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# **The estimation of critical angle in climbing as a measure of maximal metabolic steady state**

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## **Abstract**

**Purpose.** Sport climbing is a technical, self-paced sport and the workload is highly variable and mainly localized to the forearm flexors. It has not proved effective to control intensity using measures typical of other sports, such as gas exchange thresholds, heart rate or blood lactate. Therefore, the purposes of the study were to 1) determine the possibility of applying the mathematical model of critical power to the estimation of a critical angle (CA) as a measure of maximal metabolic steady state in climbing, and 2) to compare this intensity with the muscle oxygenation breakpoint (MOB) determined during an exhaustive climbing task.

**Materials and Methods.** Twenty-seven sport climbers undertook three to five exhaustive ascents on a motorized treadwall at differing angles to estimate CA, and one exhaustive climbing test with a progressive increase in angle to determine MOB, assessed using near infrared spectroscopy.

**Results.** Model fit for estimated CA was very high ( $R^2=0.99$ ;  $SEE=1.1^\circ$ ). The mean peak-angle during incremental test was  $-17\pm 5^\circ$  and CA from exhaustive trials was found at  $-2.5\pm 3.8^\circ$ . Nine climbers performing the ascent  $2^\circ$  under CA were able to sustain the task for 20 min with perceived exertion at  $12.1\pm 1.9$  (RPE). However, climbing  $2^\circ$  above CA led to task failure after  $15.9\pm 3.0$  min with  $RPE=16.4\pm 1.9$ . When MOB was plotted against estimated CA, good agreement was stated ( $ICC=0.80$ ,  $SEM=1.5^\circ$ ).

**Conclusion.** Climbers, coaches and researchers may use a predefined route with three to five different wall angles to estimate CA as an analogue of critical power to determine a maximal metabolic steady state in climbing. Moreover, a climbing test with progressive increases in wall angle using MOB also appears to provide a valid estimate of CA.

**Keywords:** sport climbing, muscle oxygenation, near infrared spectroscopy, critical power, oxygen kinetics, finger flexors

## **Introduction**

Sport climbing is a technical, self-paced sport and the workload is highly variable and mainly localized to the forearm flexors. Both maximal finger flexor strength and endurance have been found to be strong predictors of climbing ability (Fryer et al. 2018; Michailov et al. 2018), with lead climbers demonstrating greater endurance and boulderers maximal strength and power (Fanchini et al. 2013; Fryer et al. 2017). The recent debut of competition format climbing at the Tokyo Olympics 2020 (the combined performance of speed, lead, bouldering) has highlighted the divergent requirements of different disciplines, forcing athletes to pay special attention to concurrent training of strength/power and endurance to improve their combined performance.

An ascent of a climbing route is rarely “standardized” with numerous changes in wall angle and speed, as well as the types, shapes, orientation and distributions of handholds, and opportunities for partial recovery during an ascent. As such, performance requires the interaction of multiple technical, tactical, neuromuscular and metabolic factors (Orth et al. 2016; Saul et al. 2019). However, during training climbers still seek to stimulate these factors in an isolated manner using intensity-controlled devices such as hangboards, campus boards, and climbing walls of different angles (Levernier and Laffaye 2019; Stien et al. 2021; Medernach et al. 2015). Diagnostic and training methods for climbing specific strength have been well described in the literature (Levernier and Laffaye 2019; Philippe et al. 2019; Lopez-Rivera and Gonzalez-Badillo 2019; López-Rivera and González-Badillo 2012; Stien et al. 2021; Michailov et al. 2018; Medernach et al. 2015). In contrast, research on adaptations from endurance training is scarce (Lopez-Rivera and Gonzalez-Badillo 2019). Endurance training in climbing requires systemic and localized adaptations (Thompson et al. 2014; Fryer et al. 2018) and ensuring appropriate intensity of exercise, particularly for the finger flexors, is challenging. Indeed, it has been shown that intensity control during climbing using measures typical from other sports,

such as gas exchange thresholds, heart rate and blood lactate are not effective (Baláš et al. 2021; Limonta et al. 2018; Schöffl et al. 2006).

Only two studies have proposed a test to determine functional aerobic metabolic capacity in climbers using intermittent isometric handgrip contractions at differing intensities (Giles et al. 2019; Giles et al. 2020). The authors calculated critical force (CF), the force analogue of critical power (CP) to determine maximal metabolic steady state for climbing specific handgrip exercise (Poole et al. 2016; Jones et al. 2019). The CF tests proposed by Giles et al. (2020; 2019) are useful, however they may only be applied to isolated forearm models and so far have only been tested for one specific hold size and work-recovery ratio, and therefore, their practical use are currently limited.

Applying the CP concept (Poole et al. 2016), and its mathematical models to a whole-body climbing test may offer a potential solution to determine maximal metabolic steady state in climbing. Although climbing intensity has often been increased by elevating the velocity of an ascent (España-Romero et al. 2009; Rosponi et al. 2012; Booth et al. 1999), it has recently been shown that local muscle oxygen utilisation may not be altered during faster climbing; however, it does rise with steeper wall angles (Gajdošík et al. 2021). Small incremental changes in climbing angle offer a valid means of altering the intensity of a climb while maintaining its multifaceted characteristics (Noé et al. 2001; Baláš et al. 2014). Combined with measures of climbing time to exhaustion, it may be possible to calculate a ‘critical angle’ (CA) analogous to CP (Poole et al. 2016). The CA should correspond to a metabolic transitional zone below which climbing does not induce task failure for a prolonged period, and above which fatigue occurs in a finite predictable period. Moreover, with an increased angle, more pronounced finger flexor contractions stimulate mitochondrial respiration and higher intramuscular pressure restricts capillary blood flow and, thus, muscle oxygen delivery (Fryer et al. 2013; Gajdošík et al. 2021). Recently, muscle oxygenation breakpoints (MOB) have been measured locally using

near infra-red spectroscopy (NIRS) during an incremental climbing task (Baláš et al. 2021). These MOB's were suggested to represent an intensity around localized CP, however, they have not been associated with any systemic metabolic thresholds indicators and, as such validation of such a MOB is needed.

Knowledge of CA in climbers may help coaches and researchers to set climbing intensities on routes with pre-set hold configurations (specific type, shape, orientation and distribution of handholds and footholds) in the heavy or severe exercise domains during training; something which would be extremely advantageous for training, yet is currently not possible. Moreover, the use of NIRS may allow for the instantaneous control of intensity during an ascent. We hypothesise, that if a climbing CA exists, the difference in intensity will also elicit changes in muscle oxygen dynamics. Moreover, climbing slightly over CA will lead to a finite and predictable time to failure and climbing under the CA will not induce exhaustion for a prolonged, indefinite, period. Consequently, the purposes of the study were to 1) determine the possibility of applying the mathematical model of CP to the estimation of a CA as a measure of maximal metabolic steady state in climbing, and 2) to compare this intensity with the MOB determined during an exhaustive climbing task.

## **Materials and methods**

### *Participants*

Twenty-seven sport climbers of an intermediate to advanced level [11-25 International Rock-Climbing Association (IRCRA) scale; 6a-8b French/Sport scale] volunteered (19 males: age  $30.3 \pm 8.5$  years, body mass  $70.5 \pm 7.1$  kg, height  $177 \pm 6$  cm; 8 females: age  $26.2 \pm 3.0$  years, body mass  $57.4 \pm 6.9$  kg, height  $169 \pm 5$  cm). Training characteristics of the participants reported during the initial questionnaire are depicted in Table 1. All participants were informed of the experimental risks and provided informed consent prior to the commencement of data

collection. Climbers were healthy non-smokers who were not taking any vascular acting medication. The study conformed to the recommendations of World Medical Association and the Declaration of Helsinki and was approved by the Ethics Committee of Charles University, Faculty of Physical Education and Sport under the N° EK 61/2019.

### *Procedures*

All participants completed several exhaustive climbing tests during 5-7 laboratory visits separated by 2-5 days. During visit one, climbers undertook a maximal finger strength test and a familiarisation session on the motorised climbing ergometer (treadwall) at several speeds and angles on a pre-determined route. This route was also subsequently used for the exhaustive testing protocol. On visit two, climbers performed an incremental exhaustive exercise test, which progressed from a positive angle ( $+6^\circ$ ), through vertical ( $0^\circ$ ) to negative (overhanging) angle, the angle at which failure occurred was termed the 'peak-angle'. Climbers were fitted with a near infra-red spectroscopy (NIRS) device on their forearms to assess muscle oxygen dynamics. During the next 3-5 visits, one of the pre-set angles was climbed at a constant speed until failure so that time to exhaustion (TTE) occurred between 2 to 15 min (2019; Vanhatalo et al. 2011). Furthermore, the TTE range between the steepest and the least steep angle was aimed to be as broad as possible (8-12 min) (2019).

Moreover, in order to validate the CA determination from the mathematical model, nine participants completed two additional laboratory visits to climb the same route  $2^\circ$  above and below CA in randomly assigned order.

### *Finger strength*

Maximal finger flexor strength was assessed on a climbing specific dynamometer using methods previously shown to be reliable (Baláš et al. 2018; Michailov et al. 2018). Climbers were asked to progressively transfer their maximum weight ("hang") on a wooden rung (23 mm

deep) for 5 s with their dominant hand. Maximal strength was determined as the highest (peak) value from two trials.

### *Climbing tests*

Climbing tests were conducted on a motorized treadwall (ClimbStation generation, Forssa, Finland). The route was technically simple with positively oriented, and slightly crimped holds (2-3 cm size depth which enabled both the open and half-crimp grip positions) and was graded 8 on IRCRA grading scale at vertical angle (0°) by a professional routesetter. During all ascents, a speed of 9 m·min<sup>-1</sup> was applied to minimise the opportunity for static resting positions during the climbs (Baláš et al. 2021). The incremental test started at +6° (positive angle) and after each minute, the belt was stopped for 10 s to allow climbers to dry their hands with chalk, following which the angle was decreased by -3° to become progressively vertical (0°) and then negative (overhanging), therefore requiring progressively greater finger flexor and upper-body strength involvement. Climbers were not allowed to touch the ground during rest periods. The exhaustive tests at given angles were completed at the same speed and the angle of each remained constant during the whole ascent. Participants were verbally encouraged to climb for as long as possible. Each test ended when a climber reached volitional exhaustion and stepped onto the safety mattress.

### *Muscle oxygenation breakpoint*

During all ascents, a NIRS device (Portamon, Artinis Medical System, BV, Netherlands) was placed over the belly of the flexor digitorum profundus (FDP) (Fryer et al. 2018) and covered by a black forearm garment to shield the optodes from ambient light. Deoxy[heme], muscle tissue oxygen saturation (StO<sub>2</sub>) and total[heme] were used to assess muscle oxygen dynamics and perfusion. Due to the irregular intermittent nature of finger flexor contractions during climbing, deoxy[heme] and StO<sub>2</sub> were averaged over 10 s periods. Raw and corrected NIRS



signals are depicted in Fig 1. The MOB was determined visually from deoxy[heme] inflection points by 3 independent evaluators (Fig 1). The changes in slope signify that  $\Delta$  deoxy[heme] had begun to change faster or slower with increased wall angle. If there was not an agreement on a determined CA, the following procedures were used: 1) if two evaluators were in agreement and one not, then the CA from two evaluators was used; 2) if all three reviewers were differing, then the mean score was used as the CA.

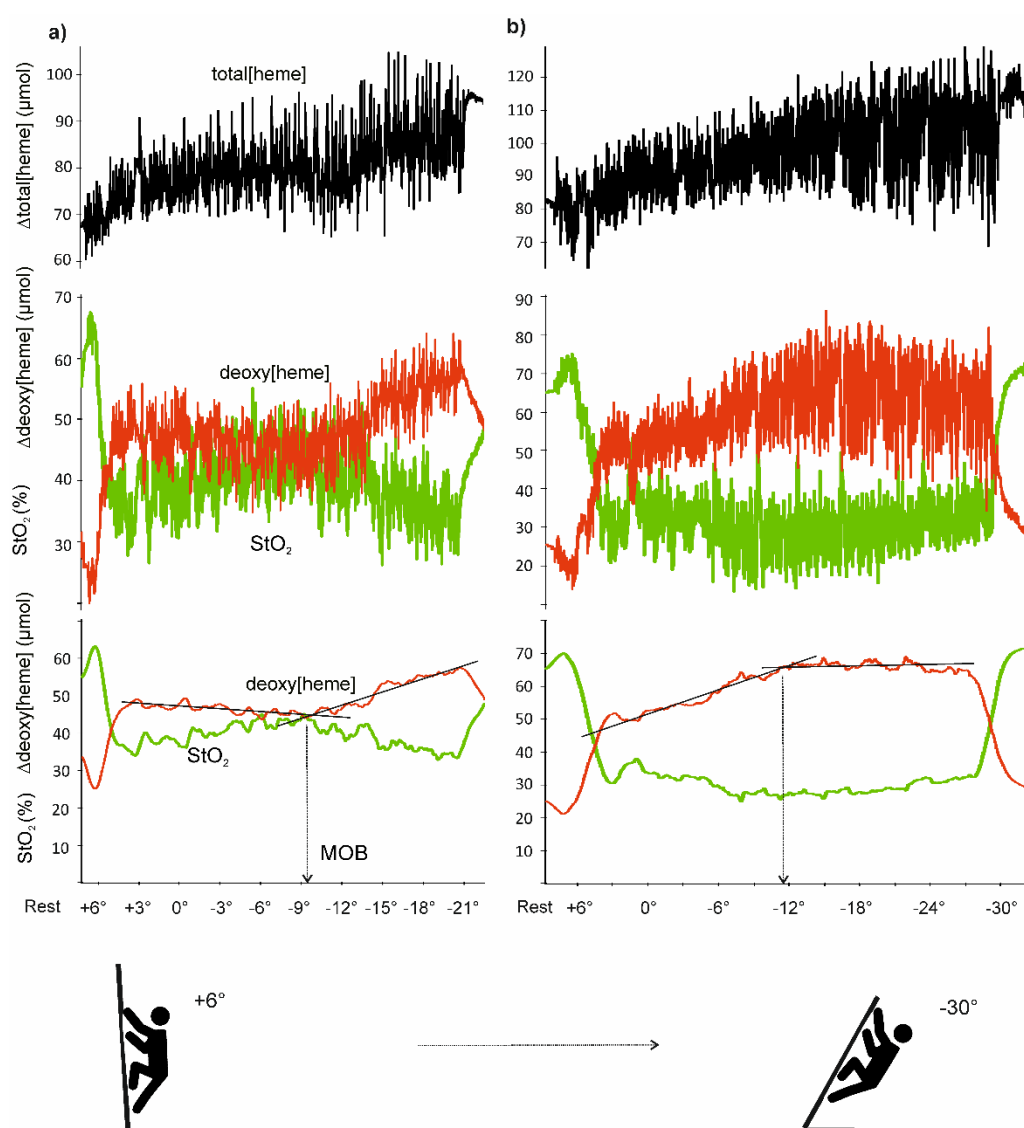


Figure 1 Example of raw and averaged (10 s interval) signal for deoxy[heme], total[heme] and muscle tissue oxygen saturation ( $StO_2$ ) during exhaustive climbing test with progressive increases in angle. Muscle oxygenation breakpoint (MOB) was detected as an inflection point of deoxy[heme] with progressive wall angle. Two typical responses represent sudden increase (a) and onset of a plateau (b) in  $\Delta$ deoxy[heme].

### *Perceived exertion*

Rate of perceived exertion (RPE) during the ascents 2° above and under CA were used to assess subjective perception of exertion intensity. Perceived exertion was assessed on a scale from 6 to 20 as suggested by Borg (Borg 1982). Immediately after the test, climbers were shown a table with numbers and corresponding verbal description of the exertion and indicated their exertion rating to the researcher.

### *Statistical analysis*

Performance and NIRS characteristics were described using mean  $\pm$  standard deviation (SD). Possible differences between males and females were evaluated using independent *t*-tests and Cohen's *d*. To calculate CA, a similar approach for CF was applied (Giles et al. 2019) and the equation with best fit was used for determination of CA:

1.  $A = W' \times \frac{1}{TTE} + CA$ ,
2.  $Wlim = TTE \times CA + W'$ ,

where “A” is the angle of the ascent (°), “CA” is the critical angle (°), “TTE” is the time to exhaustion (s), “W’” is the capacity to climb over CA (°s) and represents the finite time a climber can sustain the ascent at steeper angles than CA, while “W” (°s) can be approximated as “total work” completed by a climber during the incremental exhaustive test. This first equation model plots angle of the ascent against 1/TTE (Fig 2b); CA is given by the y-intercept and W’ by the slope of the regression line. The second equation model plots W against TTE (Fig 2c); CA is given by the slope of the regression line and W’ by the intercept. Both models were applied to all participants, and a model with higher fit was used to estimate individual CA.

To determine validity of CA from the mathematical model, nine climbers were asked to climb 2° above and under CA. The limit of 2° was calculated as 95% confidence interval (95%CI) from standard error of CA estimate (SE = 1.1), therefore 1.96 SE (95%CI = ±2.2°).

Subsequently, the agreement between the CA determination from mathematical model and NIRS was evaluated using Bland-Altman plot and intra-class correlation (ICC). The ICC was calculated as:

$$ICC = \frac{MSB - MSW}{MSB + (k - 1)MSW},$$

where MSB and MSW correspond to mean squares between and within subjects from a repeated measure ANOVA, respectively, and k is the number of trials (2 in this case). This equation encompasses both the variability due to systematic changes between trials and error variability. ICC was expressed with 95%CI.

The association between climbing ability, TTE, CA and  $W'$  were evaluated using Pearson correlation coefficients or linear regression coefficient of determination. Statistical significance was set to  $P < 0.05$ .

## Results

When TTE was plotted against wall angle, the typical hyperbolic function as for power-duration relationship was found (Fig 2a). The linear transformation (wall angle against 1/TTE, Fig 2b) showed high model fit ( $R^2 = 0.99$ ; 95%CI 0.96-1.00) and low standard error of CA estimate (SE = 1.10°; 95%CI 0.83-1.35°). The second linear model ( $W'$  against TTE, Fig 2c) provided less fit ( $R^2 = 0.72$ ; 95%CI 0.61-0.83), and a low standard error of CA estimate was found (SE = 0.99°; 95%CI 0.72-1.25°).

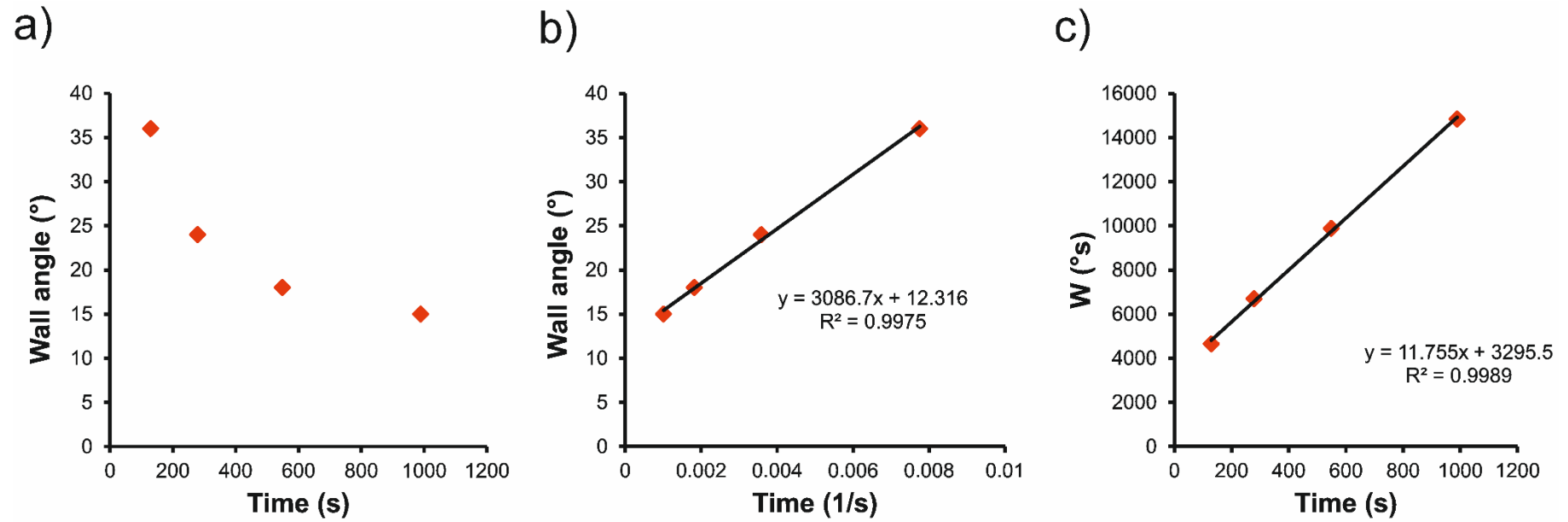


Figure 2 Example of hyperbolic relationship between wall angle and time to exhaustion (2a) and the calculation from linear models using (2b) wall angle (°) against time to failure (1/s); and (2c) work limit  $W$ (°s) against time to failure (s). Coefficient of determination ( $R^2$ ) indicates the fit of the linear model.

TTE at the steepest angle was  $118 \pm 52$  s (wall angle range  $25 - 45^\circ$ ), and the least steep angle was  $808 \pm 192$  s (wall angle range  $0 - 18^\circ$ ). The mean estimated CA ( $-2.5 \pm 3.8^\circ$ ) was significantly associated with climbing ability in lead climbing but not in bouldering ( $R = -0.406$  and  $-0.282$ , respectively), however  $W'$  ( $3251 \pm 1373$  °s) was related to both lead climbing and bouldering ability ( $R = 0.580$  and  $0.695$ , respectively).

*Table 1 Performance and training characteristics (mean  $\pm$  SD) in male and female climbers. Statistically ( $P < 0.05$ ) significant, and effect sizes greater than medium ( $d > 0.5$ ) are in bold format.*

	Males	Females	Differences	
	N = 19	N = 8	P	Cohen's d
Climbing ability lead (IRCRA scale)	$17.9 \pm 4.2$	$16.3 \pm 2.9$	0.326	0.43
Climbing ability boulder (IRCRA)	$21.4 \pm 3.6$	$18.1 \pm 3.3$	0.036	<b>0.94</b>
Experience (years)	$12.1 \pm 7.6$	$8.3 \pm 4.1$	0.188	<b>0.59</b>
Climbing specific training (hours/week)	$6.7 \pm 4.7$	$5.3 \pm 1.8$	0.445	0.35
Endurance training from total climbing time (%)	$55 \pm 28$	$64 \pm 32$	0.486	0.31
$F_{\max}$ (kg)	$57.5 \pm 11.2$	$38.0 \pm 8.3$	<b>&lt;0.001</b>	<b>1.88</b>
CA mathematical model ( $^\circ$ )	$-2.5 \pm 4.3$	$-2.6 \pm 2.1$	0.990	0.01
CA NIRS ( $^\circ$ )	$-2.7 \pm 3.0$	$-2.3 \pm 2.7$	0.728	0.15
Peak angle ( $^\circ$ )	$-16.7 \pm 5.3$	$-16.5 \pm 4.5$	0.913	0.05
$W'$ ( $^\circ$ s)	$3491 \pm 1303$	$2685 \pm 1455$	0.168	<b>0.60</b>

Footnotes. CA estimated critical angle, IRCRA International Rock Climbing Association,  $F_{\max}$  maximal finger flexor strength, NIRS near infra-red spectroscopy

The mean peak-angle' during the incremental test was  $-17 \pm 5^\circ$  and was moderately related to both lead climbing and bouldering ability ( $R = -0.661$  and  $-0.587$ , respectively). Training and performance characteristics for both males and females are depicted in Table 1.

All nine climbers performing the ascent  $2^\circ$  under CA were able to sustain the task for the maximum test duration of 20 min with perceived exertion ( $RPE = 12.1 \pm 1.9$ ). However, climbing  $2^\circ$  above CA led to task failure ( $TTE = 954 \pm 177$  s;  $RPE = 16.4 \pm 1.9$ ) (Fig 3). Only 2 climbers were able to sustain the task for 20 min which was in agreement with their exceptionally high  $W'$  ( $W' > 3500^\circ\text{s}$ ) as their TTE was predicted to last more than 30 min (Fig 3).

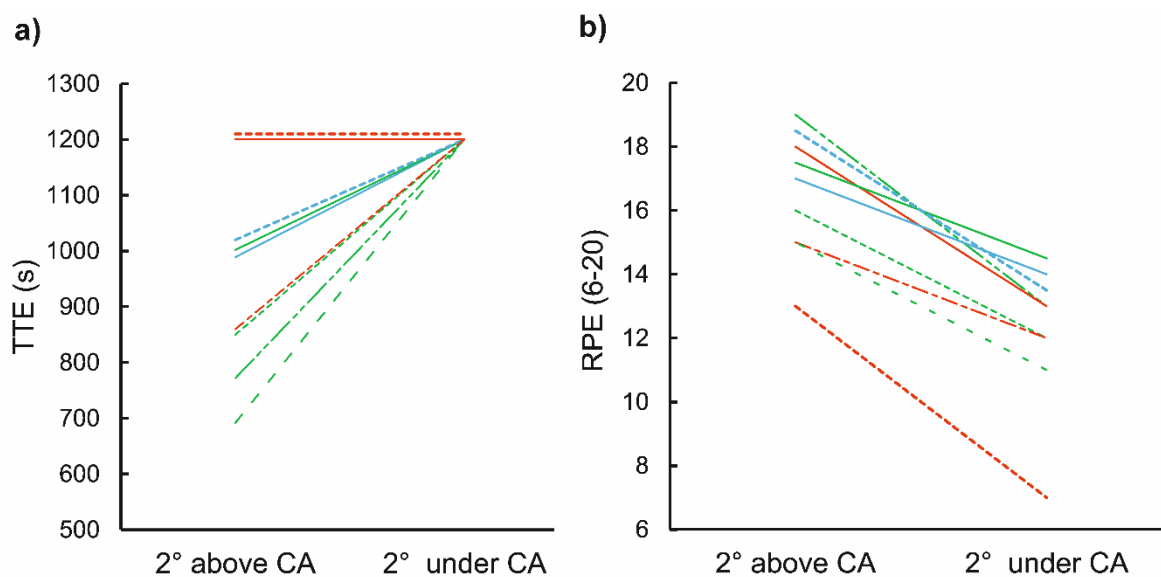


Figure 3 a) Time to exhaustion (TTE) during climbing  $2^\circ$  above and under critical angle (CA). The time of 20 min (1200s) was set as maximal irrespective exhaustion occurred or not. Immediately after the climb, rate of perceived exertion (RPE) was assessed in both conditions (b). Colour of individual lines represent climbers with different level of  $W'$ : red ( $W' > 3500^\circ\text{s}$ ), blue ( $2500 < W' < 3500^\circ\text{s}$ ), green ( $W' < 2500^\circ\text{s}$ ).

The MOB was detectable in all 27 climbers during the incremental exhaustive test, 18 showed inflection points as a faster increase in  $\Delta$ deoxy[heme], while 9 climbers as an onset of a plateau (Fig 1).

Good agreement was found between angle at MOB and CA (ICC=0.80, 95%CI 0.61-0.90, SEM = 1.5°). Limits of agreement plot showed no meaningful differences between the two methods and nearly all estimates were within  $\pm 3^\circ$  (Fig 4). The estimate of MOB as an onset of deoxy[heme] plateau provided larger variability than the inflection point of faster  $\Delta$ deoxy[heme] increase (Fig 4).

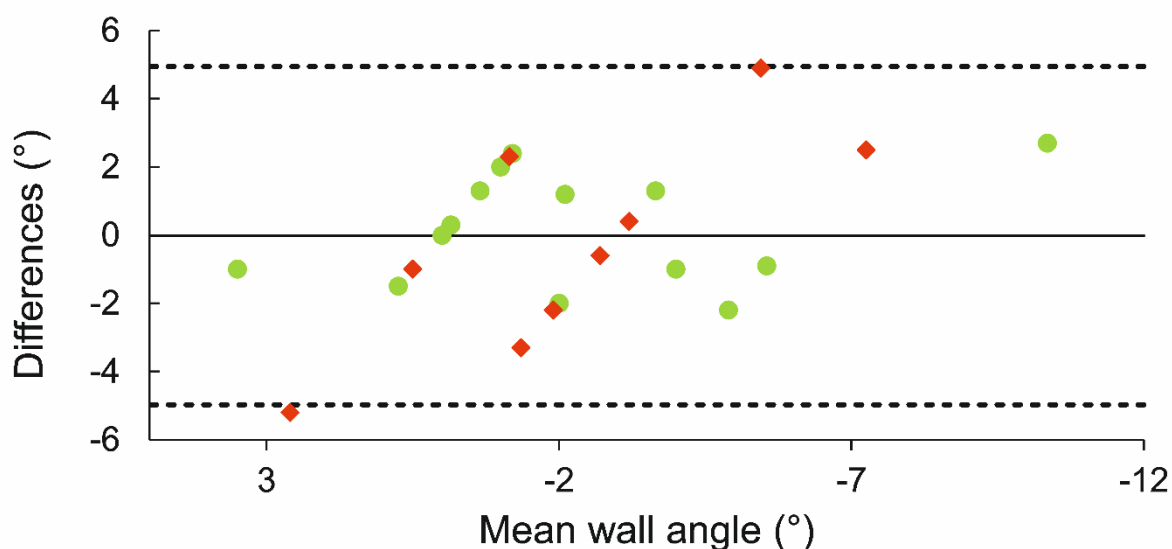


Figure 4 Limits of agreement plot of estimated critical angle (CA) from muscle oxygen breakpoint (MOB) and CA from mathematical model. The solid horizontal line represents differences between the two estimates of CA, the dashed lines upper and lower 95% limits of agreement. Green and red circles designate participants with MOB determined as a sudden increase and onset of a plateau in  $\Delta$ deoxy[heme], respectively.

## Discussion

The main findings of the current study were that: 1) multiple tests to exhaustion with differing climbing angles allow for the estimation of CA at which a maximal metabolic steady state

occurs when climbing; 2) MOB representing a metabolic transition state in the finger flexors is in good agreement with CA.

Manipulating wall angle has previously been shown to be a simple quantitative tool for changing intensity in climbing (Watts and Drobish 1998). Noé et al. (2001) reported that an increase of  $10^\circ$  ( $-10^\circ$  from vertical) induced  $\sim 47\%$  increase in mean vertical force on handholds and, therefore, more intense finger flexor contractions. Furthermore, an increase of wall angle by  $15^\circ$  from vertical elevated heart rate by an average of  $\sim 24$  beats per minute, oxygen uptake by  $\sim 9 \text{ mL}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}$  and lowered muscle oxygen saturation of the FDP by 7% (Baláš et al. 2021). In the current study, TTE decreased with steeper wall angle and the association between TTE and wall angle followed a hyperbolic function (Fig 2) same to the power/speed and duration relationship (Jones et al. 2019). The existence of a CA as a metabolic transitional zone between steady and non-steady state condition provides further support for using climbing angle to adjust intensity during climbing training. However, it should be noted that the same wall angle may induce different forces on handholds even among climbers who have similar characteristics such as body mass and finger strength-endurance. In fact, the whole-body model assessment may encompass not only the metabolic capacity of the forearm flexors but other factors such as movement economy. For instance, movement economy in more advanced climbers has been shown to reduce vertical forces on handholds (Baláš et al. 2014), which would lead to a steeper CA in more “technical” than “stiff” climbers despite their similar metabolic predispositions. Consequently, comparisons among climbers of estimated CA account not only for the level of aerobic capacity, but also for other factors such as movement economy. This is in contrast to the isolated forearm model CF determination (Giles et al. 2019; Giles et al. 2020), where only metabolic factors in specific hanging conditions are assessed. However, the primary aim of the CA determination is not the between-subject comparisons but individual threshold intensity in ecological valid setting. Although movement economy may



differ among climbers, the CA is set for each climber individually as it is expected that each climber has similar movement economy across all trials on the same route. Therefore, technically easy routes should be preferred for individual training prescription to ensure that the shift in CA is due to metabolic adaptations and not a learning effect. Moreover, it should be noted that values of estimated CA will be only valid for a predefined route, as different hold size, more complex moves or different climbing speeds may induce different physiological responses. Using motorized treadwalls appears especially appropriate for the standardisation of training, where the primary aim is to influence metabolic adaptations of finger flexors during whole body climbing movement which may differ from isolated training on hangboards or campus boards (Giles et al. 2020; Medernach et al. 2015; Levernier and Laffaye 2019)

Repeated exhaustive ascents over several days are needed to determine CA and this places high training loads on individuals. Therefore, using MOB during one exhaustive incremental test may be more advantageous for trainers and climbers to set a climbing specific maximal metabolic steady state. The MOB during an exhaustive climbing incremental protocol has been described previously (Baláš et al. 2021) however, the authors could not associate the inflection point of  $\Delta$ deoxy[heme] to any intensity threshold as no relationship to any ventilatory or cardiac responses was found. In the current study, the MOB comparison was made with the CP concept as the local forearm muscle fatigue rather than respiratory exhaustion is the main determinant of failure during climbing (Watts 2004). We found good agreement between MOB and CA (SEM = 1.5%), particularly considering 3° was the smallest change used during the incremental test. However, there were 2 of the 27 climbers who demonstrated differences of ~5°. The explanation may be linked to several mechanisms such as reliability error, error of CA determination or simply that the MOB cannot precisely reflect metabolic steady state intensity. Therefore, repeated testing or climbing slightly below the CA for extended periods of time appear useful to confirm the correct determination of CA.

Deoxy[heme] has been recommended for MOB determination as it is less affected by changes in perfusion under NIRS-probe (Wang et al. 2006; Grassi et al. 2003). Two patterns in  $\Delta$ deoxy[heme] dynamics have been revealed to represent MOB in the current results in line with the literature (Wang et al. 2006). Firstly, the onset of a plateau in deoxy[heme] may reflect microvascular  $O_2$  extraction reaching a ceiling (Boone et al. 2016a; Keir et al. 2015) or simply that short periods of finger flexor reperfusion during hand release from the hold are not sufficient to provide sufficient blood flow at higher intensities and then  $O_2$  delivery into the muscle. Only 9 climbers in the current study showed plateau of deoxy[heme], the other 18 climbers demonstrated faster increase in  $\Delta$ deoxy[heme] at MOB. According to our data (Fig 4), both forms of inflection reflected similar intensities around the CP. This discrepancy in the oxygen dynamics between climbers may be due to many interrelated factors such as relative deepness of muscle analysed under optodes (climbers had various forearm circumference), the muscles involved in the contraction (muscle fibre architecture), muscle fibre types assessed, and/or blood perfusion during the test (Okushima et al. 2015; Murias et al. 2013; Chin et al. 2011). For instance, it has been demonstrated that the deeper layers of rectus femoris have the potential to maintain a higher  $O_2$  delivery to  $O_2$  utilization ratio compared with superficial layers during incremental cycling (Okushima et al. 2015). The less activated rectus femoris provides right shifted dynamics of deoxy[heme] with respect to a more involved vastus lateralis and vastus medialis during ramp exercise (Chin et al. 2011). It is likely that other finger flexors such as the superficial flexors may have been largely involved during intermittent contractions and mitigated the activity of deeper flexors.

In the current study, good agreement between MOB and CA as the maximum steady state intensity was found. Moreover, all climbers exercising  $2^\circ$  under CA were able to sustain 20 min of climbing rating the intensity from light to somewhat hard on Borg scale of perceived exertion, while they were exhausted  $2^\circ$  above CA after  $\sim 16 \pm 3$  min rating the intensity from

hard to extremely hard. This supports our hypothesis that MOB during isometric contractions reflects metabolic changes in the muscle from steady to non-steady state conditions, rather than other intensity boundaries. However, it should be acknowledged that NIRS derived thresholds may be only mechanistically linked to CP threshold as discussed recently (Boone et al. 2016b; Broxterman et al. 2018; Poole et al. 2021).

There was a significant but practically weak relationship between CA and climbing ability ( $R^2 = 0.16$ ) which is in contrast to moderately strong association ( $R^2 = 0.66$ ) from similarly determined MOB in our previous study (Baláš et al. 2021). The discrepancy may be due to selection of climbers who were mixed in sex, and discipline preference. This is supported by generally lower relationship between peak angle and climbing ability in the current study when compared to previous research (Baláš et al. 2021; España-Romero et al. 2009). However, the significant relationship between CA and lead climbing ability supports the importance of oxidative capacity for achieving a high level of performance in lead climbing. On the other hand, a weak non-significant association ( $R^2 = 0.08$ ) with bouldering ability shows that other factors are decisive for the performance of powerful whole-body movements in bouldering. For instance, the ability to climb at intensities (angles) above CA ( $W'$ ) has been shown to be a more important metabolic determinant for bouldering ( $R^2 = 0.48$ ) than for lead climbing ( $R^2 = 0.33$ ). With respect to the current study, it has to be highlighted that climbing performance depends on many others technical and tactical factors and the association between CA and climbing ability will always be lower than typical endurance sports such as running or cycling (Poole et al. 2021). Nevertheless, endurance of the finger flexors is a key sport specific determinant of performance and lead climbers demonstrate specific adaptations (Thompson et al. 2014; Ferguson and Brown 1997). It has been suggested that using CP and  $W'$  may be extremely valuable in constructing individually optimized interval training programmes in a range of

athletes and sport disciplines (Vanhatalo et al. 2011), therefore coaches may use CA as the threshold intensity to train forearm muscles endurance under sport specific conditions.

Limitations of the study include the assumptions associated with the use of continuous-wave NIRS measurement during exercise such as adipose tissue thickness, subcutaneous blood flow or the use of physiological calibration (Barstow 2019). However, adipose tissue under the optodes should not have affected the results as skinfold thickness in climbers' forearms has been found to be very low (Fryer et al. 2018; Baláš et al. 2018). In addition, the use of spatial resolved spectroscopy, as used in the present study, appears to be unaffected by heating induced changes in cutaneous circulation (Barstow 2019), and as such there was no need for the physiological calibration of the NIRS output as changes in TSI and deoxy[heme], rather than absolute values, were evaluated (Barstow 2019). It should also be noted that the findings of the current study are based on a technically simple climbing route at one speed with handholds of a relatively similar size, which may differ from technical rock climbing ascents.

## **Conclusions**

Our data show that multiple tests to exhaustion with differing climbing angles allow for the estimation of CA. Climbers, coaches and researchers may use a predefined route/circuit at three to five angles in order to estimate CA as a parallel of metabolic transition from steady to non-steady states (heavy to severe exercise intensity domains). Climbing 2° below CA is tolerable for extended periods of time and perceived as light to somewhat hard, while climbing 2° above CA leads to finite time to failure. Moreover, an exhaustive climbing test with progressive increases in angle using the MOB appears to provide a valid estimation of CA.

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## **Declaration of interest**

It should be noted that one of the authors (DG) is employed by Lattice Training Ltd. who provides climbing coaching and assessment services. JB is currently affiliated with Climbro, a private company who provides hangboards with integrated force sensors and mobile application for climbing specific training. The remaining authors have no competing interests to declare and assert that the results of the study are presented clearly, honestly, and without fabrication, falsification, or inappropriate data manipulation.

## **Author Contribution Statement**

JB developed the theoretical framework, conceived the study, collected the data, analysed the data, and wrote the article. JG developed the theoretical framework, conceived the study, and analysed the data. SF and DG provided critical feedback on drafts and edited the final paper for submission.

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