the total type I fibre area of the triceps surae is ~60% (i.e. 0.60). Type I fibres, compared to type II fibres, were assumed to exhibit the following differences:  $\text{Ca}^{2+}$  removal rate constant 50% slower (Carroll et al. 1997; Liu et al. 1997; Baylor and Hollingworth 2003; Calderón et al. 2010);  $\text{Ca}^{2+}$  sensitivity ( $\text{pCa}_{50}$ ) 0.15  $\text{pCa}$  units greater and  $n_{\text{H}}$  40% lower (Stephenson and Williams 1981; Fink et al. 1986, 1990; Ruff 1989; Laszewski-Williams et al. 1989; Gardetto et al. 1989; Ruff and Whittlesey 1991; Plant and Lynch 2001; Gregorevic et al. 2004; Hvid et al. 2013; Xu et al. 2017; Lamboley et al. 2020);  $V_{\max}$  70% slower (Larsen and Moss 1993; Bottinelli et al. 1996; Harridge et al. 1996; Widrick et al. 2002; Trappe et al. 2003; Yu et al. 2007; Luden et al. 2008; Sundberg et al. 2018; Teigen et al. 2020). Note that much variability exists for the force-pCa relationships of type I and type II fibres.

After increasing the fractional area of type I fibres by 0.10 and 0.20, from 0.60 to 0.70 and 0.80, respectively, and incorporating adjusted values of  $\tau_2$ ,  $\text{pCa}_{50}$ ,  $n_{\text{H}}$  and  $V_{\max}$ , we described the qualitative and quantitative effect on the contraction time and half-relaxation time of the twitch, and on submaximal force and the force-frequency relationship.

## 2.5 Model optimisation to simulate plantar flexion twitch of old men

The parameters of the model were adjusted to simulate the plantar flexion twitch of old men. The optimisation approach was similar to that used initially, except parameter limits were imposed consistent with the directionality of impairment. We also incorporated a force-generating capacity (FGC) parameter—analogue to muscle PCSA—to allow twitch force to be lower in advanced age, which we observed experimentally. We assumed that the deficit in twitch force is owing, at least in part, to muscle atrophy (Narici et al. 2003; Morse et al. 2005; Thom et al. 2007). The magnitude of a



**Fig. 2** Hill-type muscle model optimisation. Experimental plantar flexion twitch torque and simulated twitch force for young (Y) adult humans. *Inset*, twitch contraction time (CT) and half-relaxation time (HRT) for experimental (filled) and simulated (open) data were identical following parameter optimization (CT: 125 ms; HRT: 102.5 ms). Agreement was achieved between twitch torque measured with the ankle at  $0^\circ$  and the knee extended and twitch force simulated at an initial CE length of  $1.0 L_0$

given parameter adjustment was compared to the parameter change incorporated to simulate age-related adaptation reported in the literature.

## 3 Results

### 3.1 Model optimisation to simulate plantar flexion twitch of young men

Force during simulated and experimental twitches are shown in Fig. 2. The time course of force rise and decay are matched well, with both the contraction time and half-relaxation time of the simulated twitch being identical to the values measured experimentally for young men (*inset* Fig. 2). All model parameters used in simulations of young muscle (i.e., control condition) are reported in Table 1. Unless specified otherwise, all simulated fixed-end contractions were performed at an initial CE length of  $1.23 L_0$  and force displayed in figures represents active CE force. This initial length for a maximal tetanic contraction resulted in a final CE length—after shortening against the stretch of the SEE—on the plateau of the force-length relationship.

### 3.2 $\text{Ca}^{2+}$ handling and thin filament activation

#### 3.2.1 Instantaneous $\text{Ca}^{2+}$ concentration

Reducing the instantaneous free  $\text{Ca}^{2+}$  concentration by either 30 or 50% dramatically lowered twitch force and abbreviated the rise and decay of twitch force (Fig. 3b, *inset*). Substantial force loss was also evident during sustained stimulation at submaximal frequencies, as shown by the marked rightward

**Table 1** Model parameters for plantar flexors muscles of young adult men

Pulse width (s)	$\tau_1$ (s)	$\tau_2$ (s)	$[a]_{50}$	$pCa_{50}$ (pCa)	$n_H$	$V_{max}$ ( $L_0 \cdot s^{-1}$ )	$a/P_0$	$\epsilon_{SEE}$	$k_{SEE}$ ( $P_0 \cdot L_0^{-1}$ )	$L_0$ (mm)	$L_{SEE}$ (mm)
0.0048	0.0422	0.256	0.1025	5.99	3	6	0.10	0.05	3.33	50	300

shift of the force-frequency relationship (Fig. 3d, e). There was a pronounced deficit in force for frequencies yielding calcium concentrations situated on the steep region of the force-pCa relationship (Fig. 3e, f). In contrast, maximum tetanic force was only modestly affected by the imposed reductions in free  $Ca^{2+}$  concentration (Fig. 3e, f). During 200 Hz stimulation, the 50% reduction in  $Ca^{2+}$  availability only lowered cross-bridge activation to 97%. Because submaximal force was disproportionately affected, reduced  $Ca^{2+}$  availability lowered the ratio of twitch-to-tetanic force.

### 3.2.2 $Ca^{2+}$ uptake

Decreasing the rate constant of  $Ca^{2+}$  decay by 30% to slow the removal of  $Ca^{2+}$  increased twitch force by 12% (elevating the ratio of twitch-to-tetanic force) and prolonged the contraction time and half-relaxation time by 25% and 38%, respectively (Fig. 4b, inset). Slowing  $Ca^{2+}$  uptake by 50% increased the size of these effects. Slower  $Ca^{2+}$  removal during sustained stimulation resulted in greater calcium accumulation (Fig. 4c), which caused force at submaximal frequencies to increase dramatically (Fig. 4d), as illustrated by the leftward-shifted force-frequency relationships (Fig. 4e).

### 3.2.3 Calcium sensitivity ( $pCa_{50}$ )

Reducing the  $Ca^{2+}$  sensitivity of force by shifting the force-pCa relationship rightward 0.05 pCa units reduced twitch force by 16% and abbreviated the twitch contraction time and half-relaxation time by 11 and 5%, respectively (Fig. 5b, inset). Lowering  $Ca^{2+}$  sensitivity by 0.10 pCa units resulted in additional force attenuation and an even briefer contraction. Reduced  $Ca^{2+}$  sensitivity also decreased force during stimulation at submaximal stimulation frequencies (< 50 Hz) such that the force-frequency relationship was shifted rightward (Fig. 5c). Force loss was greatest for frequencies that encompassed the steep region of the force-pCa relationship and increased in proportion to the reduction in  $Ca^{2+}$  sensitivity. Maximum tetanic force was unaffected by the imposed reductions in  $Ca^{2+}$  sensitivity; no force loss was evident for 100 or 200 Hz stimulation. Relative force summation—illustrated as the force during a brief tetanic contraction (50 ms, 100 Hz) expressed relative to twitch force (Fig. 5d, inset)—was higher following the reduction in  $Ca^{2+}$  sensitivity, though there remained a deficit in tetanic force.

### 3.2.4 Cooperativity of activation ( $n_H$ )

Decreasing  $n_H$ , or cooperativity, from 3 to 2 to reduce the slope of the force-pCa relationship increased twitch force by 11% and prolonged the twitch contraction time and half-relaxation time by 26 and 44%, respectively (Fig. 5f, inset). Lowering cooperativity also reduced the slope of the force-frequency relationship such that force was slightly greater at low frequencies but considerably lower at moderate and high frequencies of stimulation (Fig. 5g); increasing cooperativity had the opposite effect. Again, maximum tetanic force was largely unaffected by altering cooperativity. A small deficit (2%) in maximum cross-bridge activation level arose when cooperativity was lowered. As such, reducing cooperativity increased the ratio of twitch-to-tetanic force, whereas increasing cooperativity reduced this ratio. Similarly, lowering cooperativity also reduced relative force summation (Fig. 5h, inset). Despite twitch force being 20% ( $0.04 P_0$ ) greater for a  $n_H$  of 2 compared to a  $n_H$  of 4, peak force during the brief tetanic contraction (50 ms, 100 Hz) was 12% ( $0.06 P_0$ ) lower for the former compared to the latter (Fig. 5h).

### 3.2.5 Lower $Ca^{2+}$ concentration & lower $Ca^{2+}$ sensitivity in concert

Reducing  $Ca^{2+}$  concentration and  $Ca^{2+}$  sensitivity in concert lowered force dramatically at submaximal stimulation frequencies but only slightly reduced maximum tetanic force (Fig. 6b, c). Reducing  $Ca^{2+}$  availability by 30% and lowering  $pCa_{50}$  by 0.05 pCa units merely reduced the cross-bridge activation level to 98% during 200 Hz stimulation (Fig. 6b). Even when calcium concentration and calcium sensitivity were concurrently reduced by 50% and 0.10 pCa units, respectively, cross-bridge activation ( $Act$ ) still exceeded 92% during 200 Hz stimulation (Fig. 6c). For 100 Hz stimulation, the steady-state  $Ca^{2+}$  concentration was 29% lower compared to 200 Hz. As such, there was a more significant reduction in cross-bridge activation level during 100 Hz stimulation when a 50% reduction in  $Ca^{2+}$  concentration was imposed and  $Ca^{2+}$  sensitivity was concurrently reduced by 0.05 ( $Act = 87\%$ ) or 0.10 pCa ( $Act = 82\%$ ) units (Fig. 6c). Figure 6d illustrates how the sigmoidal form of the force-pCa relationship limits the effect of an imposed reduction in  $Ca^{2+}$  concentration on maximum tetanic force, even when the  $Ca^{2+}$  sensitivity of force is reduced by 0.1 pCa units.

**Fig. 3** Effect of calcium concentration on submaximal and maximal force generation. **a** Activator concentration and **b** active force during a twitch at  $1.23 L_0$  with varying levels of instantaneous  $\text{Ca}^{2+}$  concentration (con.). Instantaneous  $\text{Ca}^{2+}$  concentration was reduced by 30 and 50% relative to the control condition. *Inset*, twitch contraction time and half-relaxation time. **c** Activator concentration and **d** active force during sustained 10 Hz stimulation at  $1.23 L_0$ . **e** Force-frequency relationships at  $1.23 L_0$ . Active force expressed relative to  $P_0$  of control condition. **f** Activation-pCa relationships. In **e** and **f**, solid squares denote 10 Hz stimulation and small and large solid circles denote 100 and 200 Hz stimulation, respectively. In **f**, shaded regions represent the  $\text{Ca}^{2+}$  concentration range between 100 and 200 Hz

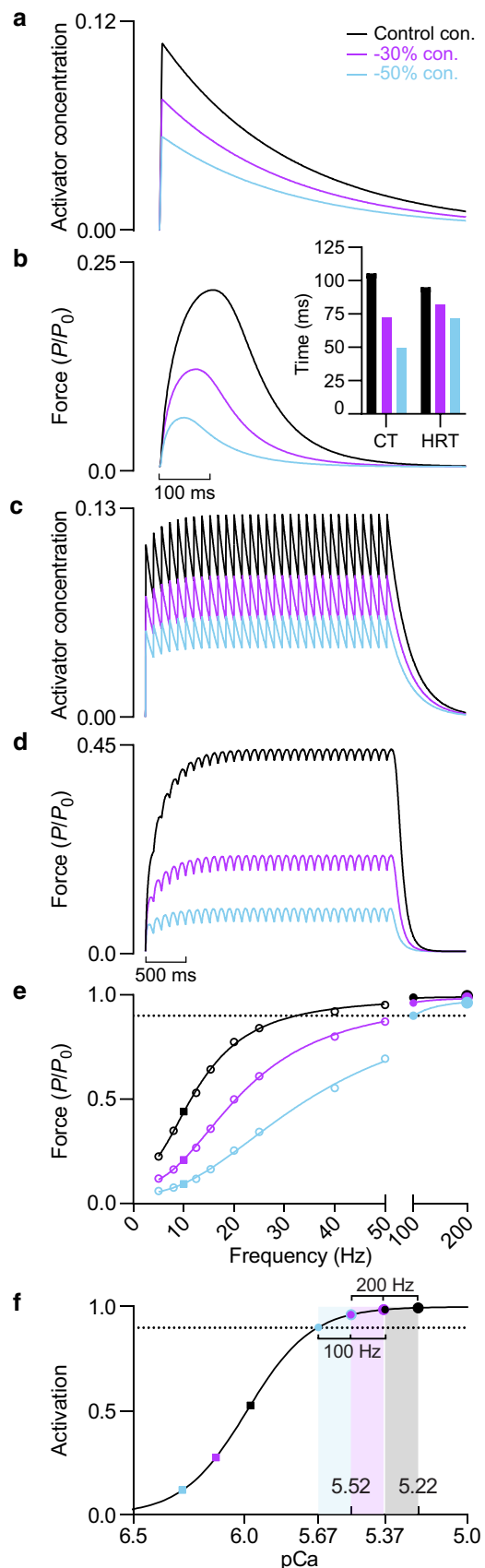
### 3.2.6 Slower $\text{Ca}^{2+}$ uptake and lower $\text{Ca}^{2+}$ release or lower $\text{Ca}^{2+}$ sensitivity in concert

The pronounced deficit in steady-state force at low and moderate stimulation frequencies that resulted from a 30% reduction in  $\text{Ca}^{2+}$  release (Fig. 3e) was more than balanced by concurrently decreasing the rate constant for  $\text{Ca}^{2+}$  uptake by 40% (Fig. 7b, c). The reduction in  $\text{Ca}^{2+}$  release caused force to be lower at the beginning of the contraction, as is evident when twitch force is compared (Fig. 7b); however, the slower rate of  $\text{Ca}^{2+}$  removal allowed  $\text{Ca}^{2+}$  to accumulate to a higher steady-state concentration (Fig. 7a). A similar compensation effect occurred when  $\text{Ca}^{2+}$  uptake rate was reduced by 30% whilst  $\text{Ca}^{2+}$  sensitivity was lowered by 0.10 pCa units. During a twitch and at very low stimulation frequencies, lower  $\text{Ca}^{2+}$  sensitivity reduced force (Fig. 7e, f). At faster frequencies, the increase in  $\text{Ca}^{2+}$  concentration more than compensated for the reduction in  $\text{Ca}^{2+}$  sensitivity, shifting the force-frequency relationship leftward (Fig. 7e, f).

## 3.3 CE-SEE interaction

### 3.3.1 Maximum velocity of shortening ( $V_{\max}$ )

Because the CE shortens against the stretch of the SEE during force development (see Fig. 8c *inset*), reducing  $V_{\max}$  by 30% reduced twitch force by 12% and increased twitch contraction time by 13%; twitch half-relaxation time was practically unaltered (Fig. 8b, *inset*). A similar effect was observed for a brief tetanic contraction (50 ms, 100 Hz) following a 30% reduction in  $V_{\max}$  (Fig. 8c). Lowering  $V_{\max}$  by 50% increased the loss of force and further prolonged the rise of force. Brief tetanic contractions were performed at an initial CE length of  $1.0 L_0$ , illustrating that the reductions in peak force with decreasing  $V_{\max}$  arise despite more favourable final CE lengths—greater force arises from greater shortening against the stretch of the SEE (Fig. 8c *inset*). Increasing  $a/P_0$  produced qualitatively similar results for twitch and tetanic contractions as increasing  $V_{\max}$  (Fig. 8).



**Fig. 4** Effect of calcium uptake rate on force generation at submaximal calcium. **a** Activator concentration and **b** active force during a twitch at  $1.23 L_0$  with varying rates of  $\text{Ca}^{2+}$  removal (rem.). The rate constant of  $\text{Ca}^{2+}$  removal was reduced by 30 and 50% relative to the control condition, representing increases in the time constant of  $\text{Ca}^{2+}$  removal,  $\tau_2$ , of 43 and 100%, respectively. *Inset*, twitch contraction time and half-relaxation time. **c** Activator concentration and **d** active force during sustained 10 Hz stimulation at  $1.23 L_0$ . **e** Force-frequency relationships at  $1.23 L_0$ . Active force expressed relative to  $P_0$  of control condition. *Inset*, activation-pCa relationship. Solid squares denote the activator concentration and activation level during sustained stimulation at 10 Hz

### 3.3.2 SEE stiffness ( $k_{\text{SEE}}$ )

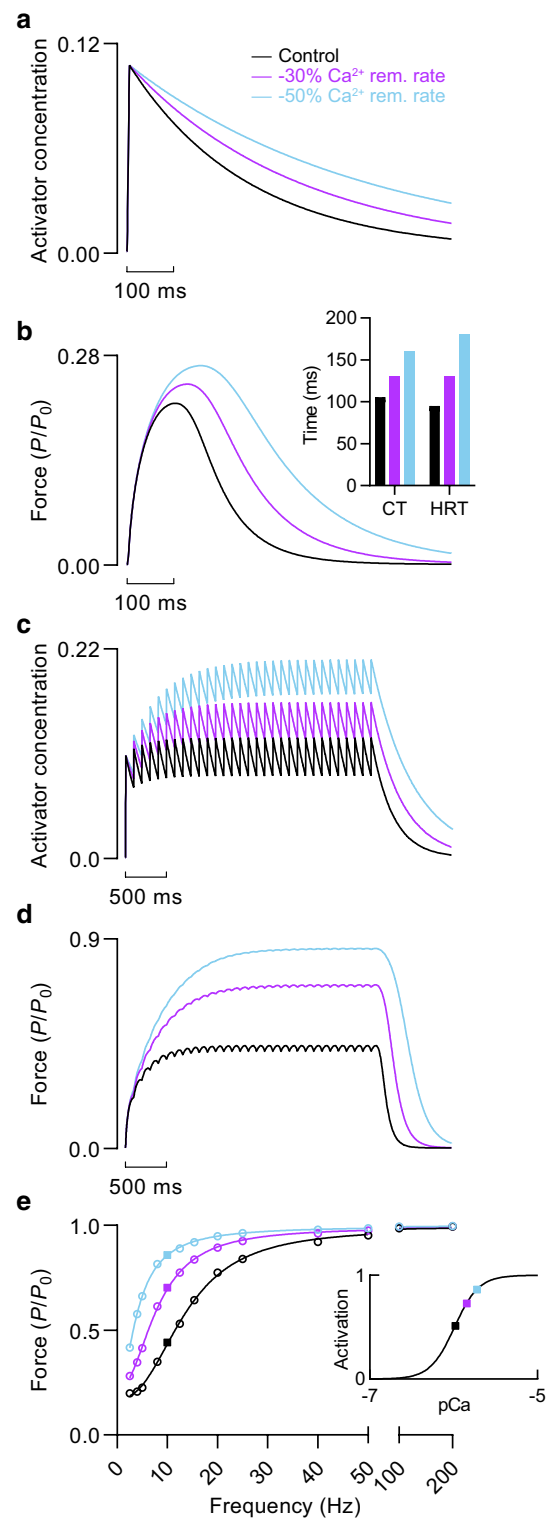
Reducing SEE stiffness by 30% prolonged twitch contraction time by 13% and attenuated twitch force by 9%. Conversely, increasing SEE stiffness by 50% abbreviated twitch rise time by 14% and increased twitch force by 9% (Fig. 8e). The attenuation or improvement of the rate of force development and peak force during a brief contraction was not the result of less or more favourable CE operating lengths, which were restricted to the descending limb of the force-length relationship. For brief tetanic contractions performed at an initial CE length of  $1.23 L_0$ , peak force was greatest for the stiffer SEE condition, even though the average operating length of the CE was less favourable (Fig. 8f, *inset*).

### 3.3.3 $V_{\text{max}}$ & SEE stiffness interaction

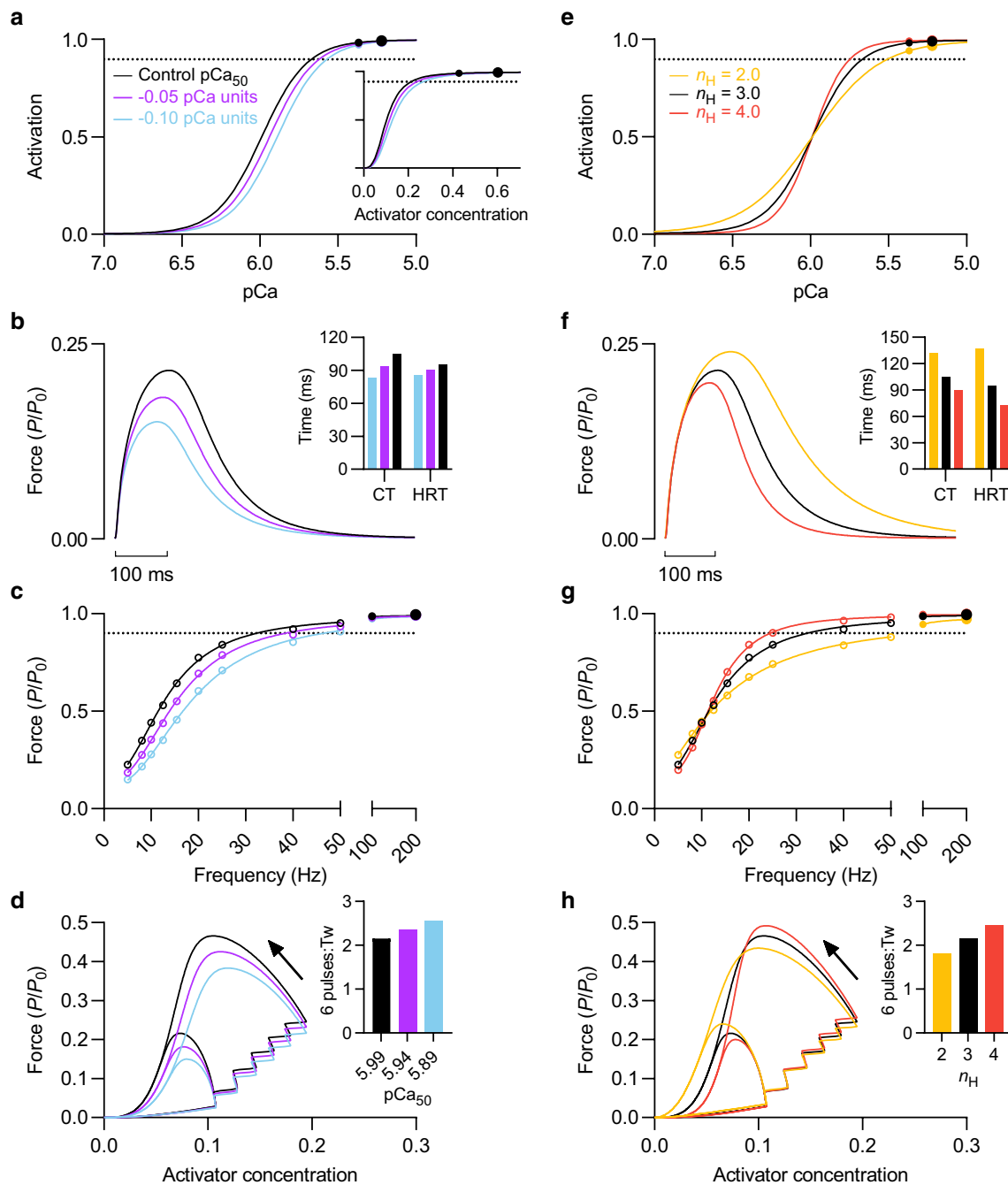
Decreasing  $V_{\text{max}}$  by 50%, from  $6$  to  $3 L_0 \cdot \text{s}^{-1}$ , had a more modest effect on peak twitch force when SEE stiffness was adjusted to give normalised SEE deformations of less than 8% (compare Fig. 9b and 8b). At 3.33% (i.e.,  $30 P_0 \cdot L_0^{-1}$ ), twitch force was 13% ( $0.05 P_0$ ) lower (Fig. 9b). In contrast, reducing  $V_{\text{max}}$  by 50% lowered twitch force (at a comparable initial CE length) by 26% ( $0.06 P_0$ ) when normalised SEE deformation was 30% [i.e.,  $3.33 P_0 \cdot L_0^{-1}$  (Fig. 8b)]. The greater effect of intrinsic shortening speed on force development with decreasing SEE stiffness was independent of differences in force-generating potential related to CE length (Fig. 9c).

## 3.4 Type I fibre fractional area

Adjusting the rate constant of  $\text{Ca}^{2+}$  decay, the force-pCa relationship, and  $V_{\text{max}}$  to reflect a fractional increase in type I fibre area resulted in elevated twitch force and prolonged force rise and decay during a twitch (Fig. 10). Specifically, increasing the type I fibre area from 0.60 to 0.70 increased the twitch contraction time and half-relaxation time by 17 and 15%, respectively (Fig. 10d, *inset*). The slowing effect increased to 37 and 33% when type I fibre area was

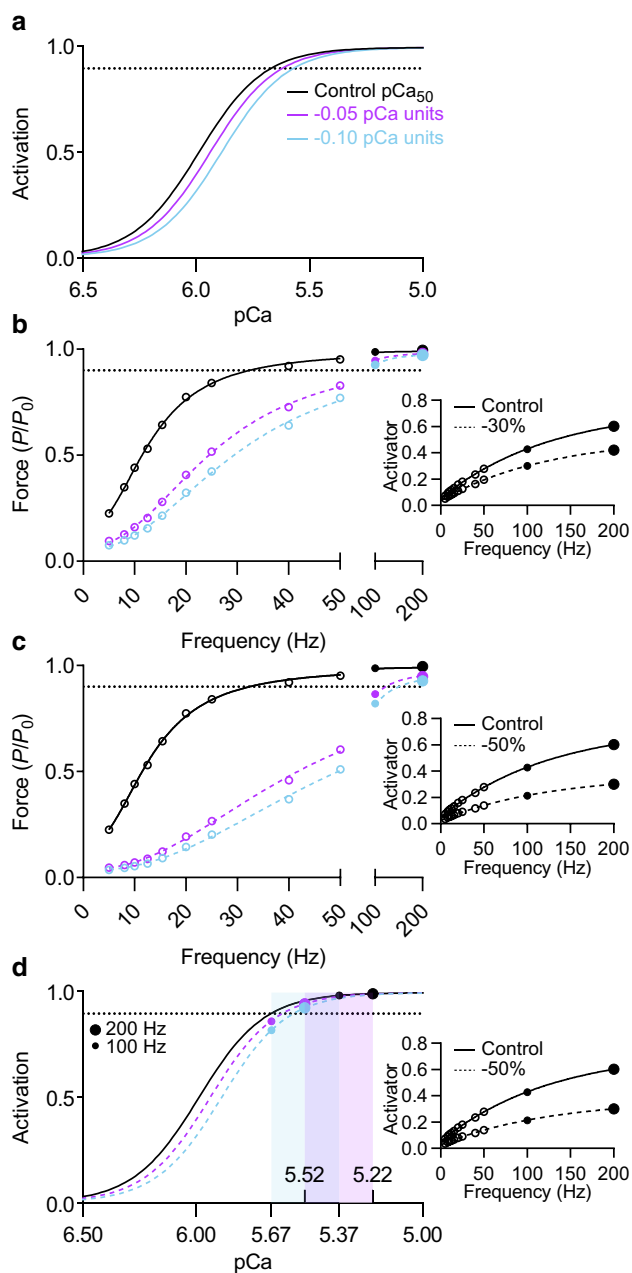


increased to 0.80. Both adjustments of type I fibre fractional area increased force at submaximal stimulation frequencies (Fig. 10e), with the latter causing the greatest leftward shift of the force-frequency relationship (Fig. 10f).



**Fig. 5** Effect of calcium sensitivity and cooperativity on force at submaximal and maximal calcium concentrations. **a** Activation-pCa relationships with varying  $\text{Ca}^{2+}$  sensitivities and **e** cooperativities.  $\text{Ca}^{2+}$  sensitivity of force was reduced by 0.05 and 0.10 pCa units relative to the control condition. Cooperativity was decreased from 3 to 2 and increased to 4. **a** *Inset*, corresponding activation-activator relationships. Small and large black circles denote 100 and 200 Hz stimula-

tion, respectively. **b, f** Twitch force at  $1.23 L_0$ . *Inset*, twitch contraction time and half-relaxation time. **c, g** Force-frequency relationships at  $1.23 L_0$ . Active force expressed relative to  $P_0$  of control condition. **d, h** Active force plotted as a function of activator concentration for a 50 ms, 100 Hz train (i.e., 6 pulses) at  $1.23 L_0$ . *Inset*, force summation; the ratio of tetanic (50 ms, 100 Hz) force-to-twitch force



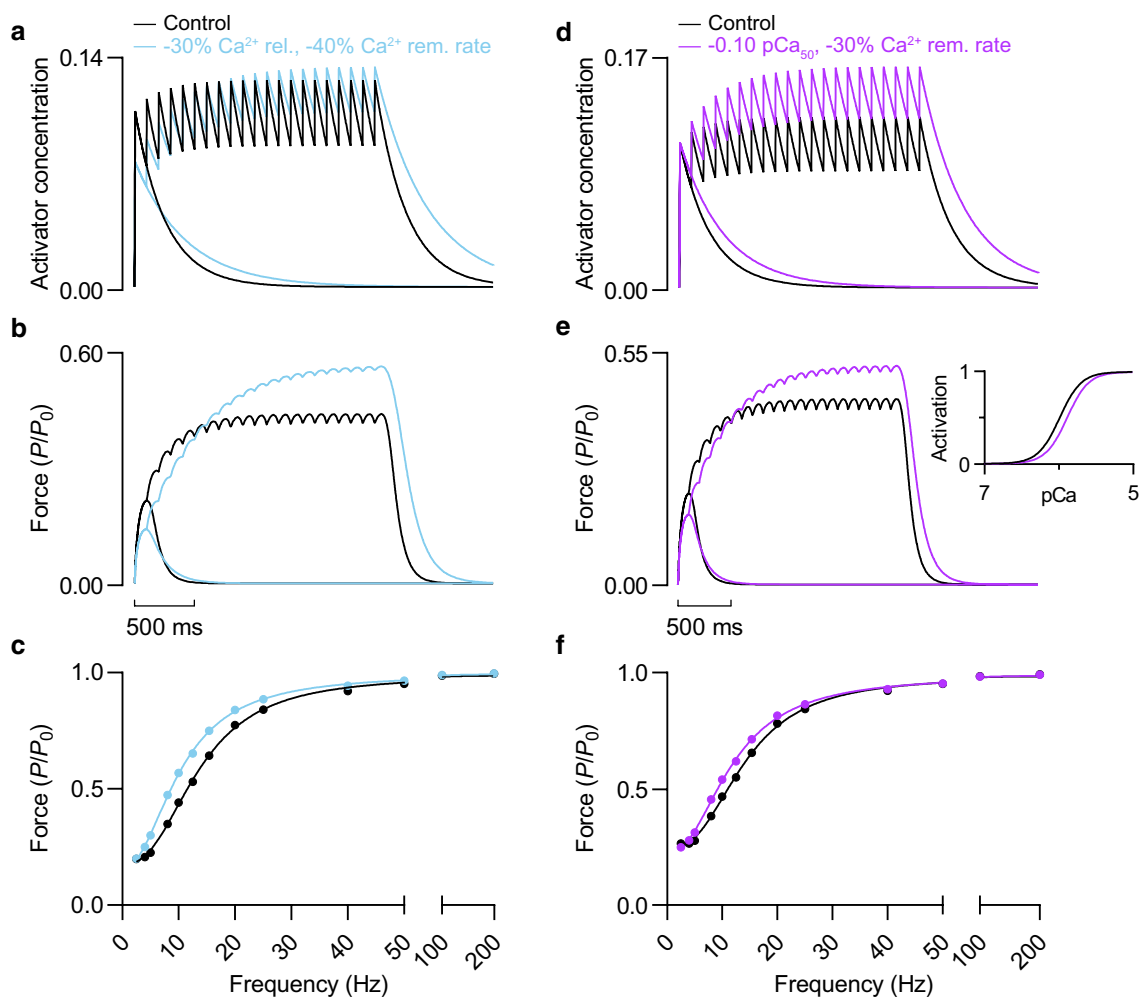
**Fig. 6** Effect of reducing calcium concentration and  $\text{Ca}^{2+}$  sensitivity in concert on maximal force generation. **a** Activation-pCa relationships with varying  $\text{Ca}^{2+}$  sensitivities.  $\text{Ca}^{2+}$  sensitivity was reduced by 0.05 and 0.10 pCa units relative to the control condition (5.99). **b**, **c** Force-frequency relationships at  $1.23 L_0$  for concomitant reduction in  $\text{Ca}^{2+}$  concentration and  $\text{Ca}^{2+}$  sensitivity. Force expressed relative to  $P_0$  of control condition. Instantaneous activator concentration was reduced by 30% in **b** and 50% in **c**. *Inset*, activator-frequency relationships for control and reduced  $\text{Ca}^{2+}$  concentration (dashed) conditions. **d** Activation-pCa relationships illustrating  $\text{Ca}^{2+}$  concentration and activation level for 100 (small circle) and 200 Hz (large circle) stimulation. Data are shown for a 50% reduction in instantaneous activator concentration. The two overlapping shaded regions represent the  $\text{Ca}^{2+}$  concentration range between the control and 50% reduction conditions for 100 and 200 Hz stimulation. *Inset*, activator-frequency relationships

### 3.5 Model optimisation to simulate plantar flexor twitch of old men

The plantar flexor twitch of older men was of a lower amplitude (18%) and exhibited a prolonged contraction time (25%) and prolonged half-relaxation time (29%) compared to young adult men (Table 2, Fig. 11a). The weaker, slower twitch in advanced age was well-simulated by the model with ageing-realistic adjustments to a few parameters (Fig. 11b, c). To emulate the time course and relative amplitude of the twitch exhibited by older men, which was possible with multiple parameter combinations, required significant slowing of  $\text{Ca}^{2+}$  uptake rate ( $\sim 25\%$ , Table 3). Because slowing the uptake of  $\text{Ca}^{2+}$  prolonged the duration of the  $\text{Ca}^{2+}$  transient, which increased twitch force, it was possible for the reduction in force-generating capacity (23%) to exceed that of the reduction in twitch force (18%) despite additional force loss from reductions in  $V_{\max}$  and SEE stiffness (Table 3). A smaller reduction in force-generating capacity (15%) was possible with the addition of modest reductions in  $\text{Ca}^{2+}$  release and  $\text{Ca}^{2+}$  sensitivity, which had to be balanced by further slowing of  $\text{Ca}^{2+}$  uptake. Incorporating slower  $\text{Ca}^{2+}$  uptake produced a leftward shift of the force-frequency relationship (Fig. 11c *inset*).

## 4 Discussion

$\text{Ca}^{2+}$  transportation and calcium-activated force are perturbed in advanced age. Model simulations in the current work show that imposing literature-informed deficits in free  $\text{Ca}^{2+}$  concentration or  $\text{Ca}^{2+}$  sensitivity of force results in a substantial loss of submaximal force and a slow-to-fast shift in several indices of contraction speed. Their combined effect is especially dramatic. Imposing slowed  $\text{Ca}^{2+}$  reuptake had the opposite effect on contractile performance, increasing twitch force and the ratio of twitch-to-tetanic force, prolonging the duration of contraction, and shifting the force-frequency leftward. Simulations estimating the effect of a fractional increase in type I fibre area produced the same outcomes, although to a lesser extent. It is difficult to find support from human or animal studies for a slow-to-fast shift in contraction speed mediated by ageing in either single muscle fibres or whole muscle. Rather, the contractile properties of muscle in advanced age are understood to be defined by slowing (reviewed by Hunter et al., 1998, 2016; Larsson et al., 2018)—twitch contraction time and half-relaxation time are longer (e.g. Vandervoort and McComas, 1986), tetanic force decay is slower (e.g. Tevald et al., 2009), and the force-frequency relationship is shifted to lower frequencies (e.g. Brooks and Faulkner, 1988). As



**Fig. 7** Effect of reducing  $\text{Ca}^{2+}$  release and  $\text{Ca}^{2+}$  uptake rate, or  $\text{Ca}^{2+}$  sensitivity and  $\text{Ca}^{2+}$  uptake rate in concert. **a, d** Activator concentration and **b, e** force during a twitch and sustained 10 Hz stimulation at  $1.23 L_0$ . In **a**,  $\text{Ca}^{2+}$  release was reduced by 30%, but the rate constant of  $\text{Ca}^{2+}$  uptake was also reduced by 40% (67% increase in  $\tau_2$ ) relative

to the control condition. In **d**, the rate constant of  $\text{Ca}^{2+}$  uptake was reduced by 30% (43% increase in  $\tau_2$ ), but the  $\text{Ca}^{2+}$  sensitivity of force (*e inset*) was reduced by 0.10 pCa units relative to the control condition. **c, f** Force-frequency relationships at  $1.23 L_0$ . Force expressed relative to  $P_0$  of control condition

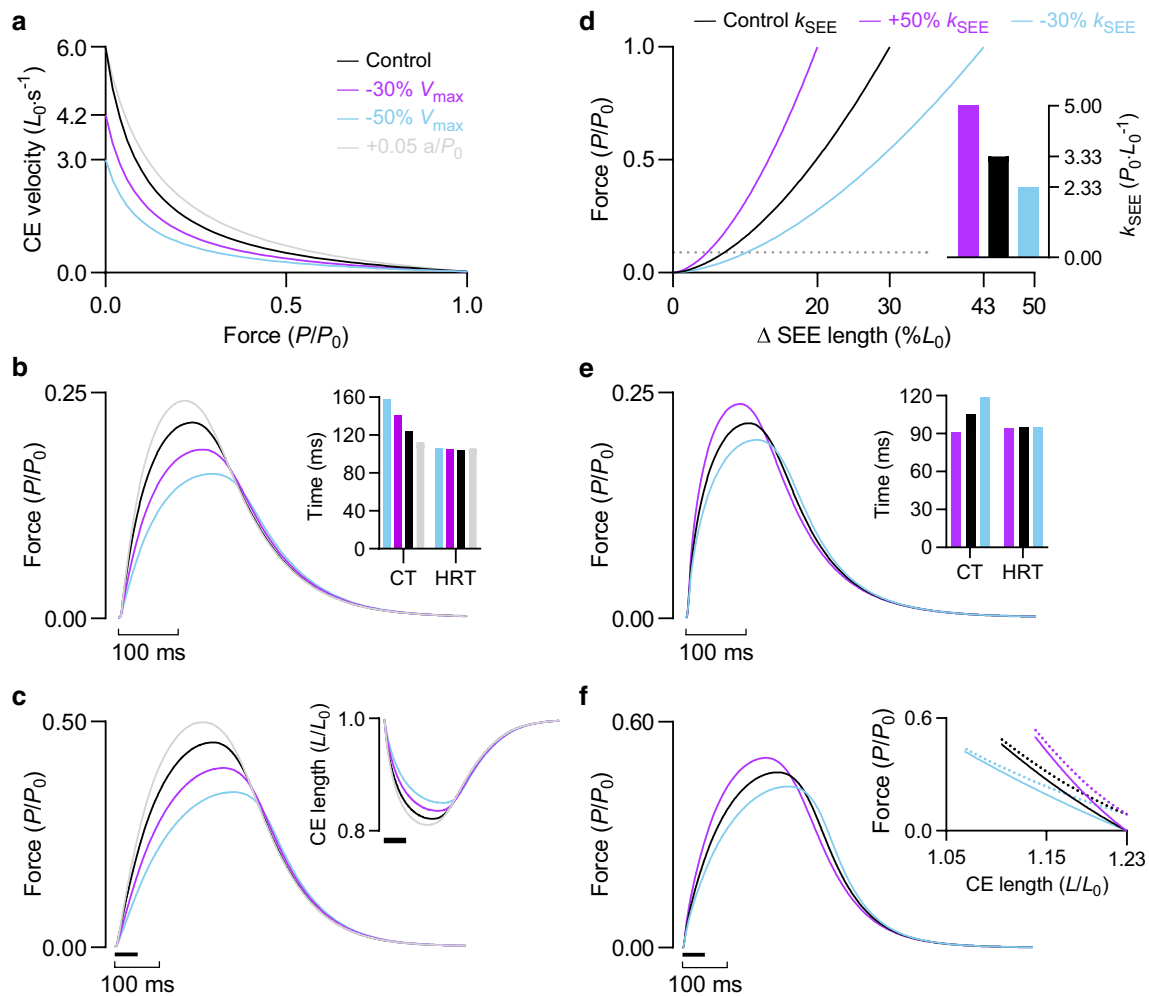
such, incorporating slower  $\text{Ca}^{2+}$  removal, or a combination of slower  $\text{Ca}^{2+}$  removal, greater  $\text{Ca}^{2+}$  sensitivity, lower cooperativity, and slower intrinsic shortening speed—to reflect an increase in type I fibre content—emulated many aspects of contractile performance frequently reported in advanced age.

#### 4.1 $\text{Ca}^{2+}$ uptake

The extent to which the rise and decay of twitch force were prolonged by slowing  $\text{Ca}^{2+}$  removal was consistent with experimental observations of slowed twitch speed in advanced age (Vandervoort and McComas 1986; Brooks and Faulkner 1988; Larsson and Salvati 1989; Hicks et al. 1991; Alway 1995; Connelly et al. 1999). In fact, the predictions were comparable to experimental data of the association between slowed SR  $\text{Ca}^{2+}$  uptake activity and twitch speed

(Narayanan et al. 1996). For the soleus muscle of old rats, a 52% deficit in SR  $\text{Ca}^{2+}$  uptake activity was accompanied by a 28 and 48% increase in twitch contraction time and half-relaxation time, respectively (Narayanan et al. 1996). When we imposed a 30% decrease in the rate constant for  $\text{Ca}^{2+}$  uptake, twitch contraction time and half-relaxation time increased by 25 and 38%. At 50%, slowing of the twitch, and the associated increase in submaximal force, far exceeded typical ageing-related slowing. To our knowledge, intracellular  $\text{Ca}^{2+}$  transients during twitches in young and old muscle have been compared in terms of amplitude but not half-width or rate of decay (González et al. 2003; Eshima et al. 2020). It would be advantageous for the model to incorporate the extent of slowing observed for the decay phase of the  $\text{Ca}^{2+}$  transient in a contracting fibre rather than the reduction





**Fig. 8** Effect of intrinsic shortening speed and SEE stiffness on force development. **a** Force–velocity relationships with varying values of  $V_{\max}$  and  $a/P_0$ .  $V_{\max}$  was reduced by 30 and 50% relative to the control condition, and  $a/P_0$  was increased by 0.05 for illustrative purposes only. **d** SEE force–length relationships with varying stiffnesses. Deformation expressed as percentage of CE  $L_0$ . Average SEE stiffness normalised to  $P_0$  and CE  $L_0$  ( $k_{\text{SEE}}$ ; inset) was reduced by 30% and increased by 50% relative to the control condition. Dotted line

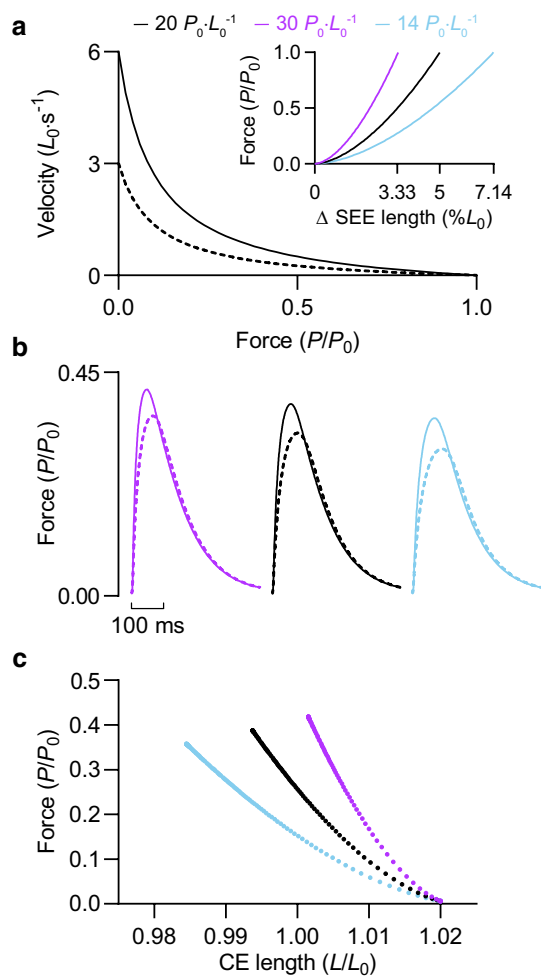
indicates passive force at optimal initial CE length of  $1.23 L_0$ . **b, e** Twitch force at an initial CE length of 1.0 and  $1.23 L_0$ , respectively. *Inset*, twitch contraction time and half-relaxation time. **c, f** Force during a brief tetanic contraction (50 ms, 100 Hz) at an initial CE length of 1.0 and  $1.23 L_0$ , respectively. *Inset*, CE length as a function of time in **c** and force in **f**; the dotted lines indicate total force. Solid bar underneath force and CE length traces at contraction onset represents duration of stimulation

in  $\text{Ca}^{2+}$  uptake rate demonstrated for an isolated SR vesicle or muscle homogenate.

Slower  $\text{Ca}^{2+}$  removal increased twitch force and, therefore, increased the ratio of twitch-to-tetanic force. Consistent with the model simulations, twitch force and twitch rise time are inversely related to the decay rate constant of the intracellular  $\text{Ca}^{2+}$  transient in single fibres (Sun and Edman 1996). Maintenance of twitch force despite a considerable deficit in maximum force or a higher ratio of twitch-to-tetanic force are commonly reported in advanced age (Carlsen and Walsh 1987; Pettigrew and Gardiner 1987; Hicks et al. 1991; van Schaik et al. 1994; Brown and Hassler 1996; Connelly et al. 1999; Klass et al. 2005; Moran et al. 2005). Slower  $\text{Ca}^{2+}$  removal, by prolonging the duration for

which the contractile apparatus is exposed to  $\text{Ca}^{2+}$  during a twitch, may partially offset or completely compensate for intrinsic processes that facilitate force loss, such as lower free  $\text{Ca}^{2+}$  concentration and lower  $\text{Ca}^{2+}$  sensitivity.

For contractions at submaximal stimulation frequencies, slower  $\text{Ca}^{2+}$  removal led to greater steady-state  $\text{Ca}^{2+}$  availability, which resulted in higher forces and a leftward shift of the force-frequency relationship. An age-related shift of the force-frequency relationship toward lower frequencies is a common observation for both human (Narici et al. 1991; Roos et al. 1999; Allman and Rice 2004; Tevald et al. 2009) and animal skeletal muscle (Larsson and Edström 1986; Brooks and Faulkner 1988; Alway 1995; González et al. 2000; Moran et al. 2005). Generally, elevated force



**Fig. 9** Effect of SEE stiffness on modulation of force development by  $V_{max}$ . **a** CE force–velocity relationships for control condition and 50% reduction in  $V_{max}$  (dashed). *Inset*, SEE force–length relationships with varying stiffnesses. Normalised stiffness ( $k_{SEE}$ ) was reduced by 30% ( $14 P_0 L_0^{-1}$ ) and increased by 50% ( $30 P_0 L_0^{-1}$ ) relative to a reference  $k_{SEE}$  of  $20 P_0 L_0^{-1}$ , which gives a normalised SEE deformation value of 5%. **b** Twitch force at an initial CE length of  $1.02 L_0$ . **c** Force as a function of instantaneous CE length during a twitch. CE length was constrained to the plateau region of the CE force–length relationship

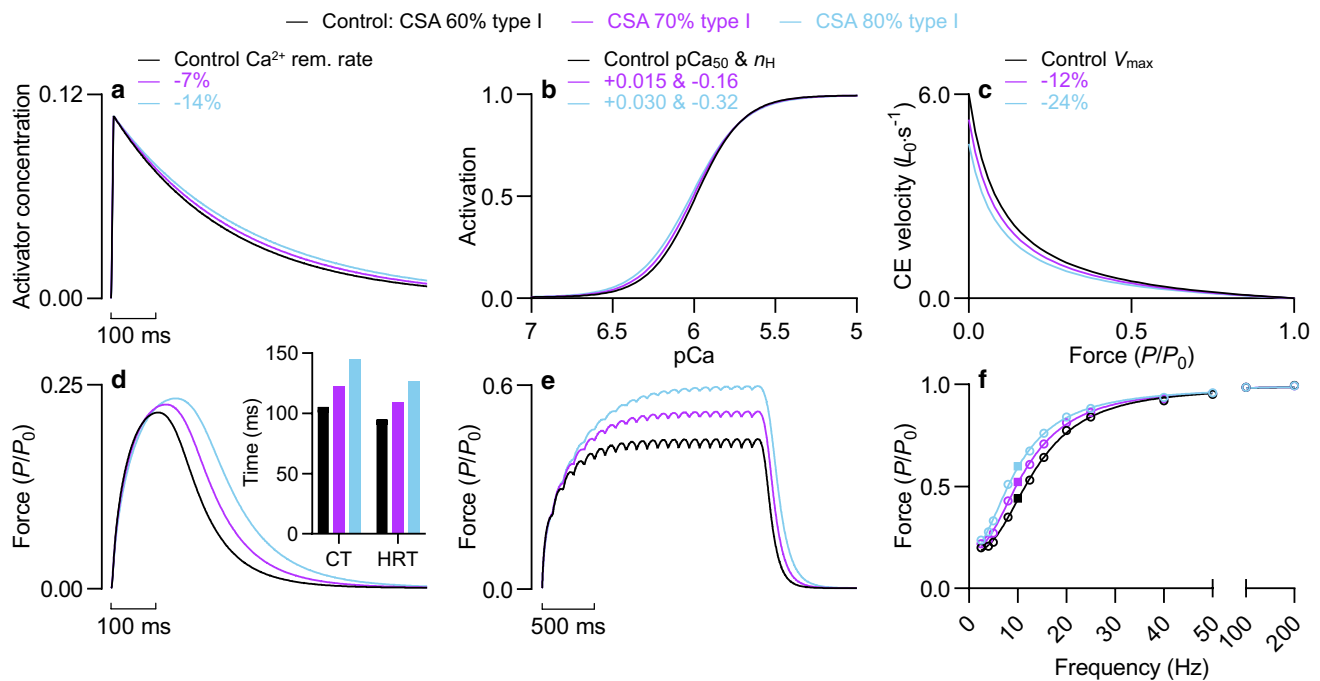
generation at submaximal frequencies is accompanied by an increase in twitch contraction time, half-relaxation time, or both. Because altered activation dynamics causing prolonged force rise and decay result in a slower fusion frequency, it is not surprising that aged muscles exhibiting normal twitch speed tend not to exhibit elevated relative force at submaximal frequencies (Walters et al. 1990; González et al. 2000; Dalton et al. 2010a; Elliott et al. 2016). Simulations incorporating a large reduction in  $Ca^{2+}$  sensitivity or moderate impairment of  $Ca^{2+}$  release in concert with slower  $Ca^{2+}$  uptake indicate that an ageing-appropriate increase in submaximal force may still be possible if these alterations coexisted. It seems less likely that a leftward shift of the

force–frequency relationship would arise if SR  $Ca^{2+}$  release was greatly impaired, especially if the impairment occurred in concert with lower  $Ca^{2+}$  sensitivity or was only balanced by a modest slowing of SR  $Ca^{2+}$  uptake.

A limited number of studies have recorded intracellular  $Ca^{2+}$  transients in contracting fibres from young and old muscles, fewer have examined a twitch or employed a range of submaximal stimulation frequencies, and none appear to have studied slow twitch fibres or examined the decay of the intracellular  $Ca^{2+}$  transient (González et al. 2003; Andersson et al. 2011; Umanskaya et al. 2014; Eshima et al. 2020). Nonetheless, these studies support the view that impaired SR  $Ca^{2+}$  leads to lower free  $Ca^{2+}$  concentrations during both submaximal and maximal contractions. Therefore, because the free  $Ca^{2+}$  concentration reflects the net effect of  $Ca^{2+}$  release and removal processes, these observations suggest that impaired SR  $Ca^{2+}$  uptake is not a universal outcome, presents at a more advanced age with respect to impaired SR  $Ca^{2+}$  release, or is only capable of minimising the deficit in free  $Ca^{2+}$  concentration caused by impaired  $Ca^{2+}$  release. According to the model predictions, for slower contraction speed to arise in the presence of a lower free  $Ca^{2+}$  concentration, there would need to be considerable involvement from an alternative mechanism. Future work should be directed at establishing whether impaired SR  $Ca^{2+}$  release and slower SR  $Ca^{2+}$  uptake coexist, how they interact, or why submaximal force in advanced age isn't disproportionately lower given the large deficit in free  $Ca^{2+}$  concentration and possible exacerbation by lower  $Ca^{2+}$  sensitivity.

## 4.2 Type I fibre fractional area

Simulating an elevated fractional area of type I fibres also produced an appropriate level of slowing. For simulations incorporating a fractional increase of 0.1 or 0.2, the relative increases in twitch contraction time and twitch half-relaxation time, and of normalised force at submaximal stimulation frequencies, were similar to the age effect reported by some studies (Fitts et al. 1984; Davies et al. 1986; Roos et al. 1999; Connelly et al. 1999). Greater age-related prolonging of the contraction time and/or half-relaxation time, a more pronounced shift in the force–frequency relationship, or both (Vandervoort and McComas 1986; Brooks and Faulkner 1988; Alway 1995; Narayanan et al. 1996; Baudry et al. 2005; McNeil et al. 2005; Dow et al. 2005), may indicate that our weighting approach was not entirely effective or that the imposed fibre type differences were too conservative. Alternatively, the greater magnitude of slowing demonstrated by these studies may implicate an additive effect or the sole involvement of slower  $Ca^{2+}$  uptake (Narayanan et al. 1996); simulations of the latter produced larger effects.



**Fig. 10** Effect of type I fibre fractional area. **a** Activator concentration during a twitch, **b** activation-pCa relationship, and **c** force-velocity relationship for varying fractions of muscle cross-sectional area (CSA) occupied by type I fibres (i.e., type I MHC content). Control values for  $Ca^{2+}$  removal (rem.) rate,  $pCa_{50}$  and  $n_H$ , and  $V_{max}$  were adjusted after back-calculation of the fibre type specific value from a defined fibre type-related difference and a weighting factor propor-

tional to the fractional area of type I fibres. The fractional area of type I fibres was increased by 0.10 and 0.20 from a control value of 0.60 (i.e., 60%). **d** Twitch force at an initial CE length of  $1.23 L_0$ . *Inset*, twitch contraction time and half-relaxation time. **e** Force during sustained 10 Hz stimulation at  $1.23 L_0$ . **f** Force-frequency relationship at  $1.23 L_0$ . Active force expressed relative to  $P_0$  of control condition. Solid squares denote the force for 10 Hz stimulation

**Table 2** Twitch properties of plantar flexors in young and older men

	Young	Older	<i>p</i> value	$\eta^2$
Contraction time (ms)	123.6 ± 8.6	154.8 ± 24.7	<0.001	0.50
Half-relaxation time (ms)	100.2 ± 17.2	129.0 ± 24.4	0.003	0.30
Torque (Nm)	29.3 ± 4.4	24.0 ± 5.2	0.011	0.22

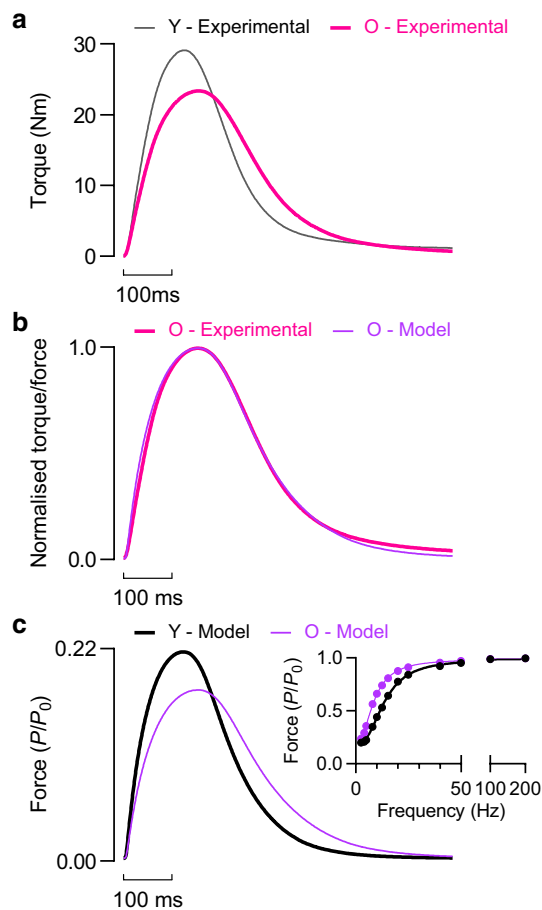
Values represent the mean ± SD

Slowed SR  $Ca^{2+}$  uptake rate has not been consistently demonstrated in advanced age, at least not for rat muscles (Fitts et al. 1984; Larsson and Salvati 1989; Narayanan et al. 1996; Thomas et al. 2010; Russ et al. 2014). Comparatively, greater evidence can be found to support an elevated fractional area of type I fibres (Coggan et al. 1992; Kadhiresan et al. 1996; Cui et al. 2008; Elliott et al. 2016), especially for the human vastus lateralis muscle (Larsson et al. 1978; Klitgaard et al. 1990a; Hunter et al. 1999; Short et al. 2005; Korhonen et al. 2006; Nilwik et al. 2013; Lamboley et al. 2015; Brocca et al. 2017; Sonjak et al. 2019; Soendenbroe et al. 2022). In some instances, the fast-to-slow shift in MHC isoform content may manifest as a reduction in MHC IIB content and an increase in MHC IIA or hybrid MHC isoforms (Hepple et al. 2004; Cui et al. 2008). Myosin isoform

composition correlates strongly with whole muscle performance (Ranatunga and Thomas 1990; Harridge et al. 1996). Slower contractile properties in advanced age have been associated with a greater fractional content of MHC I (Klitgaard et al. 1990a; Korhonen et al. 2006), demonstrated in the absence of slowed SR  $Ca^{2+}$  uptake (Larsson and Salvati 1989), and observed without slower  $Ca^{2+}$  removal being the rate-limiting process (Hunter et al. 1999). Our simulations add weight to this body of evidence—fibre-type related differences in contraction speed appear sufficient for a moderate-to-large age-related increase in type I fibre content to account for empirical observations of slowed whole muscle contraction speed.

### 4.3 $Ca^{2+}$ sensitivity and free $Ca^{2+}$ concentration

Lower  $Ca^{2+}$  sensitivity of force and excitation-SR  $Ca^{2+}$  release decoupling are thought to play a role in the age-related decline of muscle specific force (Delbono et al. 1995; González et al. 2003; Andersson et al. 2011; Lamboley et al. 2015). The model predictions suggest that the deficits in free  $Ca^{2+}$  concentration and  $Ca^{2+}$  sensitivity reported in the literature, despite dramatically reducing force at submaximal stimulation frequencies, are insufficient to appreciably lower



**Fig. 11** Model optimization to simulate time course and relative amplitude of plantar flexion twitch of old men. **a** Measured plantar flexion twitch torque of young (Y) and older (O) men. **b** Plantar flexion twitch torque of older men and simulated twitch force after parameter optimisation. Twitch contraction time and half-relaxation time for experimental and simulated data were identical following optimization (CT: 154 ms; HRT: 134.5 ms). **c** Simulated twitch force for young and old muscle. The relative deficit in twitch amplitude owing to ageing was 18% for simulated and experimental conditions. *Inset*, force-frequency relationships, where force is expressed relative to the respective  $P_0$  of each muscle

maximum tetanic force (<5%). Our findings are supported by experimental observations from studies of dantrolene exposure (Krarup 1981; Macintosh et al. 2011) and low-frequency fatigue (Westerblad et al. 1993; Chin and Allen 1996; Glass et al. 2018; Olsson et al. 2020). For example,

dantrolene partially inhibits SR  $Ca^{2+}$  release (Desmedt and Hainaut 1977), inducing moderate reductions in twitch force (27–53%) or shifting the force-frequency relationship rightward without appreciable, if any, tetanic force loss [0–6% (Krarup 1981; Macintosh et al. 2011)].

Of course, a greater deficit in maximum force would arise if the designation of thin filament activation (i.e., cross-bridge activation) during maximum tetanic stimulation was greatly overestimated in the model. This assertion would imply that maximum tetanic stimulation does not induce saturating  $Ca^{2+}$ . However, our designation seems appropriate because tetanic force plateaus with increasing stimulation frequency despite an increasing free  $Ca^{2+}$  concentration (Westerblad and Allen 1993; Glass et al. 2018, 2020). Similarly, several studies demonstrate that tetanic forces with and without caffeine—which potentiates SR  $Ca^{2+}$  release—can be virtually identical, if not equal (Lannergren and Westerblad 1991; Westerblad and Allen 1991; Glass et al. 2018; Olsson et al. 2020).

Thin filament activation is also worth considering from the perspective of voluntary muscle excitation. Motor unit discharge rates during a maximal voluntary contraction are considerably lower than the stimulation rate required for muscle maximal tetanic force (Roos et al. 1999; Dalton et al. 2010a; Kirk and Rice 2016). Asynchronous stimulation, by minimising the oscillation of fibre length against series elasticity (Sandercock 2006), can elevate force at low and intermediate stimulation frequencies without reducing the frequency required for maximal tetanic force (Rack and Westbury 1969). As such, the discrepancy could infer submaximal thin filament activation during a volitional effort. Voluntary muscle activation isn't easily quantified (Horstman 2009), and raising single fibre force from just 0.95 to 1.0  $P_0$  can require a near two-fold increase in stimulation frequency and free  $Ca^{2+}$  concentration (Glass et al. 2018). If voluntary activation were submaximal, even only slightly, maximal voluntary contraction force would be lowered dramatically by a reduction in free  $Ca^{2+}$  concentration or  $Ca^{2+}$  sensitivity.

This notion must be viewed with caution, however, because Lind and Petrofsky (1978) found that the entire force-frequency relationship could indeed be shifted to lower frequencies through asynchronous stimulation. Thus, the differences between the two modes of excitation appear

**Table 3** Comparison of optimized model parameters

	$\tau_1$ (s)	$\tau_2$ (s)	$[a]_{50}$	pCa <sub>50</sub> (pCa)	$n_H$	$V_{max}$ ( $L_0 \cdot s^{-1}$ )	$k_{SEE}$ ( $P_0 \cdot L_0^{-1}$ )	FGC
Young	0.0422	0.256	0.1025	5.99	3	6	3.33	1.0
Old (a)	0.0422	0.339	0.1025	5.99	3	4.8	3.13	0.77
Old (b)	0.0431	0.345	0.1060	5.97	3	5	2.94	0.85

FGC force-generating capacity. Multiple solutions possible for Old muscle with varying FGC

to be more complex than appreciated. Nonetheless, the force-frequency relationship of the model, where force is  $0.95 P_0$  at 50 Hz, is generally consistent with relationships established for human muscle groups in vivo (Marsh et al. 1981; Davies et al. 1982; Roos et al. 1999; Allman and Rice 2004) and animal studies of predominantly slow muscle at physiological temperatures (Ranatunga 1982; Larsson and Edström 1986).

A more significant deficit in maximum tetanic force (8%) arose when free  $\text{Ca}^{2+}$  concentration and  $\text{Ca}^{2+}$  sensitivity were lowered in concert by 50% and 0.10 pCa units, respectively. However, these modifications represent the upper limit of the age effect for  $\text{Ca}^{2+}$  sensitivity and  $\text{Ca}^{2+}$  availability reported in the literature. It's possible that moderate ageing-related reductions in  $\text{Ca}^{2+}$  availability or  $\text{Ca}^{2+}$  sensitivity may compromise tetanic specific force when  $\text{Ca}^{2+}$  sensitivity is lowered further by reducing fibre length (Stephenson and Williams 1982; Martyn and Gordon 1988; Balnave and Allen 1996), decreasing muscle temperature (Maughan et al. 1995; Debold et al. 2006; Nelson and Fitts 2014) or inducing fatigue, which also impairs SR  $\text{Ca}^{2+}$  release (Westerblad and Allen 1991, 1993).

Although there are concurrent measurements of free  $\text{Ca}^{2+}$  and force from intact single fibres (González et al. 2003), as well as combined measurements from single fibres and whole muscle (Andersson et al. 2011; Umanskaya et al. 2014), respectively, that implicate impaired SR  $\text{Ca}^{2+}$  release as an important determinant of the age-related deficit in specific force, it is unlikely that this mechanism is wholly responsible. Specific force remains lower for old compared to young intact single fibres after caffeine administration, which mitigates the age-related deficit in free  $\text{Ca}^{2+}$  concentration (González et al. 2003). Corroborating this finding are numerous studies using skinned fibres from young and old muscle (Lowe et al. 2002; D'Antona et al. 2003; Zhong et al. 2006; Yu et al. 2007; Kim and Thompson 2013; Hvid et al. 2013; Lamboley et al. 2015), some of which demonstrated a deficit in specific force of 25% or more (Thompson and Brown 1999; Frontera et al. 2000; Lowe et al. 2001; Ochala et al. 2007; Power et al. 2016; Brocca et al. 2017). These bodies of work, along with our findings, suggest that a substantial proportion of the deficit in tetanic specific force exhibited by intact single fibres, as well as whole muscle, is independent of lower tetanic free  $\text{Ca}^{2+}$  concentration. Although, as we have illustrated, the latter may exert a more considerable effect when accompanied by a moderate-to-large reduction in  $\text{Ca}^{2+}$  sensitivity.

#### 4.4 CE-SEE interaction

In addition to activation dynamics, force development is regulated by the intrinsic speed of shortening and the stiffness of the SEE being acted upon by the CE (Hill 1938;

Edman and Josephson 2007). Incorporating ageing-related reductions in  $V_{\max}$  and SEE stiffness slowed and prolonged the rise of force. During a twitch or brief tetanic contraction, both modifications also attenuated peak force. The effect on force development of a given reduction in intrinsic shortening speed depended on SEE stiffness, being more modest for low normalised SEE compliances (<8%), suggesting that force rise during a twitch of a single fibre may not be appreciably affected by a slower  $V_{\max}$ . The current work supports the involvement of slower intrinsic shortening speed and higher SEE compliance as factors contributing to prolonged and slower force rise in advanced age, although consideration may need to be given to the muscle preparation. Elevated tendon stiffness, conversely, would likely act to offset factors causing force development to be slowed or twitch force to be attenuated.

The simulations with altered SEE stiffness are generally consistent with experimental work with added compliance (Hill 1951; Brown and Matthews 1960; Bawa et al. 1976; Mayfield et al. 2016b) and where active shortening has been limited by means of a small muscle stretch (Hill 1949; Griffiths 1991; Sawicki and Roberts 2009; Mayfield et al. 2016a). Our findings also appear to be quantitatively appropriate, although there is limited information to draw upon. We found that 33 (5 vs.  $3.33 P_0 \cdot L_0^{-1}$ ) and 53% (5 vs.  $2.33 P_0 \cdot L_0^{-1}$ ) reductions in normalised SEE stiffness reduced twitch force by 16 and 29%, respectively. Cat soleus twitch force was reduced by 35–40% (Bawa et al. 1976) following the addition of a spring that we estimate reduced the in-series stiffness by ~87% [isometric twitch force: ~5 N; spring stiffness: ~1.52 N·mm<sup>-1</sup>; tendon stiffness from spindle null method at 5 N: ~10 N·mm<sup>-1</sup> (Rack and Westbury 1984)].

We found that twitch force and contraction time were similarly affected by increased SEE compliance. However, empirical measurements show that the reduction in force mediated by added compliance is more pronounced compared to the associated delay in peak force, and that the latter may not increase in proportion to the former (Hill 1951; Bawa et al. 1976; Mayfield et al. 2016b). Modest delays in peak force in response to a large amount of added compliance may relate to the effects of length or active shortening on factors such as cross-bridge kinetics (Fenwick et al. 2021),  $\text{Ca}^{2+}$  sensitivity of force (Stephenson and Williams 1982; Martyn and Gordon 1988), and force depression (Joumaa et al. 2012). With this observation in mind and the fact that imposing lower SEE stiffness prolonged the twitch contraction time by just 13%, it appears that this adaptation may not be an important determinant of twitch rise time.

Importantly, neither adaptation produced other facets of slowed contractile speed, such as slower force decay or elevated force at submaximal stimulation frequencies. Whilst the effect of added compliance on force decay is

inconsistent and only modest (Bawa et al. 1976; Mayfield et al. 2016b), slower force decay should accompany a slower intrinsic shortening speed, especially at intermediate loads (Jones et al. 2006). Ignoring a dramatic change in SEE stiffness, which would bring force–length effects and possibly length-dependent  $\text{Ca}^{2+}$  sensitivity into play, a shift in the force–frequency relationship must arise from factors affecting  $\text{Ca}^{2+}$  concentration and calcium-activated force. Greater compliance and slower intrinsic shortening may minimise force oscillations or increase the apparent degree of fusion without affecting average force.

#### 4.5 Model simulation of age effect observed for experimental twitch data

The age-related prolonging of force rise and decay during a twitch observed for the plantar flexors in this study was within the range of slowing reported by others for the same muscle group (Davies et al. 1986; Vandervoort and McComas 1986; Simoneau et al. 2005; Dalton et al. 2009, 2010b). Simulating this age-related shift in twitch contraction speed was possible with parameter adjustments that fell within the ranges of age-related adaptation obtained from empirical observations used to inform earlier simulations. Specifically, the slower, weaker twitch was achieved with reductions in force-generating capacity (23%),  $\text{Ca}^{2+}$  uptake rate (24%),  $V_{\max}$  (20%), and SEE stiffness (6%). Multiple solutions were possible, and it is likely that the slowing of twitch speed could have been emulated with parameter adjustments more consistent with an increase in type I fibre content. An increase in  $\text{Ca}^{2+}$  sensitivity and reduction in cooperativity would likely lessen the required reduction in  $\text{Ca}^{2+}$  uptake rate. We speculate because we imposed parameter limits that were consistent with the directionality of impairment reported in the literature.

### 5 Summary

Age-related reductions in  $\text{Ca}^{2+}$  sensitivity and  $\text{Ca}^{2+}$  release abbreviated the twitch and dramatically lowered force during submaximal contractions (e.g., twitch, unfused tetanic contraction) without greatly influencing maximum tetanic force, even when acting in concert (< 10%). These predictions are at odds with experimental observations of the effect of age on indices of isometric contraction speed (i.e., twitch contraction time and half-relaxation time, force–frequency relationship), and suggest that reduced  $\text{Ca}^{2+}$  sensitivity and impaired SR  $\text{Ca}^{2+}$  release may contribute only modestly to the reduction in specific force in advanced age (depending on  $\text{Ca}^{2+}$  saturation during

tetanic stimulation). Conversely, simulations that incorporated slowed  $\text{Ca}^{2+}$  removal or a greater fractional area of type I fibres prolonged the rise and decay of twitch force and shifted the force–frequency relationship leftward. These predictions are consistent with the characteristic fast-to-slow shift in contractile performance associated with ageing. Slowed and prolonged force development, and lower twitch force, also resulted from imposing a slower intrinsic shortening speed and lower SEE stiffness but occurred without a concomitant slowing of force decay or elevation of submaximal force. As such, these properties alone did not produce the characteristic slowing of contraction speed. The effect of  $V_{\max}$  depended on SEE stiffness, and empirical observations do not always support a pronounced delay in peak force from added compliance, possibly because of additional factors related to active shortening not captured in the model. Simulating the slower, weaker twitch observed experimentally for the plantar flexors of older men required significant slowing of  $\text{Ca}^{2+}$  uptake (~25%) and could be coupled with an appreciable reduction in force-generating capacity (i.e., the reduction in force-generating capacity exceeded that of the deficit in twitch force). Slowed  $\text{Ca}^{2+}$  removal, when acting in concert, negated the depressive effects of moderate and large reductions in  $\text{Ca}^{2+}$  release and  $\text{Ca}^{2+}$  sensitivity, respectively.

### 6 Conclusion

Whole muscle contractile performance in advanced age is characterised by slowed isometric contraction speed. This work provides support for the involvement of multiple mechanisms, although these adaptations do not necessarily affect the same aspects of contraction speed. As such, identifying the most important adaptations should be aided by characterising an array of isometric contractile properties in advanced age. Both slower  $\text{Ca}^{2+}$  uptake and a greater fractional area of type I fibres seem to be suitable mechanisms for explaining the slower isometric contraction speed exhibited by aged muscle. Simulations incorporating these adaptations with a degree of impairment reported in the literature generated realistic age-related changes in contractile behaviour. Ageing-appropriate adjustments to these parameters also emulated the age-related slowing of twitch speed observed experimentally. In general, the model simulations were well-supported by empirical observations. We propose that this model or similar models might be effective in determining a meaningful impairment threshold or identifying the factors contributing to altered contractile properties.

Adaptation of muscle function and structure in advanced age is inconsistent and wide-ranging, thus, careful consideration should be given to the strength of evidence implicating

the presence of a particular adaptation (e.g., fibre type, species, activity level, age). With the multifaceted nature of impairment in mind, we adjusted multiple model parameters concurrently and have illustrated the importance of considering interaction effects. Inconsistent reports regarding the effect of age on contractile performance may relate to variation in the disruption of function and structure. We believe this work underscores the utility of simple, yet physiologically-grounded and parameter rich Hill-type muscle models for studying conditions that involve a multitude of adaptations (e.g. ageing, disuse, training). Such models also hold great value in being able to predict functional performance (e.g. walking, standing from a chair) when used in musculoskeletal simulations (e.g. Song and Geyer 2018; Ong et al. 2019).

**Acknowledgements** This study benefited from the contributions of members belonging to the University of Jyväskylä Neuromuscular Research Centre, in particular, Drs Janne Avela and Marko Korhonen. We are also grateful to Dr Andrew Cresswell for insightful discussions, the participants who volunteered for this study, and two anonymous reviewers for their constructive comments.

**Author contributions** Conceptualization: D.L.M., N.J.C., and G.A.L.; Investigation: D.L.M. and N.J.C.; Software: D.L.M. and G.A.L.; Formal analysis: D.L.M.; Visualisation: D.L.M.; Writing—original draft: D.L.M.; Writing—review & editing: D.L.M., N.J.C., and G.A.L.

**Funding** No funds, grants, or other support was received to directly support this work. G.A.L. is supported by an Australian Research Council Future Fellowship (FT190100129).

**Data availability** The Hill-type muscle model developed in Simulink and a MATLAB application that can be used to run simulations are accessible as open source (under the MIT license) from GitHub [<https://github.com/dlmayfield/Muscle-Model> (Mayfield and Lichtwark 2022)]. Experimental twitch data from young and older human adults are accessible from this repository.

## Declarations

**Conflict of interests** The authors declare no competing or financial interests.

**Ethical approval** Experimental work was approved by and performed in accordance with the guidelines outlined by the human research ethical review committee of the University of Jyväskylä. Written informed consent was obtained from all participants.

**Open Access** This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit <http://creativecommons.org/licenses/by/4.0/>.

## References

- Albracht K, Arampatzis A, Baltzopoulos V (2008) Assessment of muscle volume and physiological cross-sectional area of the human triceps surae muscle in vivo. *J Biomech* 41:2211–2218. <https://doi.org/10.1016/j.jbiomech.2008.04.020>
- Allman BL, Rice CL (2004) An age-related shift in the force-frequency relationship affects quadriceps fatigability in old adults. *J Appl Physiol* 96:1026–1032. <https://doi.org/10.1152/jappphysiol.00991.2003>
- Alway SE (1995) Slowing of contractile properties in quail skeletal muscle with aging. *J Gerontol A Biol Sci Med Sci* 50A:B26–B33. <https://doi.org/10.1093/gerona/50A.1.B26>
- Andersson DC, Betzenhauser MJ, Reiken S et al (2011) Ryanodine receptor oxidation causes intracellular calcium leak and muscle weakness in aging. *Cell Metab* 14:196–207. <https://doi.org/10.1016/j.cmet.2011.05.014>
- Arampatzis A, Stafiliadis S, DeMonte G et al (2005) Strain and elongation of the human gastrocnemius tendon and aponeurosis during maximal plantarflexion effort. *J Biomech* 38:833–841. <https://doi.org/10.1016/j.jbiomech.2004.04.031>
- Asmussen G, Maréchal G (1989) Maximal shortening velocities, isomyosins and fibre types in soleus muscle of mice, rats and guinea-pigs. *J Physiol* 416:245–254. <https://doi.org/10.1113/jphysiol.1989.sp017758>
- Azizi E, Roberts TJ (2014) Geared up to stretch: pennate muscle behavior during active lengthening. *J Exp Biol* 217:376–381. <https://doi.org/10.1242/jeb.094383>
- Ballak SB, Degens H, de Haan A, Jaspers RT (2014) Aging related changes in determinants of muscle force generating capacity: a comparison of muscle aging in men and male rodents. *Ageing Res Rev* 14:43–55. <https://doi.org/10.1016/j.arr.2014.01.005>
- Balnavae CD, Allen DG (1996) The effect of muscle length on intracellular calcium and force in single fibres from mouse skeletal muscle. *J Physiol* 492:705–713. <https://doi.org/10.1113/jphysiol.1996.sp021339>
- Barclay CJ (2012) Quantifying Ca<sup>2+</sup> release and inactivation of Ca<sup>2+</sup> release in fast- and slow-twitch muscles. *J Physiol* 590:6199–6212. <https://doi.org/10.1113/jphysiol.2012.242073>
- Baudry S, Klass M, Duchateau J (2005) Postactivation potentiation influences differently the nonlinear summation of contractions in young and elderly adults. *J Appl Physiol* 98:1243–1250. <https://doi.org/10.1152/jappphysiol.00735.2004>
- Bawa P, Mannard A, Stein RB (1976) Effects of elastic loads on the contractions of cat muscles. *Biol Cybern* 22:129–137. <https://doi.org/10.1007/BF00365523>
- Baylor SM, Hollingworth S (2003) Sarcoplasmic reticulum calcium release compared in slow-twitch and fast-twitch fibres of mouse muscle. *J Physiol* 551:125–138. <https://doi.org/10.1113/jphysiol.2003.041608>
- Bennett MB, Ker RF, Imery NJ, Alexander RMN (1986) Mechanical properties of various mammalian tendons. *J Zool* 209:537–548. <https://doi.org/10.1111/j.1469-7998.1986.tb03609.x>
- Bottinelli R, Canepari M, Pellegrino MA, Reggiani C (1996) Force-velocity properties of human skeletal muscle fibres: myosin heavy chain isoform and temperature dependence. *J Physiol* 495:573–586. <https://doi.org/10.1113/jphysiol.1996.sp021617>
- Brocca L, McPhee JS, Longa E et al (2017) Structure and function of human muscle fibres and muscle proteome in physically active older men. *J Physiol* 595:4823–4844. <https://doi.org/10.1113/JP274148>
- Brooks SV, Faulkner JA (1988) Contractile properties of skeletal muscles from young, adult and aged mice. *J Physiol* 404:71–82. <https://doi.org/10.1113/jphysiol.1988.sp017279>

- Brooks SV, Faulkner JA (1994) Isometric, shortening, and lengthening contractions of muscle fiber segments from adult and old mice. *Am J Physiol Cell Physiol* 267:C507–C513. <https://doi.org/10.1152/ajpcell.1994.267.2.C507>
- Brown, M.C., Matthews, P.B., 1960. An investigation into the possible existence of polyneuronal innervation of individual skeletal muscle fibres in certain hind-limb muscles of the cat. *J. Physiol.* 151, 436–457. <https://doi.org/10.1113/jphysiol.1960.sp006450>
- Brown M, Hasser EM (1996) Complexity of age-related change in skeletal muscle. *J Gerontol A Biol Sci Med Sci* 51:B117–B123. <https://doi.org/10.1093/gerona/51a.2.b117>
- Calderón JC, Bolaños P, Caputo C (2010) Myosin heavy chain isoform composition and Ca<sup>2+</sup> transients in fibres from enzymatically dissociated murine soleus and extensor digitorum longus muscles. *J Physiol* 588:267–279. <https://doi.org/10.1113/jphysiol.2009.180893>
- Caputo C, Bolaños P, Gonzalez A (2004) Inactivation of Ca<sup>2+</sup> transients in amphibian and mammalian muscle fibres. *J Muscle Res Cell Motil* 25:315–328. <https://doi.org/10.1007/s10974-004-4071-z>
- Carlsen RC, Walsh DA (1987) Decrease in force potentiation and appearance of  $\alpha$ -adrenergic mediated contracture in aging rat skeletal muscle. *Pflügers Arch* 408:224–230. <https://doi.org/10.1007/BF02181463>
- Carroll SL, Klein MG, Schneider MF (1997) Decay of calcium transients after electrical stimulation in rat fast- and slow-twitch skeletal muscle fibres. *J Physiol* 501:573–588. <https://doi.org/10.1111/j.1469-7793.1997.573bm.x>
- Carroll CC, Dickinson JM, Haus JM et al (2008) Influence of aging on the in vivo properties of human patellar tendon. *J Appl Physiol* 105:1907–1915. <https://doi.org/10.1152/jappphysiol.00059.2008>
- Chin ER, Allen DG (1996) The role of elevations in intracellular [Ca<sup>2+</sup>] in the development of low frequency fatigue in mouse single muscle fibres. *J Physiol* 491:813–824. <https://doi.org/10.1113/jphysiol.1996.sp021259>
- Clafflin DR, Faulkner JA (1989) The force-velocity relationship at high shortening velocities in the soleus muscle of the rat. *J Physiol* 411:627–637. <https://doi.org/10.1113/jphysiol.1989.sp017595>
- Clafflin DR, Larkin LM, Cederna PS et al (2011) Effects of high- and low-velocity resistance training on the contractile properties of skeletal muscle fibers from young and older humans. *J Appl Physiol* 111:1021–1030. <https://doi.org/10.1152/jappphysiol.01119.2010>
- Coggan AR, Spina RJ, King DS et al (1992) Histochemical and enzymatic comparison of the gastrocnemius muscle of young and elderly men and women. *J Gerontol* 47:71–76. <https://doi.org/10.1093/geronj/47.3.B71>
- Connelly DM, Rice CL, Roos MR, Vandervoort AA (1999) Motor unit firing rates and contractile properties in tibialis anterior of young and old men. *J Appl Physiol* 87:843–852. <https://doi.org/10.1152/jappl.1999.87.2.843>
- Couppé C, Suetta C, Kongsgaard M et al (2012) The effects of immobilization on the mechanical properties of the patellar tendon in younger and older men. *Clin Biomech* 27:949–954. <https://doi.org/10.1016/j.clinbiomech.2012.06.003>
- Crouzier M, Lacourpaille L, Nordez A et al (2018) Neuromechanical coupling within the human triceps surae and its consequence on individual force-sharing strategies. *J Exp Biol* 221:jeb187260. <https://doi.org/10.1242/jeb.187260>
- Csapo R, Malis V, Hodgson J, Sinha S (2014) Age-related greater achilles tendon compliance is not associated with larger plantar flexor muscle fascicle strains in senior women. *J Appl Physiol* 116:961–969. <https://doi.org/10.1152/jappphysiol.01337.2013>
- Cui L, Ju Y, Ding L et al (2008) Arteriolar and venular capillary distribution in skeletal muscles of old rats. *J Gerontol A Biol Sci Med Sci* 63:928–935. <https://doi.org/10.1093/gerona/63.9.928>
- Cui L, Maas H, Perreault EJ, Sandercock TG (2009) In situ estimation of tendon material properties: differences between muscles of the feline hindlimb. *J Biomech* 42:679–685. <https://doi.org/10.1016/j.jbiomech.2009.01.022>
- Curtin NA, Gardner-Medwin AR, Woledge RC (1998) Predictions of the time course of force and power output by dogfish white muscle fibres during brief tetani. *J Exp Biol* 201:103–114
- D'Antona G, Pellegrino MA, Adami R et al (2003) The effect of ageing and immobilization on structure and function of human skeletal muscle fibres. *J Physiol* 552:499–511. <https://doi.org/10.1113/jphysiol.2003.046276>
- D'Antona G, Pellegrino MA, Carlizzi CN, Bottinelli R (2007) Deterioration of contractile properties of muscle fibres in elderly subjects is modulated by the level of physical activity. *Eur J Appl Physiol* 100:603–611. <https://doi.org/10.1007/s00421-007-0402-2>
- Dalton BH, Harwood B, Davidson AW, Rice CL (2009) Triceps surae contractile properties and firing rates in the soleus of young and old men. *J Appl Physiol* 107:1781–1788. <https://doi.org/10.1152/jappphysiol.00464.2009>
- Dalton BH, Jakobi JM, Allman BL, Rice CL (2010a) Differential age-related changes in motor unit properties between elbow flexors and extensors. *Acta Physiol* 200:45–55. <https://doi.org/10.1111/j.1748-1716.2010.02100.x>
- Dalton BH, Power GA, Vandervoort AA, Rice CL (2010b) Power loss is greater in old men than young men during fast plantar flexion contractions. *J Appl Physiol* 109:1441–1447. <https://doi.org/10.1152/jappphysiol.00335.2010>
- Danieli-Betto D, Betto R, Midrio M (1990) Calcium sensitivity and myofibrillar protein isoforms of rat skinned skeletal muscle fibres. *Pflugers Arch* 417:303–308. <https://doi.org/10.1007/BF00370996>
- Danos N, Holt NC, Sawicki GS, Azizi E (2016) Modeling age-related changes in muscle-tendon dynamics during cyclical contractions in the rat gastrocnemius. *J Appl Physiol* 121:1004–1012. <https://doi.org/10.1152/jappphysiol.00396.2016>
- Davies CTM, Mecrow IK, White MJ (1982) Contractile properties of the human triceps surae with some observations on the effects of temperature and exercise. *Eur J Appl Physiol Occup Physiol* 49:255–269. <https://doi.org/10.1007/BF02334074>
- Davies CTM, Thomas DO, White MJ (1986) Mechanical properties of young and elderly human muscle. *Acta Med Scand* 220:219–226. <https://doi.org/10.1111/j.0954-6820.1986.tb08954.x>
- Debold EP, Romatowski J, Fitts RH (2006) The depressive effect of Pi on the force-pCa relationship in skinned single muscle fibers is temperature dependent. *Am J Physiol Cell Physiol* 290:C1041–C1050. <https://doi.org/10.1152/ajpcell.00342.2005>
- Degens H, Yu F, Li X, Larsson L (1998) Effects of age and gender on shortening velocity and myosin isoforms in single rat muscle fibres. *Acta Physiol Scand* 163:33–40. <https://doi.org/10.1046/j.1365-201x.1998.00329.x>
- Delbono O, O'Rourke KS, Ettinger WH (1995) Excitation-calcium release uncoupling in aged single human skeletal muscle fibers. *J Membr Biol* 148:211–222. <https://doi.org/10.1007/BF00235039>
- Desmedt JE, Hainaut K (1977) Inhibition of the intracellular release of calcium by dantrolene in barnacle giant muscle fibres. *J Physiol* 265:565–585. <https://doi.org/10.1113/jphysiol.1977.sp011731>
- Dow DE, Dennis RG, Faulkner JA (2005) Electrical stimulation attenuates denervation and age-related atrophy in extensor digitorum longus muscles of old rats. *J Gerontol A Biol Sci Med Sci* 60:416–424. <https://doi.org/10.1093/gerona/60.4.416>
- Eddinger TJ, Cassens RG, Moss RL (1986) Mechanical and histochemical characterization of skeletal muscles from senescent rats. *Am*



- J Physiol Cell Physiol 251:C421–C430. <https://doi.org/10.1152/ajpcell.1986.251.3.C421>
- Edman KAP, Josephson RK (2007) Determinants of force rise time during isometric contraction of frog muscle fibres. *J Physiol* 580:1007–1019. <https://doi.org/10.1113/jphysiol.2006.119982>
- Edström L, Nyström BO (1969) Histochemical types and sizes of fibres in normal human muscles. *Acta Neurol Scand* 45:257–269. <https://doi.org/10.1111/j.1600-0404.1969.tb01238.x>
- Elliott JE, Omar TS, Mantilla CB, Sieck GC (2016) Diaphragm muscle sarcopenia in Fischer 344 and Brown Norway rats. *Exp Physiol* 101:883–894. <https://doi.org/10.1113/EP085703>
- Eriksen CS, Henkel C, Svensson RB et al (2018) Lower tendon stiffness in very old compared with old individuals is unaffected by short-term resistance training of skeletal muscle. *J Appl Physiol* 125:205–214. <https://doi.org/10.1152/jappphysiol.00028.2018>
- Eshima H, Tamura Y, Kakehi S et al (2020) A chronic high-fat diet exacerbates contractile dysfunction with impaired intracellular Ca<sup>2+</sup> release capacity in the skeletal muscle of aged mice. *J Appl Physiol* 128:1153–1162. <https://doi.org/10.1152/jappphysiol.00530.2019>
- Fenwick AJ, Lin DC, Tanner BCW (2021) Myosin cross-bridge kinetics slow at longer muscle lengths during isometric contractions in intact soleus from mice. *Proc R Soc B* 288:20202895. <https://doi.org/10.1098/rspb.2020.2895>
- Fink RH, Stephenson DG, Williams DA (1986) Calcium and strontium activation of single skinned muscle fibres of normal and dystrophic mice. *J Physiol* 373:513–525. <https://doi.org/10.1113/jphysiol.1986.sp016060>
- Fink RH, Stephenson DG, Williams DA (1990) Physiological properties of skinned fibres from normal and dystrophic (Duchenne) human muscle activated by Ca<sup>2+</sup> and Sr<sup>2+</sup>. *J Physiol* 420:337–353. <https://doi.org/10.1113/jphysiol.1990.sp017916>
- Fitts RH, Troup JP, Witzmann FA, Holloszy JO (1984) The effect of ageing and exercise on skeletal muscle function. *Mech Ageing Dev* 27:161–172. [https://doi.org/10.1016/0047-6374\(84\)90041-1](https://doi.org/10.1016/0047-6374(84)90041-1)
- Fodor J, Al-Gaadi D, Czirják T et al (2020) Improved calcium homeostasis and force by selenium treatment and training in aged mouse skeletal muscle. *Sci Rep* 10:1707. <https://doi.org/10.1038/s41598-020-58500-x>
- Frontera WR, Suh D, Krivickas LS et al (2000) Skeletal muscle fiber quality in older men and women. *Am J Physiol Cell Physiol* 279:C611–C618. <https://doi.org/10.1152/ajpcell.2000.279.3.C611>
- Gao Y, Kostrominova TY, Faulkner JA, Wineman AS (2008) Age-related changes in the mechanical properties of the epimysium in skeletal muscles of rats. *J Biomech* 41:465–469. <https://doi.org/10.1016/j.jbiomech.2007.09.021>
- Gardetto PR, Schluter JM, Fitts RH (1989) Contractile function of single muscle fibers after hindlimb suspension. *J Appl Physiol* 66:2739–2749. <https://doi.org/10.1152/jappphysiol.1989.66.6.2739>
- Gilliver SF, Degens H, Rittweger J et al (2009) Variation in the determinants of power of chemically skinned human muscle fibres. *Exp Physiol* 94:1070–1078. <https://doi.org/10.1113/expphysiol.2009.048314>
- Glass LD, Cheng AJ, MacIntosh BR (2018) Role of Ca<sup>2+</sup> in changing active force during intermittent submaximal stimulation in intact, single mouse muscle fibers. *Pflügers Arch - Eur J Physiol* 470:1243–1254. <https://doi.org/10.1007/s00424-018-2143-y>
- Glass LD, Cheng AJ, MacIntosh BR (2020) Calcium sensitivity during staircase with sequential incompletely fused contractions. *J Muscle Res Cell Motil* 42:59–65. <https://doi.org/10.1007/s10974-019-09572-4>
- González E, Messi ML, Delbono O (2000) The specific force of single intact extensor digitorum longus and soleus mouse muscle fibers declines with aging. *J Membr Biol* 178:175–183. <https://doi.org/10.1007/s002320010025>
- González E, Messi ML, Zheng Z, Delbono O (2003) Insulin-like growth factor-1 prevents age-related decrease in specific force and intracellular Ca<sup>2+</sup> in single intact muscle fibres from transgenic mice. *J Physiol* 552:833–844. <https://doi.org/10.1113/jphysiol.2003.048165>
- Gordon AM, Huxley AF, Julian FJ (1966) The variation in isometric tension with sarcomere length in vertebrate muscle fibres. *J Physiol* 184:170–192. <https://doi.org/10.1113/jphysiol.1966.sp007909>
- Green HJ, Daub B, Houston ME et al (1981) Human vastus lateralis and gastrocnemius muscles: a comparative histochemical and biochemical analysis. *J Neurol Sci* 52:201–210. [https://doi.org/10.1016/0022-510X\(81\)90005-8](https://doi.org/10.1016/0022-510X(81)90005-8)
- Gregorevic P, Plant DR, Stupka N, Lynch GS (2004) Changes in contractile activation characteristics of rat fast and slow skeletal muscle fibres during regeneration. *J Physiol* 558:549–560. <https://doi.org/10.1113/jphysiol.2004.066217>
- Gries KJ, Minchev K, Raue U et al (2019) Single-muscle fiber contractile properties in lifelong aerobic exercising women. *J Appl Physiol* 127:1710–1719. <https://doi.org/10.1152/jappphysiol.00459.2019>
- Griffiths, R.I., 1991. Shortening of muscle fibres during stretch of the active cat medial gastrocnemius muscle: the role of tendon compliance. *J. Physiol.* 436, 219–236. <https://doi.org/10.1113/jphysiol.1991.sp018547>
- Grosicki GJ, Gries KJ, Minchev K et al (2021) Single muscle fibre contractile characteristics with lifelong endurance exercise. *J Physiol* 599:3549–3565. <https://doi.org/10.1113/JP281666>
- Harridge SDR, Bottinelli R, Canepari M et al (1996) Whole-muscle and single-fibre contractile properties and myosin heavy chain isoforms in humans. *Pflügers Arch* 432:913–920. <https://doi.org/10.1007/s004240050215>
- Harridge SDR, Bottinelli R, Canepari M et al (1998) Sprint training, in vitro and in vivo muscle function, and myosin heavy chain expression. *J Appl Physiol* 84:442–449. <https://doi.org/10.1152/jappphysiol.1998.84.2.442>
- Hasson CJ, Caldwell GE (2012) Effects of age on mechanical properties of dorsiflexor and plantarflexor muscles. *Ann Biomed Eng* 40:1088–1101. <https://doi.org/10.1007/s10439-011-0481-4>
- Hatcher DD, Luff AR (1987) Force-velocity properties of fatigue-resistant units in cat fast-twitch muscle after fatigue. *J Appl Physiol* 63:1511–1518. <https://doi.org/10.1152/jappphysiol.1987.63.4.1511>
- Hauraix H, Nordez A, Guilhem G et al (2015) In vivo maximal fascicle-shortening velocity during plantar flexion in humans. *J Appl Physiol* 119:1262–1271. <https://doi.org/10.1152/jappphysiol.00542.2015>
- Hellam DC, Podolsky RJ (1969) Force measurements in skinned muscle fibres. *J Physiol* 200:807–819. <https://doi.org/10.1113/jphysiol.1969.sp008723>
- Hepple RT, Hagen JL, Krause DJ, Baker DJ (2004) Skeletal muscle aging in F344BN F1-hybrid rats: II. improved contractile economy in senescence helps compensate for reduced ATP-generating capacity. *J Gerontol A Biol Sci Med Sci* 59:1111–1119. <https://doi.org/10.1093/gerona/59.11.1111>
- Hessel AL, Raiteri BJ, Marsh MJ, Hahn D (2021) Rightward shift of optimal fascicle length with decreasing voluntary activity level in the soleus and lateral gastrocnemius muscles. *J Exp Biol* 224:jeb235614. <https://doi.org/10.1242/jeb.235614>
- Hicks AL, Cupido CM, Martin J, Dent J (1991) Twitch potentiation during fatiguing exercise in the elderly: the effects of training. *Eur J Appl Physiol Occup Physiol* 63:278–281. <https://doi.org/10.1007/BF00233862>
- Hill AV (1938) The heat of shortening and the dynamic constants of muscle. *Proc R Soc B* 126:136–195. <https://doi.org/10.1098/rspb.1938.0050>

- Hill AV (1949) The abrupt transition from rest to activity in muscle. *Proc. R. Soc. B* 136, 399–420. <https://doi.org/10.1098/rspb.1949.0033>
- Hill AV (1951) The effect of series compliance on the tension developed in a muscle twitch. *Proc R Soc B* 138:325–329. <https://doi.org/10.1098/rspb.1951.0025>
- Hill C, James RS, Cox VM et al (2020) Age-related changes in isolated mouse skeletal muscle function are dependent on sex, muscle, and contractility mode. *Am J Physiol Regul Integr Comp Physiol* 319:R296–R314. <https://doi.org/10.1152/ajpregu.00073.2020>
- Holt NC, Wakeling JM, Biewener AA (2014) The effect of fast and slow motor unit activation on whole-muscle mechanical performance: The size principle may not pose a mechanical paradox. *Proc R Soc B* 281:2–7. <https://doi.org/10.1098/rspb.2014.0002>
- Holt NC, Danos N, Roberts TJ, Azizi E (2016) Stuck in gear: age-related loss of variable gearing in skeletal muscle. *J Exp Biol* 219:998–1003. <https://doi.org/10.1242/jeb.133009>
- Höök P, Sriramoju V, Larsson L (2001) Effects of aging on actin sliding speed on myosin from single skeletal muscle cells of mice, rats, and humans. *Am J Physiol Cell Physiol* 280:782–788
- Horstman AM (2009) Comments on point: counterpoint: the interpolated twitch does/does not provide a valid measure of the voluntary activation of muscle. *J Appl Physiol* 107:359–366. <https://doi.org/10.1152/jappphysiol.00362.2009>
- Hunter S, White M, Thompson M (1998) Techniques to evaluate elderly human muscle function: a physiological basis. *J Gerontol A Biol Sci Med Sci* 53:B204–B216. <https://doi.org/10.1093/gerona/53a.3.b204>
- Hunter SK, Thompson MW, Ruell PA et al (1999) Human skeletal sarcoplasmic reticulum Ca<sup>2+</sup> uptake and muscle function with aging and strength training. *J Appl Physiol* 86:1858–1865. <https://doi.org/10.1152/jappl.1999.86.6.1858>
- Hunter SK, Pereira XHM, Keenan KG (2016) The aging neuromuscular system and motor performance. *J Appl Physiol* 121:982–995. <https://doi.org/10.1152/jappphysiol.00475.2016>
- Hvid LG, Ørtenblad N, Aagaard P et al (2011) Effects of ageing on single muscle fibre contractile function following short-term immobilisation. *J Physiol* 589:4745–4757. <https://doi.org/10.1113/jphysiol.2011.215434>
- Hvid LG, Suetta C, Aagaard P et al (2013) Four days of muscle disuse impairs single fiber contractile function in young and old healthy men. *Exp Gerontol* 48:154–161. <https://doi.org/10.1016/j.exger.2012.11.005>
- Hvid LG, Brocca L, Ørtenblad N et al (2017) Myosin content of single muscle fibers following short-term disuse and active recovery in young and old healthy men. *Exp Gerontol* 87:100–107. <https://doi.org/10.1016/j.exger.2016.10.009>
- Jiménez-Moreno R, Wang ZM, Gerring RC, Delbono O (2008) Sarcoplasmic reticulum Ca<sup>2+</sup> release declines in muscle fibers from aging mice. *Biophys J* 94:3178–3188. <https://doi.org/10.1529/biophysj.107.118786>
- Jones DA, de Ruiter CJ, de Haan A (2006) Change in contractile properties of human muscle in relationship to the loss of power and slowing of relaxation seen with fatigue. *J Physiol* 576:913–922. <https://doi.org/10.1113/jphysiol.2006.116343>
- Joumaa V, MacIntosh BR, Herzog W (2012) New insights into force depression in skeletal muscle. *J Exp Biol* 215:2135–2140. <https://doi.org/10.1242/jeb.060863>
- Kadhiresan VA, Hassett CA, Faulkner JA (1996) Properties of single motor units in medial gastrocnemius muscles of adult and old rats. *J Physiol* 493:543–552. <https://doi.org/10.1113/jphysiol.1996.sp021402>
- Karamanidis K, Arampatzis A (2005) Mechanical and morphological properties of different muscle-tendon units in the lower extremity and running mechanics: effect of aging and physical activity. *J Exp Biol* 208:3907–3923. <https://doi.org/10.1242/jeb.01830>
- Karamanidis K, Arampatzis A (2006) Mechanical and morphological properties of human quadriceps femoris and triceps surae muscle-tendon unit in relation to aging and running. *J Biomech* 39:406–417. <https://doi.org/10.1016/j.jbiomech.2004.12.017>
- Karamanidis K, Stafilidis S, DeMonte G et al (2005) Inevitable joint angular rotation affects muscle architecture during isometric contraction. *J Electromyogr Kinesiol* 15:608–616. <https://doi.org/10.1016/j.jelekin.2005.02.001>
- Kim J-H, Thompson LV (2013) Inactivity, age, and exercise: single-muscle fiber power generation. *J Appl Physiol* 114:90–98. <https://doi.org/10.1152/jappphysiol.00525.2012>
- Kirk EA, Rice CL (2016) Contractile function and motor unit firing rates of the human hamstrings. *J Neurophysiol* 117:243–250. <https://doi.org/10.1152/jn.00620.2016>
- Klass M, Baudry S, Duchateau J (2005) Aging does not affect voluntary activation of the ankle dorsiflexors during isometric, concentric, and eccentric contractions. *J Appl Physiol* 99:31–38. <https://doi.org/10.1152/jappphysiol.01426.2004>
- Klitgaard H, Marc R, Brunet A et al (1989) Contractile properties of old rat muscles: effect of increased use. *J Appl Physiol* 67:1401–1408. <https://doi.org/10.1152/jappl.1989.67.4.1401>
- Klitgaard H, Mantoni M, Schiaffino S et al (1990a) Function, morphology and protein expression of ageing skeletal muscle: a cross-sectional study of elderly men with different training backgrounds. *Acta Physiol Scand* 140:41–54. <https://doi.org/10.1111/j.1748-1716.1990.tb08974.x>
- Klitgaard H, Zhou M, Schiaffino S et al (1990b) Ageing alters the myosin heavy chain composition of single fibres from human skeletal muscle. *Acta Physiol Scand* 140:55–62. <https://doi.org/10.1111/j.1748-1716.1990.tb08975.x>
- Korhonen MT, Cristea A, Alén M et al (2006) Aging, muscle fiber type, and contractile function in sprint-trained athletes. *J Appl Physiol* 101:906–917. <https://doi.org/10.1152/jappphysiol.00299.2006>
- Krarup C (1981) The effect of dantrolene on the enhancement and diminution of tension evoked by staircase and by tetanus in rat muscle. *J Physiol* 311:389–400. <https://doi.org/10.1113/jphysiol.1981.sp013591>
- Krivickas LS, Suh D, Wilkins J et al (2001) Age- and gender-related differences in maximum shortening velocity of skeletal muscle fibers. *Am J Phys Med Rehabil* 80(6):447–455
- LaCroix AS, Duenwald-Kuehl SE, Brickson S et al (2013) Effect of age and exercise on the viscoelastic properties of rat tail tendon. *Ann Biomed Eng* 41:1120–1128. <https://doi.org/10.1007/s10439-013-0796-4>
- Lambole CR, Wyckelsma VL, Dutka TL et al (2015) Contractile properties and sarcoplasmic reticulum calcium content in type I and type II skeletal muscle fibres in active aged humans. *J Physiol* 593:2499–2514. <https://doi.org/10.1113/JP270179>
- Lambole CR, Rouffet DM, Dutka TL et al (2020) Effects of high-intensity intermittent exercise on the contractile properties of human type I and type II skeletal muscle fibers. *J Appl Physiol* 128:1207–1216. <https://doi.org/10.1152/jappphysiol.00014.2020>
- Lannergren J, Westerblad H (1991) Force decline due to fatigue and intracellular acidification in isolated fibres from mouse skeletal muscle. *J Physiol* 434:307–322. <https://doi.org/10.1113/jphysiol.1991.sp018471>
- Larsson L, Edström L (1986) Effects of age on enzyme-histochemical fibre spectra and contractile properties of fast- and slow-twitch skeletal muscles in the rat. *J Neurol Sci* 76:69–89. [https://doi.org/10.1016/0022-510X\(86\)90143-7](https://doi.org/10.1016/0022-510X(86)90143-7)
- Larsson L, Moss RL (1993) Maximum velocity of shortening in relation to myosin isoform composition in single fibres from human

- skeletal muscles. *J Physiol* 472:595–614. <https://doi.org/10.1113/jphysiol.1993.sp019964>
- Larsson L, Salvati G (1989) Effects of age on calcium transport activity of sarcoplasmic reticulum in fast- and slow-twitch rat muscle fibres. *J Physiol* 419:253–264. <https://doi.org/10.1113/jphysiol.1989.sp017872>
- Larsson L, Sjödin B, Karlsson J et al (1978) Histochemical and biochemical changes in human skeletal muscle with age in sedentary males, age 22–65 years. *Acta Physiol Scand* 103:31–39. <https://doi.org/10.1111/j.1748-1716.1978.tb06187.x>
- Larsson L, Li X, Frontera WR (1997) Effects of aging on shortening velocity and myosin isoform composition in single human skeletal muscle cells. *Am J Physiol Cell Physiol* 272:C638–C649. <https://doi.org/10.1152/ajpcell.1997.272.2.C638>
- Larsson L, Degens H, Li M et al (2018) Sarcopenia: aging-related loss of muscle mass and function. *Physiol Rev* 99:427–511. <https://doi.org/10.1152/physrev.00061.2017>
- Laszewski-Williams B, Ruff RL, Gordon AM (1989) Influence of fiber type and muscle source on Ca<sup>2+</sup> sensitivity of rat fibers. *Am J Physiol Cell Physiol* 256:C420–C427. <https://doi.org/10.1152/ajpcell.1989.256.2.C420>
- Leahy TP, Nuss CA, Evans MK et al (2022) Achilles tendon ruptures in middle-aged rats heal poorly compared with those in young and old rats. *Am J Sports Med* 50:170–181. <https://doi.org/10.1177/03635465211055476>
- Lichtwark GA, Barclay CJ (2010) The influence of tendon compliance on muscle power output and efficiency during cyclic contractions. *J Exp Biol* 213:707–714. <https://doi.org/10.1242/jeb.038026>
- Lichtwark GA, Wilson AM (2005a) A modified Hill muscle model that predicts muscle power output and efficiency during sinusoidal length changes. *J Exp Biol* 208:2831–2843. <https://doi.org/10.1242/jeb.01709>
- Lichtwark GA, Wilson AM (2005b) Effects of series elasticity and activation conditions on muscle power output and efficiency. *J Exp Biol* 208:2845–2853. <https://doi.org/10.1242/jeb.01710>
- Lieber RL, Leonard ME, Brown CG, Trestik CL (1991) Frog semitendinosus tendon load-strain and stress-strain properties during passive loading. *Am J Physiol Cell Physiol* 261:C86–92. <https://doi.org/10.1152/ajpcell.1991.261.1.C86>
- Lind AR, Petrofsky JS (1978) Isometric tension from rotary stimulation of fast and slow cat muscles. *Muscle Nerve* 1:213–218. <https://doi.org/10.1002/mus.880010306>
- Liu Y, Kranias EG, Schneider MF (1997) Regulation of Ca<sup>2+</sup> handling by phosphorylation status in mouse fast- and slow-twitch skeletal muscle fibers. *Am J Physiol Cell Physiol* 273:C1915–C1924. <https://doi.org/10.1152/ajpcell.1997.273.6.C1915>
- Loren GJ, Lieber RL (1995) Tendon biomechanical properties enhance human wrist muscle specialization. *J Biomech* 28:791–799. [https://doi.org/10.1016/0021-9290\(94\)00137-S](https://doi.org/10.1016/0021-9290(94)00137-S)
- Lowe DA, Surer JT, Thomas DD et al (2001) Electron paramagnetic resonance reveals age-related myosin structural changes in rat skeletal muscle fibers. *Am J Physiol Cell Physiol* 280:540–547. <https://doi.org/10.1152/ajpcell.2001.280.3.C540>
- Lowe DA, Thomas DD, Thompson LV (2002) Force generation, but not myosin ATPase activity, declines with age in rat muscle fibers. *Am J Physiol Cell Physiol* 283:C187–C192. <https://doi.org/10.1152/ajpcell.00008.2002>
- Luden N, Minchev K, Hayes E et al (2008) Human vastus lateralis and soleus muscles display divergent cellular contractile properties. *Am J Physiol Regul Integr Comp Physiol* 295:1593–1598. <https://doi.org/10.1152/ajpregu.90564.2008>
- Luff AR (1981) Dynamic properties of the inferior rectus, extensor digitorum longus, diaphragm and soleus muscles of the mouse. *J Physiol* 313:161–171. <https://doi.org/10.1113/jphysiol.1981.sp013656>
- Lynch GS, Stephenson DG, Williams DA (1991) Endurance exercise effects on the contractile properties of single, skinned skeletal muscle fibres of young rats. *Pflügers Arch* 418:161–167. <https://doi.org/10.1007/BF00370466>
- Lynch GS, Stephenson DG, Williams DA (1995) Analysis of Ca<sup>2+</sup> and Sr<sup>2+</sup> activation characteristics in skinned muscle fibre preparations with different proportions of myofibrillar isoforms. *J Muscle Res Cell Motil* 16:65–78. <https://doi.org/10.1007/BF00125311>
- Macintosh BR, Glumpak JJ, MacNaughton MB, Rassier DE (2011) Pattern of summation with fatigue and inhibition of calcium release in rat muscle. *Muscle Nerve* 44:410–417. <https://doi.org/10.1002/mus.22073>
- Marsh E, Sale D, McComas AJ, Quinlan J (1981) Influence of joint position on ankle dorsiflexion in humans. *J Appl Physiol* 51:160–167. <https://doi.org/10.1152/jappl.1981.51.1.160>
- Martyn DA, Gordon AM (1988) Length and myofilament spacing-dependent changes in calcium sensitivity of skeletal fibres: effects of pH and ionic strength. *J Muscle Res Cell Motil* 9:428–445. <https://doi.org/10.1007/BF01774069>
- Martyn DA, Gordon AM (2001) Influence of length on force and activation-dependent changes in troponin C structure in skinned cardiac and fast skeletal muscle. *Biophys J* 80:2798–2808. [https://doi.org/10.1016/S0006-3495\(01\)76247-9](https://doi.org/10.1016/S0006-3495(01)76247-9)
- Maughan DW, Molloy JE, Brotto MA, Godt RE (1995) Approximating the isometric force-calcium relation of intact frog muscle using skinned fibers. *Biophys J* 69:1484–1490. [https://doi.org/10.1016/S0006-3495\(95\)80019-6](https://doi.org/10.1016/S0006-3495(95)80019-6)
- Mayfield DL, Lichtwark GA, Cronin NJ et al (2015) Doublet potentiation in the triceps surae is limited by series compliance and dynamic fascicle behavior. *J Appl Physiol*. <https://doi.org/10.1152/jappphysiol.00403.2015>
- Mayfield DL, Cresswell AG, Lichtwark GA (2016a) Effects of series elastic compliance on muscle force summation and the rate of force rise. *J Exp Biol* 219:3261–3270. <https://doi.org/10.1242/jeb.142604>
- Mayfield DL, Launikonis BS, Cresswell AG, Lichtwark GA (2016b) Additional in-series compliance reduces muscle force summation and alters the time course of force relaxation during fixed-end contractions. *J Exp Biol* 219:3587–3596. <https://doi.org/10.1242/jeb.143123>
- Mayfield DL, Lichtwark GA (2022) Muscle-Model. <https://doi.org/10.5281/ZENODO.6423696>
- Mazara N, Zwambag DP, Noonan AM et al (2021) Rate of force development is Ca<sup>2+</sup>-dependent and influenced by Ca<sup>2+</sup>-sensitivity in human single muscle fibres from older adults. *Exp Gerontol* 150:111348. <https://doi.org/10.1016/j.exger.2021.111348>
- McCrum C, Leow P, Epro G et al (2018) Alterations in leg extensor muscle-tendon unit biomechanical properties with ageing and mechanical loading. *Front Physiol* 9:1–7. <https://doi.org/10.3389/fphys.2018.00150>
- McNeil CJ, Doherty TJ, Stashuk DW, Rice CL (2005) Motor unit number estimates in the tibialis anterior muscle of young, old, and very old men. *Muscle Nerve* 31:461–467. <https://doi.org/10.1002/mus.20276>
- McNeil CJ, Vandervoort AA, Rice CL (2007) Peripheral impairments cause a progressive age-related loss of strength and velocity-dependent power in the dorsiflexors. *J Appl Physiol* 102:1962–1968. <https://doi.org/10.1152/jappphysiol.01166.2006>
- Miller MS, Bedrin NG, Callahan DM et al (2013) Age-related slowing of myosin actin cross-bridge kinetics is sex specific and predicts decrements in whole skeletal muscle performance in humans. *J Appl Physiol* 115:1004–1014. <https://doi.org/10.1152/jappphysiol.00563.2013>
- Monti E, Reggiani C, Franchi MV et al (2021) Neuromuscular junction instability and altered intracellular calcium handling as early

- determinants of force loss during unloading in humans. *J Physiol* 599:3037–3061. <https://doi.org/10.1113/JP281365>
- Moo EK, Leonard TR, Herzog W (2020) The sarcomere force-length relationship in an intact muscle-tendon unit. *J Exp Biol* 223:215020. <https://doi.org/10.1242/jeb.215020>
- Moran AL, Warren GL, Lowe DA (2005) Soleus and EDL muscle contractility across the lifespan of female C57BL/6 mice. *Exp Gerontol* 40:966–975. <https://doi.org/10.1016/j.exger.2005.09.005>
- Morse CI, Thom JM, Birch KM, Narici MV (2005) Changes in triceps surae muscle architecture with sarcopenia. *Acta Physiol Scand* 183:291–298. <https://doi.org/10.1111/j.1365-201X.2004.01404.x>
- Muramatsu T, Muraoka T, Takeshita D et al (2001) Mechanical properties of tendon and aponeurosis of human gastrocnemius muscle in vivo. *J Appl Physiol* 90:1671–1678
- Nakagawa Y, Hayashi K, Yamamoto N, Nagashima K (1996) Age-related changes in biomechanical properties of the Achilles tendon in rabbits. *Eur J Appl Physiol Occup Physiol* 73:7–10. <https://doi.org/10.1007/BF00262803>
- Narayanan N, Jones DL, Xu A, Yu JC (1996) Effects of aging on sarcoplasmic reticulum function and contraction duration in skeletal muscles of the rat. *Am J Physiol Cell Physiol* 271:C1032–C1040. <https://doi.org/10.1152/ajpcell.1996.271.4.C1032>
- Narici MV, Bordini M, Cerretelli P (1991) Effect of aging on human adductor pollicis muscle function. *J Appl Physiol* 71:1277–1281. <https://doi.org/10.1152/jappl.1991.71.4.1277>
- Narici MV, Maganaris CN, Reeves ND, Capodaglio P (2003) Effect of aging on human muscle architecture. *J Appl Physiol* 95:2229–2234. <https://doi.org/10.1152/jappphysiol.00433.2003>
- Nelson CR, Fitts RH (2014) Effects of low cell pH and elevated inorganic phosphate on the pCa-force relationship in single muscle fibers at near-physiological temperatures. *Am J Physiol Cell Physiol* 306:C670–C678. <https://doi.org/10.1152/ajpcell.00347.2013>
- Nilwik R, Snijders T, Leenders M et al (2013) The decline in skeletal muscle mass with aging is mainly attributed to a reduction in type II muscle fiber size. *Exp Gerontol* 48:492–498. <https://doi.org/10.1016/j.exger.2013.02.012>
- Ochala J, Frontera WR, Dorer DJ et al (2007) Single skeletal muscle fiber elastic and contractile characteristics in young and older men. *J Gerontol A Biol Sci Med Sci* 62:375–381. <https://doi.org/10.1093/gerona/62.4.375>
- Olsson K, Cheng AJ, Al-Ameri M et al (2020) Impaired sarcoplasmic reticulum Ca<sup>2+</sup> release is the major cause of fatigue-induced force loss in intact single fibres from human intercostal muscle. *J Physiol* 598:773–787. <https://doi.org/10.1113/JP279090>
- Onambele GL, Narici MV, Maganaris CN (2006) Calf muscle-tendon properties and postural balance in old age. *J Appl Physiol* 100:2048–2056. <https://doi.org/10.1152/jappphysiol.01442.2005>
- Ong CF, Geijtenbeek T, Hicks JL, Delp SL (2019) Predicting gait adaptations due to ankle plantarflexor muscle weakness and contracture using physics-based musculoskeletal simulations. *PLoS Comput Biol* 15:e1006993. <https://doi.org/10.1371/journal.pcbi.1006993>
- Otten E (1987) A myocybernetic model of the jaw system of the rat. *J Neurosci Methods* 21:287–302. [https://doi.org/10.1016/0165-0270\(87\)90123-3](https://doi.org/10.1016/0165-0270(87)90123-3)
- Pardes AM, Beach ZM, Raja H et al (2017) Aging leads to inferior Achilles tendon mechanics and altered ankle function in rodents. *J Biomech* 60:30–38. <https://doi.org/10.1016/j.jbiomech.2017.06.008>
- Pettigrew FP, Gardiner PF (1987) Changes in rat plantaris motor unit profiles with advanced age. *Mech Ageing Dev* 40:243–259. [https://doi.org/10.1016/0047-6374\(87\)90022-4](https://doi.org/10.1016/0047-6374(87)90022-4)
- Plant DR, Lynch GS (2001) Rigor force responses of permeabilized fibres from fast and slow skeletal muscles of aged rats. *Clin Exp Pharmacol Physiol* 28:779–781. <https://doi.org/10.1046/j.1440-1681.2001.03521.x>
- Power GA, Minozzo FC, Spendiff S et al (2016) Reduction in single muscle fiber rate of force development with aging is not attenuated in world class older masters athletes. *Am J Physiol Cell Physiol* 310:C318–C327. <https://doi.org/10.1152/ajpcell.00289.2015>
- Rack PM, Westbury DR (1969) The effects of length and stimulus rate on tension in the isometric cat soleus muscle. *J Physiol* 204:443–460. <https://doi.org/10.1113/jphysiol.1969.sp008923>
- Rack PM, Westbury DR, (1984) Elastic properties of the cat soleus tendon and their functional importance. *J Physiol* 347:479–495. <https://doi.org/10.1113/jphysiol.1984.sp015077>
- Ranatunga KW (1982) Temperature-dependence of shortening velocity and rate of isometric tension development in rat skeletal muscle. *J Physiol* 329:465–483. <https://doi.org/10.1113/jphysiol.1982.sp014314>
- Ranatunga KW (1998) Temperature dependence of mechanical power output in mammalian (rat) skeletal muscle. *Exp Physiol* 83:371–376. <https://doi.org/10.1113/expphysiol.1998.sp004120>
- Ranatunga KW, Thomas PE (1990) Correlation between shortening velocity, force-velocity relation and histochemical fibre-type composition in rat muscles. *J Muscle Res Cell Motil* 11:240–250. <https://doi.org/10.1007/BF01843577>
- Reid KF, Doros G, Clark DJ et al (2012) Muscle power failure in mobility-limited older adults: preserved single fiber function despite lower whole muscle size, quality and rate of neuromuscular activation. *Eur J Appl Physiol* 112:2289–2301. <https://doi.org/10.1007/s00421-011-2200-0>
- Rice KM, Linderman JK, Kinnard RS, Blough ER (2005) The Fischer 344/NNiaHSd X Brown Norway/BiNia is a better model of sarcopenia than the Fischer 344/NNiaHSd: a comparative analysis of muscle mass and contractile properties in aging male rat models. *Biogerontology* 6:335–343. <https://doi.org/10.1007/s10522-005-4808-0>
- Roberts TJ (2002) The integrated function of muscles and tendons during locomotion. *Comp Biochem Physiol - A Mol Integr Physiol* 133:1087–1099. [https://doi.org/10.1016/S1095-6433\(02\)00244-1](https://doi.org/10.1016/S1095-6433(02)00244-1)
- Roos MR, Rice CL, Connelly DM, Vandervoort AA (1999) Quadriceps muscle strength, contractile properties, and motor unit firing rates in young and old men. *Muscle Nerve* 22:1094–1103. [https://doi.org/10.1002/\(SICI\)1097-4598\(199908\)22:8<3c1094::AID-MUS14%3e3.0.CO;2-G](https://doi.org/10.1002/(SICI)1097-4598(199908)22:8<3c1094::AID-MUS14%3e3.0.CO;2-G)
- Rubenson J, Pires NJ, Loi HO et al (2012) On the ascent: the soleus operating length is conserved to the ascending limb of the force-length curve across gait mechanics in humans. *J Exp Biol* 215:3539–3551. <https://doi.org/10.1242/jeb.070466>
- Ruff RL (1989) Calcium sensitivity of fast- and slow-twitch human muscle fibers. *Muscle Nerve* 12:32–37. <https://doi.org/10.1002/mus.880120107>
- Ruff RL, Whittlesey D (1991) Ca-, Sr-tension relationships and contraction velocities of human muscle fibers. *Muscle Nerve* 14:1219–1226. <https://doi.org/10.1002/mus.880141214>
- Russ DW, Grandy JS, Toma K, Ward CW (2011) Ageing, but not yet senescent, rats exhibit reduced muscle quality and sarcoplasmic reticulum function. *Acta Physiol* 201:391–403. <https://doi.org/10.1111/j.1748-1716.2010.02191.x>
- Russ DW, Wills AM, Boyd IM, Krause J (2014) Weakness, SR function and stress in gastrocnemius muscles of aged male rats. *Exp Gerontol* 50:40–44. <https://doi.org/10.1016/j.exger.2013.11.018>
- Sale D, Quinlan J, Marsh E et al (1982) Influence of joint position on ankle plantarflexion in humans. *J Appl Physiol Respir Environ Exerc Physiol* 52:1636–1642

- Sandercock TG (2006) Extra force from asynchronous stimulation of cat soleus muscle results from minimizing the stretch of the common elastic elements. *J Neurophysiol* 96:1401–1405. <https://doi.org/10.1152/jn.01304.2005>
- Sawicki GS, Roberts TJ (2009) Isometric force production requires asymmetric muscle-tendon length trajectory, in: 33rd Annual Meeting of American Society of Biomechanics. State College, PA: ASB.
- Seow CY (2013) Hill's equation of muscle performance and its hidden insight on molecular mechanisms. *J Gen Physiol* 142:561–573. <https://doi.org/10.1085/jgp.201311107>
- Short KR, Vittone JL, Bigelow ML et al (2005) Changes in myosin heavy chain mRNA and protein expression in human skeletal muscle with age and endurance exercise training. *J Appl Physiol* 99:95–102. <https://doi.org/10.1152/jappphysiol.00129.2005>
- Simoneau E, Martin A, Van Hoecke J (2005) Muscular performances at the ankle joint in young and elderly men. *J Gerontol A Biol Sci Med Sci* 60:439–447. <https://doi.org/10.1093/gerona/60.4.439>
- Soendenbroe C, Dahl CL, Meulengracht C et al (2022) Preserved stem cell content and innervation profile of elderly human skeletal muscle with lifelong recreational exercise. *J Physiol* 600:1969–1989. <https://doi.org/10.1113/JP282677>
- Song S, Geyer H (2018) Predictive neuromechanical simulations indicate why walking performance declines with ageing. *J Physiol* 596:1199–1210. <https://doi.org/10.1113/JP275166>
- Sonjak V, Jacob K, Morais JA et al (2019) Fidelity of muscle fibre reinnervation modulates ageing muscle impact in elderly women. *J Physiol* 597:5009–5023. <https://doi.org/10.1113/JP278261>
- Stenroth L, Peltonen J, Cronin NJ et al (2012) Age-related differences in Achilles tendon properties and triceps surae muscle architecture in vivo. *J Appl Physiol* 113:1537–1544. <https://doi.org/10.1152/jappphysiol.00782.2012>
- Stephenson DG, Williams DA (1981) Calcium-activated force responses in fast- and slow-twitch skinned muscle fibres of the rat at different temperatures. *J Physiol* 317:281–302. <https://doi.org/10.1113/jphysiol.1981.sp013825>
- Stephenson DG, Williams DA (1982) Effects of sarcomere length on the force—pCa relation in fast- and slow-twitch skinned muscle fibres from the rat. *J Physiol* 333:637–653. <https://doi.org/10.1113/jphysiol.1982.sp014473>
- Straight CR, Ades PA, Toth MJ, Miller MS (2018) Age-related reduction in single muscle fiber calcium sensitivity is associated with decreased muscle power in men and women. *Exp Gerontol* 102:84–92. <https://doi.org/10.1016/j.exger.2017.12.007>
- Sullivan VK, Powers SK, Criswell DS et al (1995) Myosin heavy chain composition in young and old rat skeletal muscle: effects of endurance exercise. *J Appl Physiol* 78:2115–2120. <https://doi.org/10.1152/jappl.1995.78.6.2115>
- Sun YB, Lou F, Edman KAP (1996) The relationship between the intracellular Ca<sup>2+</sup> transient and the isometric twitch force in frog muscle fibres. *Exp Physiol* 81:711–724. <https://doi.org/10.1113/expphysiol.1996.sp003971>
- Sundberg CW, Hunter SK, Trappe SW et al (2018) Effects of elevated H<sup>+</sup> and Pi on the contractile mechanics of skeletal muscle fibres from young and old men: implications for muscle fatigue in humans. *J Physiol* 596:3993–4015. <https://doi.org/10.1113/JP276018>
- Svensson RB, Heinemeier KM, Couppé C et al (2016) Effect of aging and exercise on the tendon. *J Appl Physiol* 121:1353–1362. <https://doi.org/10.1152/jappphysiol.00328.2016>
- Teigen LE, Sundberg CW, Kelly LJ et al (2020) Ca<sup>2+</sup> dependency of limb muscle fiber contractile mechanics in young and older adults. *Am J Physiol Cell Physiol* 318:C1238–C1251. <https://doi.org/10.1152/ajpcell.00575.2019>
- Tevald MA, Foulis SA, Lanza IR, Kent-Braun JA (2009) Lower energy cost of skeletal muscle contractions in older humans. *Am J Physiol Regul Integr Comp Physiol* 298:R729–R739. <https://doi.org/10.1152/ajpregu.00713.2009>
- Thelen DG (2003) Adjustment of muscle mechanics model parameters to simulate dynamic contractions in older adults. *J Biomech Eng* 125:70–77. <https://doi.org/10.1115/1.1531112>
- Thom JM, Morse CI, Birch KM, Narici MV (2007) Influence of muscle architecture on the torque and power-velocity characteristics of young and elderly men. *Eur J Appl Physiol* 100:613–619. <https://doi.org/10.1007/s00421-007-0481-0>
- Thomas MM, Vigna C, Betik AC et al (2010) Initiating treadmill training in late middle age offers modest adaptations in Ca<sup>2+</sup> handling but enhances oxidative damage in senescent rat skeletal muscle. *Am J Physiol Regul Integr Comp Physiol* 298:R1269–R1278. <https://doi.org/10.1152/ajpregu.00663.2009>
- Thompson LV, Brown M (1999) Age-related changes in contractile properties of single skeletal fibers from the soleus muscle. *J Appl Physiol* 86:881–886. <https://doi.org/10.1152/jappphysiol.1999.86.3.881>
- Thompson LV, Johnson SA, Shoeman JA (1998) Single soleus muscle fiber function after hindlimb unweighting in adult and aged rats. *J Appl Physiol* 84:1937–1942. <https://doi.org/10.1152/jappl.1998.84.6.1937>
- Trappe S, Gallagher P, Harber M et al (2003) Single muscle fibre contractile properties in young and old men and women. *J Physiol* 552:47–58. <https://doi.org/10.1113/jphysiol.2003.044966>
- Trestik CL, Lieber RL (1993) Relationship between achilles tendon mechanical properties and gastrocnemius muscle function. *J Biomech Eng* 115:225–230. <https://doi.org/10.1115/1.2895479>
- Umanskaya A, Santulli G, Xie W et al (2014) Genetically enhancing mitochondrial antioxidant activity improves muscle function in aging. *Proc Natl Acad Sci USA* 111:15250–15255. <https://doi.org/10.1073/pnas.1412754111>
- van Schaik CS, Hicks AL, McCartney N (1994) An evaluation of the length-tension relationship in elderly human ankle dorsiflexors. *J Gerontol* 49:B121–B127. <https://doi.org/10.1093/geronj/49.3.b121>
- Vandervoort AA, McComas AJ (1986) Contractile changes in opposing muscles of the human ankle joint with aging. *J Appl Physiol* 61:361–367. <https://doi.org/10.1152/jappphysiol.1986.61.1.361>
- Wakeling JM, Johnston IA (1999) Predicting muscle force generation during fast-starts for the common carp *Cyprinus carpio*. *J Comp Physiol B* 169:391–401. <https://doi.org/10.1007/s003600050235>
- Wakeling JM, Lee SSM, Arnold AS et al (2012) A muscle's force depends on the recruitment patterns of its fibers. *Ann Biomed Eng* 40:1708–1720. <https://doi.org/10.1007/s10439-012-0531-6>
- Walker JS, Li X, Buttrick PM (2010) Analysing force–pCa curves. *J Muscle Res Cell Motil* 31:59–69. <https://doi.org/10.1007/s10974-010-9208-7>
- Walters TJ, Sweeney HL, Farrar RP (1990) Aging does not affect contractile properties of type IIB FDL muscle in Fischer 344 rats. *Am J Physiol Cell Physiol* 258:C1031–C1035. <https://doi.org/10.1152/ajpcell.1990.258.6.C1031>
- Wang ZM, Messi ML, Delbono O (2000) L-type Ca<sup>2+</sup> channel charge movement and intracellular Ca<sup>2+</sup> in skeletal muscle fibers from aging mice. *Biophys J* 78:1947–1954. [https://doi.org/10.1016/S0006-3495\(00\)76742-7](https://doi.org/10.1016/S0006-3495(00)76742-7)
- Wang Z-M, Messi ML, Delbono O (2002) Sustained overexpression of IGF-1 prevents age-dependent decrease in charge movement and intracellular Ca<sup>2+</sup> in mouse skeletal muscle. *Biophys J* 82:1338–1344. [https://doi.org/10.1016/S0006-3495\(02\)75489-1](https://doi.org/10.1016/S0006-3495(02)75489-1)
- Westerblad H, Allen DG (1991) Changes of myoplasmic calcium concentration during fatigue in single mouse muscle fibers. *J Gen Physiol* 98:615–635. <https://doi.org/10.1085/jgp.98.3.615>
- Westerblad H, Allen DG (1993) The contribution of [Ca<sup>2+</sup>]<sub>i</sub> to the slowing of relaxation in fatigued single fibres from mouse skeletal muscle. *J Physiol* 468:729–740. <https://doi.org/10.1113/jphysiol.1993.sp019797>

- Westerblad H, Duty S, Allen DG (1993) Intracellular calcium concentration during low-frequency fatigue in isolated single fibers of mouse skeletal muscle. *J Appl Physiol* 75:382–388. <https://doi.org/10.1152/jappl.1993.75.1.382>
- Widrick JJ, Trappe SW, Costill DL, Fitts RH (1996) Force-velocity and force-power properties of single muscle fibers from elite master runners and sedentary men. *Am J Physiol* 271:C676–C683. <https://doi.org/10.1152/ajpcell.1996.271.2.C676>
- Widrick JJ, Norenberg KM, Romatowski JG et al (1998) Force-velocity-power and force-pCa relationships of human soleus fibers after 17 days of bed rest. *J Appl Physiol* 85:1949–1956. <https://doi.org/10.1152/jappl.1998.85.5.1949>
- Widrick JJ, Stelzer JE, Shoepe TC, Garner DP (2002) Functional properties of human muscle fibers after short-term resistance exercise training. *Am J Physiol Regul Integr Comp Physiol* 283:R408–R416. <https://doi.org/10.1152/ajpregu.00120.2002>
- Williams T, Bowtell G, Curtin NA (1998) Predicting force generation by lamprey muscle during applied sinusoidal movement using a simple dynamic model. *J Exp Biol* 201:869–875. <https://doi.org/10.1242/jeb.201.6.869>
- Winters TM, Takahashi M, Lieber RL, Ward SR (2011) Whole muscle length-tension relationships are accurately modeled as scaled sarcomeres in rabbit hindlimb muscles. *J Biomech* 44:109–115. <https://doi.org/10.1016/j.jbiomech.2010.08.033>
- Wisdom KM, Delp SL, Kuhl E (2015) Use it or lose it: multiscale skeletal muscle adaptation to mechanical stimuli. *Biomech Model Mechanobiol* 14:195–215. <https://doi.org/10.1007/s10237-014-0607-3>
- Wood LK, Brooks SV (2016) Ten weeks of treadmill running decreases stiffness and increases collagen turnover in tendons of old mice. *J Orthop Res* 34:346–353. <https://doi.org/10.1002/jor.22824>
- Wood LK, Arruda EM, Brooks SV (2011) Regional stiffening with aging in tibialis anterior tendons of mice occurs independent of changes in collagen fibril morphology. *J Appl Physiol* 111:999–1006. <https://doi.org/10.1152/jappphysiol.00460.2011>
- Xu H, Lamb GD, Murphy RM (2017) Changes in contractile and metabolic parameters of skeletal muscle as rats age from 3 to 12 months. *J Muscle Res Cell Motil* 38:405–420. <https://doi.org/10.1007/s10974-017-9484-6>
- Yu F, Hedström M, Cristea A et al (2007) Effects of ageing and gender on contractile properties in human skeletal muscle and single fibres. *Acta Physiol* 190:229–241. <https://doi.org/10.1111/j.1748-1716.2007.01699.x>
- Zajac FE (1989) Muscle and tendon: properties, models, scaling, and application to biomechanics and motor control. *Crit Rev Biomed Eng* 17:359–411
- Zhong S, Lowe DA, Thompson LV (2006) Effects of hindlimb unweighting and aging on rat semimembranosus muscle and myosin. *J Appl Physiol* 101:873–880. <https://doi.org/10.1152/jappphysiol.00526.2005>
- Zuurbier CJ, Everard AJ, van der Wees P, Huijing PA (1994) Length-force characteristics of the aponeurosis in the passive and active muscle condition and in the isolated condition. *J Biomech* 27:445–453. [https://doi.org/10.1016/0021-9290\(94\)90020-5](https://doi.org/10.1016/0021-9290(94)90020-5)

**Publisher's Note** Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.