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**Stenroth, Lauri, Cronin, Neil ORCID logoORCID:
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Triceps surae muscle-tendon properties in older endurance- and sprint-trained athletes

Lauri Stenroth,^{1,2} Neil J. Cronin,¹ Jussi Peltonen,¹ Marko T. Korhonen,² Sarianna Sipilä,² and Taija Finni¹

¹ Neuromuscular Research Center, Department of Biology of Physical Activity, University of Jyväskylä, Jyväskylä, Finland; and ²Gerontology Research Center and Department of Health Sciences, University of Jyväskylä, Jyväskylä, Finland

Abstract

Previous studies have shown that aging is associated with alterations in muscle architecture and tendon properties (Morse CI, Thom JM, Birch KM, Narici MV. *Acta Physiol Scand* 183: 291–298, 2005; Narici MV, Maganaris CN, Reeves ND, Capodaglio P. *J Appl Physiol* 95: 2229–2234, 2003; Stenroth L, Peltonen J, Cronin NJ, Sipilä S, Finni T. *J Appl Physiol* 113: 1537–1544, 2012). However, the possible influence of different types of regular exercise loading on muscle architecture and tendon properties in older adults is poorly understood. To address this, triceps surae muscle-tendon properties were examined in older male endurance (OE, $n = 10$, age = 74.0 ± 2.8 yr) and sprint runners (OS, $n = 10$, age = 74.4 ± 2.8 yr), with an average of 42 yr of regular training experience, and compared with age-matched [older control (OC), $n = 33$, age = 74.8 ± 3.6 yr] and young untrained controls (YC, $n = 18$, age = 23.7 ± 2.0 yr). Compared with YC, Achilles tendon cross-sectional area (CSA) was 22% ($P = 0.022$), 45% ($P = 0.001$), and 71% ($P < 0.001$)

larger in OC, OE, and OS, respectively. Among older groups, OS had significantly larger tendon CSA compared with OC ($P = 0.033$). No significant between-group differences were observed in Achilles tendon stiffness. In older groups, Young's modulus was 31-44%, and maximal tendon stress 44 –55% lower, than in YC ($P \leq 0.001$). OE showed shorter soleus fascicle length than both OC ($P < 0.05$) and YC ($P < 0.05$). These data suggest that long-term running does not counteract the previously reported age-related increase in tendon CSA, but, instead, may have an additive effect. The greatest Achilles tendon CSA was observed in OS followed by OE and OC, suggesting that adaptation to running exercise is loading intensity dependent. Achilles tendon stiffness was maintained in older groups, even though all older groups displayed larger tendon CSA and lower tendon Young's modulus. Shorter soleus muscle fascicles in OE runners may be an adaptation to life-long endurance running.

Key words

Achilles tendon; mechanical properties; muscle architecture; aging; exercise

Loss of muscle function with aging is associated with physical limitations and disability (40). Decline in muscle mass is undoubtedly an important contributor to the deterioration in muscle function with aging (16). However, longitudinal studies have shown a clear dissociation in loss of muscle function and cross-sectional area or mass with aging (9, 17), suggesting that other factors may also contribute to the age-related loss of muscle function. Muscle architecture and tendon mechanical properties greatly affect muscle performance (28, 51) and have been found to differ between young and old sedentary adults (36, 37, 44). Thus age-related alterations in muscle architecture and tendon mechanical properties may partially explain the loss of muscle performance with age that occurs at a disproportionately faster rate than the decline in muscle mass.

Regular exercise is a key aspect supporting healthy aging. Indeed, it has been suggested that older athletes provide a model of exceptionally successful biological aging (46). For example, previous studies have shown that aged athletes with systematic exercise training habits exhibit much better cardiorespiratory, metabolic, and bone health than their less active counterparts (22, 49). Regular exercise training, especially strength and sprint exercise, also helps to maintain muscle mass, function (21, 52), and composition (43), thus counteracting the age-related decline in functional performance typically observed in normal populations (9, 39).

Despite several known beneficial effects of regular exercise on the musculoskeletal system in old age, little is known about the effects of regular participation in planned exercise on muscle architecture and tendon properties in older adults. Two previous studies have compared untrained older adults to older endurance runners. First, Karamanidis and Arampatzis (19) found that muscle architecture and tendon stiffness in medial gastrocnemius and vastus lateralis were largely similar in older endurance runners compared with untrained older adults. The only significant difference was greater medial gastrocnemius pennation angle in endurance runners. Second, Couppé et al. (7) recently found that older endurance runners had a greater patella tendon cross-sectional area but similar tendon stiffness compared with untrained peers. These previous studies were conducted on endurance runners, and thus knowledge of

the long-term effects of different types of exercise loading on muscle architecture and tendon properties in older adults is missing.

Therefore, the aim of this study was to examine the association between different types of life-long exercise and muscle-tendon properties by comparing muscle architecture and tendon properties in older sprint and endurance runners to both age-matched and young untrained adults. Triceps surae muscles were studied because of their important role in locomotion and because they exhibit the greatest functional limitation of all lower limb muscle groups in older adults during locomotion (24). Endurance running provides a model of high-volume and moderate-intensity loading, while sprint running represents a model of low-volume but high-intensity loading of triceps surae muscles. The hypothesis was that older athletes with a life-long regular running background would exhibit muscle fascicle length, pennation angle, muscle size, muscle strength, and tendon mechanical properties in the triceps surae muscle group that are more similar to those of young adults than untrained older adults. In addition, based on previous cross-sectional studies conducted in young adults (1, 2), it was hypothesized that sprint-trained older athletes would be stronger, have stiffer Achilles tendons, lower pennation angle, and longer muscle fascicles compared with endurance-trained older athletes.

Materials and methods

Subjects.

Male subjects were recruited in two age categories, one from 18 to 30 yr old [untrained young controls (YC), $n = 18$] and the other from 70 to 80 yr old. The older cohort was recruited in three groups: untrained older controls (OC, $n = 33$), older athletes competing in endurance running events (OE, $n = 10$) and older athletes competing in sprint running events (OS, $n = 10$).

Untrained YC and OC groups were part of a Europe-wide collaborative study called MyoAge (34) and included in the present study to represent general populations of healthy young and older adults. We defined untrained as a person who may be recreationally active but is not training for, or participating in, competitive sport. YC were recruited from among university students using study advertisements via e-mail and bulletin boards. We excluded those who studied sport sciences, as well as competitive athletes. OC were recruited from the University of the Third Age or from weekly community meetings of retired people. The aim was to recruit healthy older people who were socially active and free from comorbidity. Using telephone interviews, an equal number of sedentary and physically active (competitive athletes excluded) older subjects were recruited to obtain a representative sample of older people with varying physical activity levels. Sedentariness was defined as exercising for fitness and health one or fewer times per week. Physically active was defined as exercise three or more times per week (30 min or more with intensity sufficient to cause sweating or breathlessness). Results (44) and more detailed description of the recruitment (34) of YC and OC have been presented earlier.

Older athletes were recruited among the participants of the World Master Athletics Indoor Championships held in Jyväskylä, Finland in 2012. Twenty male athletes were recruited based on the events in which they participated during the championships. Ten subjects were recruited from sprint running events (60 m, 60 m hurdles, 200 m, 400 m) and 10 were recruited from endurance running events (3 km, half marathon, and 8 km cross country running). Some subjects in the OS and OE groups participated in several sprint or endurance running events, respectively. Mean results of the subjects competing in the championships were as follows: 60 m, 9.13 ± 0.48 s ($n = 8$); 60-m hurdles, 10.15 s ($n = 1$); 200 m, 30.64 ± 1.97 s ($n = 7$); 400 m, $1:13 \pm 8$ min:s ($n = 3$); 3,000 m, $13:48 \pm 60$ min:s ($n = 4$); half marathon, $1:43:37 \pm 11:34$ h:min:s ($n = 5$); and 8 km cross country running, $44:19 \pm 6:25$ min:s ($n = 7$). These results correspond to 8, 1, 11, 16, 22, and 16% slower than the world record times for 75-yr-old men in 60 m, 60-m hurdles, 200 m, 400 m, 3,000 m, and half marathon, respectively. Thus the participating subjects can be considered to be highly competitive athletes.

Subject exclusion criteria were Achilles tendon pain, history of Achilles tendon rupture or surgery, pain in calf muscles during measurements, neurological and progressive severe illnesses, insulin-treated diabetes, fracture within the previous year, immobilization for 1 wk during the last 3 mo, daily use of painkillers, use of immunosuppressive drugs or anticoagulants, or severe visual or hearing impairment.

The ethics committee of the Central Finland Health Care District approved the study. All participants signed an informed consent before participating in the study, and measurements were conducted according to the standards set by the latest revision of the Declaration of Helsinki.

Measurements.

Training characteristics of OE and OS groups were assessed with self-reported questionnaire. The athletes were asked about their training history (yr), overall training volume (h/wk), and amount of endurance (km/wk), sprint (sessions/wk), and strength training (sessions/wk) in their current normal training routines.

Laboratory measurements included assessment of triceps surae muscle architecture and size and Achilles tendon cross-sectional area and mechanical properties. The measurement procedures have been previously described in detail (44), but are briefly described below.

For the measurements of Achilles tendon and both gastrocnemius and soleus muscle architecture and size at rest, the subjects were lying prone facing down with ankle angle at 90°. Tendon cross-sectional area (mm²) was measured from a B-mode ultrasound image taken 4 cm proximal from the proximal border of the calcaneal tubercle where the free Achilles tendon typically reaches its smallest cross-sectional area (38). Body mass normalized tendon cross-sectional area was calculated by dividing cross-sectional area by body mass^{2/3} (20). Muscle architecture from medial gastrocnemius and soleus muscles

was assessed from ultrasound images taken at 50% of medial gastrocnemius length and mid-muscle belly in the medial-lateral direction. Fascicle length (mm), pennation angle ($^{\circ}$), and muscle thickness (mm) were measured from the images. To take into account between-subject differences in stature, fascicle length was normalized to tibia length. The combined anatomical cross-sectional area (cm^2) of medial and lateral gastrocnemius was measured from a panoramic B-mode ultrasound image taken at 50% of medial gastrocnemius length as a measure of the size of the gastrocnemius muscles. All measurements from ultrasound images were taken twice using an open-source computer program (ImageJ 1.44b, National Institutes of Health), and the mean was used for subsequent data analysis.

For the measurement of Achilles tendon mechanical properties, the subjects were seated in a custom-built dynamometer with ankle angle at 90° and knee fully extended and hip at 60° of flexion (full extension 0°). After a standardized warm-up, three maximal voluntary contractions (MVC) lasting ~ 3 s were performed with strong verbal encouragement to measure plantar flexion strength (Nm). The highest value obtained during MVC trials was used for subsequent analysis. Warm-up and plantar flexion MVCs served to precondition the tendon before the measurement of tendon mechanical properties (30). Achilles tendon mechanical properties were measured from several isometric plantar flexion contractions up to a force level of 80% of MVC. Tendon force was calculated by multiplying measured reaction force by the ratio between Achilles tendon moment arm length and moment arm of the reaction force. Achilles tendon moment arm was defined as the distance from the center of the Achilles tendon to the outermost tip of the medial malleolus in the sagittal plane measured using a ruler. The moment arm of the reaction force around the ankle joint was defined as the sagittal plane distance between the outermost tip of the medial malleolus and the head of the first metatarsal. Achilles tendon elongation (mm) was defined as the change in the distance between the proximal border of the calcaneal tubercle and the medial gastrocnemius muscle-tendon junction. Changes in the location of the calcaneal tubercle in the laboratory coordinate system were measured using a potentiometer that measures heel lift from the dynamometer footplate. Medial gastrocnemius muscle-tendon junction location in the laboratory coordinate system was measured with a combination of B-mode ultrasonography and motion analysis.

Ultrasound images of the muscle-tendon junction were collected at 70 Hz, and the location of the muscle tendon junction within the image was defined by automatic tracking software (32). The location of the muscle-tendon junction was converted to the laboratory coordinate system using video-based motion capture of the ultrasound probe. Two parameters that describe tendon mechanical properties were calculated, tendon stiffness (N/mm) and Young's modulus (GPa). Tendon stiffness characterizes mechanical properties of the tendon and is defined as the slope of the linear portion of the tendon force-elongation curve. We calculated tendon stiffness as a linear fit to force-elongation data from 10 to 80% MVC force, as the curves were almost perfectly linear in this region (Fig. 1, $r^2 = 0.999$ from linear fits to average force-elongation curves). Tendon Young's modulus is the slope of the linear portion of the tendon stress-strain curve and represents tendon stiffness normalized to tendon dimensions. Young's modulus describes the mechanical properties of the material from which a tendon is composed. To derive Young's modulus, Achilles tendon stress (Pa) was calculated by dividing Achilles tendon force (N) by tendon cross-sectional area (m^2), and strain (%) was calculated by dividing elongation (mm) by initial tendon length (mm) multiplied by 100. Young's modulus was calculated as a linear fit to force-elongation data from 10 to 80% MVC force.

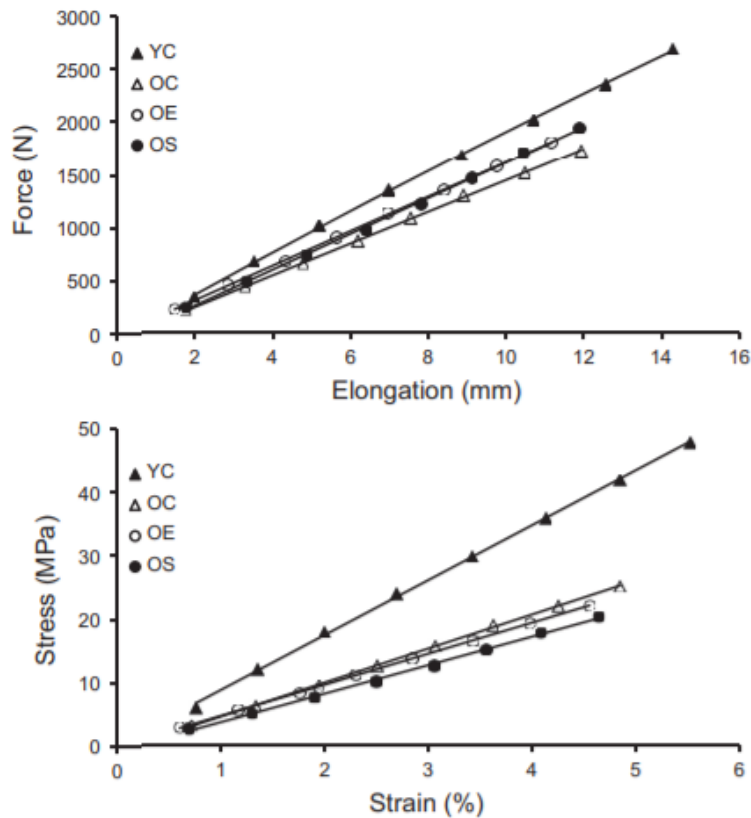


FIGURE 1 MEAN ACHILLES TENDON FORCE-ELONGATION (TOP) AND STRESS-STRAIN (BOTTOM) RELATIONSHIPS FOR YOUNG CONTROLS (YC), OLDER CONTROLS (OC), OLDER ENDURANCE RUNNERS (OE), AND OLDER SPRINT RUNNERS (OS). LINES ARE LINEAR FITS AND REPRESENT ACHILLES TENDON STIFFNESS (TOP) AND YOUNG'S MODULUS (BOTTOM). VALUES ARE CALCULATED AT 10% MAXIMAL VOLUNTARY CONTRACTION INCREMENTS FROM 10 TO 80% MAXIMAL VOLUNTARY CONTRACTION. SDs ARE OMITTED FOR CLARITY.

Statistical analyses.

Due to inadequate image quality, soleus muscle architecture data were excluded for two subjects from the OS group and three from the OC group, whereas medial gastrocnemius muscle architecture data were excluded for one subject from OE, and gastrocnemius cross-sectional area data from one subject from OC. Data were first checked for normality with the Shapiro-Wilk test and for homogeneity of variance with Levene's test. Differences in muscle and tendon properties between the groups were tested using single-factor analysis of variance and Tukey-Kramer post hoc test. Games-Howell post hoc test was used when inhomogeneous variances between the groups were observed, and Kruskal-Wallis test with Bonferroni correction for nonnormally distributed variables. Differences in training

characteristics between OE and OS were tested using Mann-Whitney U-test. The level of statistical significance was set at $\alpha = 0.05$ for all tests. Statistical analyses were performed using IBM SPSS Statistics (version 20.0.0.2). Standardized mean differences between YC and groups of older adults were calculated for main results of the study (see Tables 2 and 3) as a measure of effect sizes using Hedges' g , including a correction for small sample bias (12).

Results

Subject characteristics and training status for the older athletes are reported in Table 1. Older adults in the three different groups were matched for age, height, and body mass. YC were significantly taller than OC ($P < 0.001$). OC had significantly greater body mass index compared with YC ($P = 0.006$) and OE ($P = 0.009$). Significantly lower plantar flexion strength was found in OC (34%, $P = 0.001$) and OE (42%, $P < 0.001$) compared with YC, but not in OS compared with YC ($P = 0.077$). OE and OS groups did not differ in years of training, hours of training per week, or number of strength training sessions per week. Endurance training measured in distance was eight times greater in OE compared with OS ($P < 0.001$), and OS did three times more sprint training sessions per week than OE ($P = 0.006$).

TABLE 1 SUBJECT CHARACTERISTICS AND TRAINING STATUS OF OLDER ATHLETES

	YC	OC	OE	OS
Subjects, no.	18	33	10	10
Age, yr	23.7 \pm 2.0	74.8 \pm 3.6*	74.0 \pm 2.8*	74.4 \pm 2.8*
Height, cm	181 \pm 6	173 \pm 5*	175 \pm 7	176 \pm 7
Body mass, kg	75.4 \pm 9.0	76.1 \pm 7.7	69.9 \pm 6.9	74.3 \pm 7.1
BMI, kg/m²	23.1 \pm 2.6	25.4 \pm 2.4*†	22.7 \pm 1.6	24.1 \pm 1.9
Plantar flexion strength, Nm	199 \pm 56	132 \pm 21*	116 \pm 25*	153 \pm 39
Length of training, yr			39.4 \pm 20.9	44.7 \pm 19.7
Training per week, h			6.8 \pm 3.3	6.2 \pm 2.6
Endurance training per week, km			55.2 \pm 8.8	6.5 \pm 2.8†
Sprint training sessions per week, no.			0.8 \pm 0.7	2.3 \pm 1.2†
Strength training sessions per week, no.			0.5 \pm 0.2	0.9 \pm 0.2

Values are means \pm SD. BMI, body mass index; YC, young controls; OC, older controls; OE, older endurance runners; OS, older sprint runners. Significantly different from *YC and †OE: $P < 0.01$.

Achilles tendon cross-sectional area was 22, 45, and 71% larger in OC ($P = 0.022$), OE ($P = 0.001$), and OS ($P < 0.001$) compared with YC, respectively (Table 2). Tendon cross-sectional area in OS was significantly larger than in OC ($P = 0.033$). Body mass-normalized tendon cross-sectional area yielded similar results to the unnormalized values. No statistically significant differences were observed between the groups in Achilles tendon stiffness (Fig. 1), but Young's modulus was 31, 35, and 44% smaller in OC ($P < 0.001$), OE ($P = 0.001$), and OS ($P < 0.001$) compared with YC, respectively. Maximal tendon force during MVC was significantly lower in OC (35%, $P < 0.001$) and OE (38%, $P < 0.001$), but not in OS ($P = 0.156$), compared with YC. Average tendon stress during MVC was greater in YC than the older groups ($P < 0.001$). Tendon elongation at 80% MVC was significantly greater in YC compared with OC ($P = 0.014$), but the difference did not reach statistical significance in OE ($P = 0.114$) or OS ($P = 0.352$). However, effect sizes between YC and OE and OS were greater than the effect size between YC and OC. The groups did not differ significantly in tendon strain at 80% MVC.

TABLE 2 ACHILLES TENDON CROSS-SECTIONAL AREA AND MECHANICAL PROPERTIES

	YC	OC	OE	OS
Cross-sectional area, mm²	56.5 ± 9.6	69.0 ± 12.2 (-1.05)*‡	82.0 ± 19.8 (-1.69)†	96.5 ± 24.9 (-2.26)†
Stiffness, N/mm	186 ± 37	164 ± 47 (0.49)	172 ± 39 (0.34)	166 ± 35 (0.51)
Young's modulus, GPa	0.86 ± 0.20	0.59 ± 0.17 (1.46)†	0.56 ± 0.22 (1.40)†	0.48 ± 0.19 (1.85)†
Maximum tendon force, kN	3.4 ± 0.9	2.2 ± 0.6 (1.58)†	2.1 ± 0.4 (1.64)†	2.6 ± 0.8 (0.80)
Maximum tendon stress, MPa	59.3 ± 14.9	33.1 ± 9.0 (2.22)†	26.5 ± 8.3 (2.36)†	30.1 ± 14.3 (1.86)†
Elongation at 80% MVC, mm	14.3 ± 2.5	11.9 ± 6.4 (0.42)*	11.2 ± 4.4 (0.88)	11.9 ± 4.2 (0.70)
Strain at 80% MVC, %	5.6 ± 1.5	4.8 ± 2.2 (0.42)	4.5 ± 1.8 (0.66)	4.7 ± 1.7 (0.56)

Values are means ± SD (with effect size compared with YC in parentheses). MVC, maximal voluntary contraction. Significantly different from YC: * $P < 0.05$, † $P < 0.01$. ‡Significantly different from OS, $P < 0.05$.

Results of soleus and gastrocnemius muscle architecture and size, as well as plantar flexion muscle strength, are presented in Table 3. Soleus fascicle length was significantly shorter in OE compared with YC (absolute $P = 0.014$, normalized $P = 0.002$) and also compared with OC (absolute $P = 0.047$, normalized $P < 0.001$). No significant differences were found in soleus pennation angle or muscle thickness. Medial gastrocnemius fascicle length and pennation angle did not differ between the groups. In OC, medial

gastrocnemius muscle thickness was significantly smaller in contrast to YC ($P = 0.043$) and gastrocnemius cross-sectional area was significantly smaller in contrast to YC ($P = 0.011$) and OS ($P = 0.011$).

TABLE 3 MUSCLE ARCHITECTURE AND SIZE

	YV	OC	OE	OS
Soleus fascicle length, mm	40.6 ± 8.8	38.6 ± 7.6 (0.24) ^c	31.2 ± 3.9 (1.18) ^a	35.3 ± 8.3 (0.57)
Normalized solus fascicle length, mm/mm	0.102 ± 0.021	0.100 ± 0.021 (0.11) ^d	0.073 ± 0.008 (1.55) ^b	0.083 ± 0.022 (0.83)
Soleus pennation angle, °	21.0 ± 5.7	21.2 ± 4.0 (-0.05)	23.7 ± 5.3 (-0.46)	21.6 ± 8.3 (-0.08)
Soleus thickness, mm	14.3 ± 2.6	13.1 ± 2.7 (0.44)	13.4 ± 2.7 (0.33)	12.8 ± 3.7 (0.49)
MG fascicle length, mm	47.7 ± 6.6	45.0 ± 7.6 (0.35)	45.3 ± 6.5 (0.34)	47.7 ± 7.0 (0.00)
Normalized MG fascicle length, mm/mm	0.121 ± 0.018	0.117 ± 0.022 (0.17)	0.108 ± 0.015 (0.71)	0.111 ± 0.021 (0.46)
MG pennation angle, °	24.8 ± 4.0	24.4 ± 4.2 (0.09)	23.3 ± 4.8 (0.34)	24.1 ± 3.5 (0.18)
MG thickness, mm	20.1 ± 2.5	17.7 ± 3.2 (0.77) ^a	17.2 ± 3.6 (0.94)	18.6 ± 2.7 (0.55)
Gastrocnemius cross-sectional area, cm²	24.2 ± 4.5	20.1 ± 4.5 (0.89) ^{a,e}	20.9 ± 3.4 (0.73)	25.1 ± 4.4 (-0.19)

Values are means ± SD (with effect size compared with YC in parentheses). MG, medial gastrocnemius. Significantly different from YC: ^a $P < 0.05$, ^b $P < 0.01$. Significantly different from OE: ^c $P < 0.05$, ^d $P < 0.01$. ^eSignificantly different from OS: $P < 0.05$.

Discussion

We examined selected triceps surae muscle-tendon properties of two differently trained groups of older athletes with an average of 42 yr of regular running training and compared them to untrained age-matched older and young adults. The main findings of the study were that Achilles tendon cross-sectional area was significantly larger in all older adult groups than young adults, and in older sprinters compared with age-matched untrained older adults, whereas there were no statistically significant group differences in Achilles tendon stiffness. The greater tendon cross-sectional area was also reflected in tendon Young's modulus and tendon average tensile stress during maximal isometric force production, both of which were significantly lower in all older groups compared with young untrained adults. Only minor differences were observed in triceps surae muscle architecture, the most important being significantly shorter fascicle length in soleus muscle in older endurance runners. The present study adds new insight into possible effects of exercise loading on muscle and tendon structure and function in older age. The novelty of the present study is that measurements of triceps surae muscle architecture and

Achilles tendon properties were made from top-level older athletes that included both endurance and sprint runners.

Achilles tendon properties.

To the best of our knowledge, this is the first study to show greater Achilles tendon cross-sectional area in older adults with a regular exercise training background. Contradicting our hypothesis, the results suggest that long-term exercise did not counteract the age-related increase in Achilles tendon cross-sectional area. Previous cross-sectional studies suggest that Achilles tendon cross-sectional area increases in response to both long-term exercise loading (20, 33) and normal aging (31, 44). The present results suggest that the Achilles tendon responds to regular loading by increasing cross-sectional area in an intensity-dependent manner. Moreover, the increase in cross-sectional area appears to be additive to the increase due to normal aging. This finding supports recent findings by Couppé et al. (7), who showed that regular endurance running was associated with larger patella tendon cross-sectional area in both young and older adults.

A possible explanation for aging and exercise training to be associated with larger tendon cross-sectional area is that tendon hypertrophy is needed to compensate for an age-related decrease in mechanical properties of the tendon collagen structure. Another possible explanation is that greater tendon cross-sectional area in older adults is observed as a consequence of intratendinous accumulation of lipids or water. These two possible mechanisms are not exclusive and could together explain the observed results. The following paragraphs introduce these proposed explanations in more detail.

In animal models, aging has been linked with an increase in type V collagen and a greater proportion of small collagen fibrils, which probably contribute to concurrently observed reduced ultimate tensile stress (10, 48). Greater tendon cross-sectional area in older adults could be due to a necessary adaptation to reduce maximal tendon stress to safe levels for older tendons that possibly have reduced ultimate tensile

stress. To reduce the stress to a safe level, cross-sectional area must be proportional to maximal force acting on the tendon, thus explaining the greater cross-sectional area in older sprint runners compared with older untrained adults observed in the present study.

Greater tendon cross-sectional area in older adults could also serve to maintain sufficient stiffness, which could be important both for protecting the tendon from strain-induced damage and for muscle function. A possible age-related reduction in stiffness of tendon collagen structure may be partly compensated by an age-related increase in collagen cross-links, especially in advanced glycation end-product cross-links (6), which stabilize collagen structure and may increase tendon stiffness. Life-long endurance running has been shown to be associated with lower advanced glycation end product cross-link density (7). If older athletes in the present study had a lower density of collagen cross-links, this could explain the requirement for older athletes to have even greater tendon cross-sectional area compared with untrained older adults, to maintain tendon stiffness with aging.

Based on current knowledge of tendon adaptation, loading intensity is the main factor determining adaptations in tendon mechanical properties (5). Thus it seems unlikely that sprint-trained older athletes would have the lowest Achilles tendon Young's modulus among the groups in the present study. A possible explanation could be that larger tendon cross-sectional area in older adults is not an adaptation to lowered tendon Young's modulus. Instead it could be due to accumulation of tendon subcomponents that do not markedly affect tendon mechanical behavior. These could include extracellular lipid deposits and proteoglycans and glycosaminoglycans that attract water. Extracellular lipid deposits within tendon have been associated with aging (14), and this could be common to all older adults, irrespective of exercise training. On the other hand, production of proteoglycans and glycosaminoglycans could be increased with exercise training-induced tendon loading (15). This would explain the observed lower Young's modulus and stress of the tendon in older adults in the present study and also explains why greater tendon cross-sectional area was not related to greater tendon stiffness.

Within- and between-operator reliability of Achilles tendon cross-sectional area measurement using ultrasound imaging has been reported to be good (11, 50). In the present study, duplicate analysis of tendon cross-sectional area images produced intraclass correlation 0.989 and typical error 2.1%. However, validity of tendon cross-sectional area measurement using ultrasound imaging is not known; thus the results should be interpreted with some caution. Future studies should try to replicate the findings of the present study, preferably using magnetic resonance imaging, which allows measurements of tendon cross-sectional area along the whole tendon. More research examining tendon composition and collagen structure in older adults is also warranted to explain the mechanisms behind changes in tendon cross-sectional area.

In contrast to our hypothesis that life-long running would mitigate age-related changes in tendon mechanical properties, we found that Young's modulus was significantly lower in older compared with young adults, irrespective of training status, with no significant differences between the older groups. There were also no significant between-group differences in initial tendon length or tendon stiffness. Thus the lower Young's modulus in older compared with young adults can be attributed mainly to the larger tendon cross-sectional area in older adults.

It should be noted that a toe-region with a lower slope of the tendon force-elongation curve at low forces or stresses was not observed (Fig. 1). We think that the reason for highly linear force-elongation/stress-strain curves is initial force acting on the Achilles tendon at a 90° ankle angle, and the fact that we calculated the curve starting from 10% MVC force. Lack of toe-region has also been previously observed for Achilles tendon in vivo when elongation is measured from the medial gastrocnemius muscle-tendon junction (27), as done in the present study.

To summarize the findings regarding tendon mechanical properties, Young's modulus of the Achilles tendon was significantly lower in older compared with young adults, irrespective of training status. Despite this, Achilles tendon stiffness was conserved in all groups of older adults. Thus the lower muscle

strength, greater tendon cross-sectional area, and conserved tendon stiffness resulted in reduced maximal tendon stress and strain in older adults. Reduced tendon stress and strain could be a necessary mechanism to decrease the probability of tendon injury, as aging may decrease tendon fascicle sliding that possibly leads to greater loading of the fascicles themselves (47). A functional consequence of similar Achilles tendon stiffness but lower muscle strength in older compared with young adults is a limited maximal capacity for elastic energy storage and subsequent utilization during locomotion. This may contribute to the reported greater metabolic cost of transport in older compared with young adults (35).

Triceps surae muscle architecture, size, and strength.

The present data also suggest that, in general, muscle architecture is not greatly different in older habitual runners in contrast to both untrained older or young adults. Soleus fascicle length was found to be significantly shorter in endurance-trained older adults than young and older untrained adults. Although somewhat speculative, it may be that shorter fascicles observed in long-term endurance runners in the present study are due to adaptation that improves the efficiency of force production in locomotion. Soleus has short muscle fascicles compared with tendon length (51). Consequently, soleus muscle operates mainly as a force rather than a power producer in locomotion (4). Thus, as this muscle does not need to produce large amounts of work, short fascicles may decrease the energy cost of force production due to lower activated muscle volume per unit of force output compared with longer fascicles (29). We recently observed that shorter fascicle length in soleus and gastrocnemius was associated with better mobility in older adults (45), further supporting the suggestion that shorter soleus fascicle length in older endurance runners may be an adaptive response to life-long exercise training.

Another finding of the present study is that long-term endurance running was not associated with greater strength or size of triceps surae muscles compared with untrained older controls. Plantar flexion strength and maximal tendon force in endurance-trained older adults was significantly lower compared with that in young adults. Moreover, the effect sizes for the difference in gastrocnemius thickness and cross-

sectional area were comparable to those between young and older controls, which were also statistically significant. Taken together, these results suggest that endurance running is not a sufficient stimulus for maintenance of muscle mass and size with aging.

In contrast, the present data suggest that high-intensity loading due to sprint training may be an effective stimulus to counteract the age-related decline in both muscle mass and strength in triceps surae muscles. We observed that gastrocnemius muscle cross-sectional area was significantly larger in sprint-trained older adults compared with untrained older controls. In addition, plantar flexion strength and maximal tendon force were not significantly different from those of young controls, with about one-half the effect size as in endurance-trained older adults compared with young controls. These findings are supported by previous studies in young adults in which sprint running but not endurance running was associated with greater muscle strength and size in triceps surae muscles (18, 23). It may be that the beneficial effects of sprint training preferentially target gastrocnemius muscle, which contains more fast-twitch muscle fibers than soleus (13).

Methodological considerations.

The strengths of the present study are that the world-class older athletes measured in the present study had a life-long physical activity background and had performed many decades of regular exercise training. In addition, both the trained and untrained older adults were over 70 yr old and thus can be assumed to be affected by primary biological aging.

Limitations of the present study include the cross-sectional study design, which does not allow conclusions about cause-effect relationships that a longitudinal study design may allow. Cross-sectional studies can be affected by selection bias. It is possible that subjects with favorable muscle-tendon properties for endurance or sprint running were more likely to participate in such activities. However, we did not observe differences between older trained and untrained subjects in genetically determined

variables such as Achilles tendon moment arm, forefoot length, or Achilles tendon length, all of which are related to running performance (3, 25, 26, 42). This suggests that selection bias caused by genetic predisposition toward favorable musculoskeletal properties for running did not considerably affect our data, although the possibility of selection bias cannot be completely excluded. Another limitation of the present study is the small sample size. However, it was not possible to obtain a larger sample of older athletes from the highest performance level.

Conclusions.

The present findings suggest that triceps surae muscle size, architecture, strength, and tendon stiffness are relatively unaffected by long-term running training in older adults. The reason for this finding may be that the triceps surae muscle group is highly loaded in daily activities, and thus training produces only a small relative overload to this muscle group. Considering the unparalleled physical performance of the older athletes in the present study, it appears that the measured triceps surae muscle-tendon properties are not the key determining factors in their physical performance. However, relatively high individual variation in these properties suggests that a well-functioning muscle-tendon unit may be achieved via different combinations of muscle and tendon properties. In addition, it is likely that, in the present study, there were differences between the groups in factors that were not measured but that affect physical performance. These include muscle fiber type, composition, molecular level modifications in contractile proteins, and neural activation (8, 21, 41). To further elucidate the importance of muscle architecture and tendon mechanical properties for physical performance, future studies should investigate how aging and physical loading affect muscle-tendon interaction during locomotion.

In conclusion, our data suggest that long-term physical loading induced by either endurance or sprint running does not have a significant effect on Achilles tendon stiffness in older adults. However, the loading patterns associated with sprint and endurance training in older age both appear to increase Achilles tendon cross-sectional area in an intensity-dependent manner. Furthermore, the present results

suggest that sprint running but not endurance running may mitigate age-related loss of muscle mass and strength in triceps surae muscles. On the other hand, endurance training in older age may alter muscle architecture in a way that is beneficial for movement economy.

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Disclosures

No conflicts of interest, financial or otherwise, are declared by the author(s).

Author contributions

Author contributions: L.S., N.J.C., S.S., and T.F. conception and design of research; L.S. performed experiments; L.S. and J.P. analyzed data; L.S. and M.T.K. interpreted results of experiments; L.S. prepared figures; L.S. drafted manuscript; L.S., N.J.C., J.P., M.T.K., S.S., and T.F. edited and revised manuscript; L.S., N.J.C., J.P., M.T.K., S.S., and T.F. approved final version of manuscript.

References

1. Abe T, Kumagai K, Brechue WF. Fascicle length of leg muscles is greater in sprinters than distance runners. *Med Sci Sports Exerc* 32: 1125–1129, 2000.
2. Arampatzis A, Karamanidis K, Morey-Klapsing G, De Monte G, Stafilidis S. Mechanical properties of the triceps surae tendon and aponeurosis in relation to intensity of sport activity. *J Biomech* 40: 1946 – 1952, 2007.
3. Baxter JR, Novack TA, Van Werkhoven H, Pennell DR, Piazza SJ. Ankle joint mechanics and foot proportions differ between human sprinters and non-sprinters. *Proc Biol Sci* 279: 2018 –2024, 2012.
4. Biewener AA, Roberts TJ. Muscle and tendon contributions to force, work, and elastic energy savings: a comparative perspective. *Exerc Sport Sci Rev* 28: 99 –107, 2000.
5. Bohm S, Mersmann F, Arampatzis A. Human tendon adaptation in response to mechanical loading: a systematic review and meta-analysis of exercise intervention studies on healthy adults. *Sport Med-Open* 1: 7, 2015.
6. Couppé C, Hansen P, Kongsgaard M, Kovanen V, Suetta C, Aagaard P, Kjaer M, Magnusson SP. Mechanical properties and collagen crosslinking of the patellar tendon in old and young men. *J Appl Physiol* 107: 880 –886, 2009.
7. Couppé C, Svensson RB, Grosset JF, Kovanen V, Nielsen RH, Olsen MR, Larsen JO, Praet SFE, Skovgaard D, Hansen M, Aagaard P, Kjaer M, Magnusson SP. Life-long endurance running is associated with reduced glycation and mechanical stress in connective tissue. *Age (Dordr)* 36: 9665, 2014.
8. D'Antona G, Pellegrino MA, Carlizzi CN, Bottinelli R. Deterioration of contractile properties of muscle fibres in elderly subjects is modulated by the level of physical activity. *Eur J Appl Physiol* 100: 603–611, 2007.

9. Delmonico MJ, Harris TB, Visser M, Park SW, Conroy MB, Velasquez-Mieyer P, Boudreau R, Manini TM, Nevitt M, Newman AB, Goodpaster BH; Health, Aging, and Body. Longitudinal study of muscle strength, quality, and adipose tissue infiltration. *Am J Clin Nutr* 90: 1579–1585, 2009.
10. Dressler MR, Butler DL, Wenstrup R, Awad HA, Smith F, Boivin GP. A potential mechanism for age-related declines in patellar tendon biomechanics. *J Orthop Res* 20: 1315–1322, 2002.
11. Dudley-Javoroski S, McMullen T, Borgwardt MR, Peranich LM, Shields RK. Reliability and responsiveness of musculoskeletal ultrasound in subjects with and without spinal cord injury. *Ultrasound Med Biol* 36: 1594–1607, 2010.
12. Durlak JA. How to select, calculate, and interpret effect sizes. *J Pediatr Psychol* 34: 917–928, 2009.
13. Edgerton VR, Smith JL, Simpson DR. Muscle fibre type populations of human leg muscles. *Histochem J* 7: 259–266, 1975.
14. Finlayson R, Woods SJ. Lipid in the Achilles tendon. A comparative study. *Atherosclerosis* 21: 371–389, 1975.
15. Franchi M, Torricelli P, Giavaresi G, Fini M. Role of moderate exercising on Achilles tendon collagen crimping patterns and proteoglycans. *Connect Tissue Res* 54: 267–274, 2013.
16. Frontera WR, Hughes VA, Lutz KJ, Evans WJ. A cross-sectional study of muscle strength and mass in 45- to 78-yr-old men and women. *J Appl Physiol* 71: 644–650, 1991.
17. Goodpaster B, Park S, Harris T, Kritchevsky S, Nevitt M, Schwartz A, Simonsick E, Tylavsky F, Visser M, Newman A. The loss of skeletal muscle strength, mass, and quality in older adults: the health, aging and body composition study. *J Gerontol A Biol Sci Med Sci* 61: 1059–1064, 2006.
18. Hansen P, Aagaard P, Kjaer M, Larsson B, Magnusson SP. Effect of habitual running on human Achilles tendon load-deformation properties and cross-sectional area. *J Appl Physiol* 95: 2375–2380, 2003.
19. Karamanidis K, Arampatzis A. Mechanical and morphological properties of human quadriceps femoris and triceps surae muscle-tendon unit in relation to aging and running. *J Biomech* 39: 406–417, 2006.

20. Kongsgaard M, Aagaard P, Kjaer M, Magnusson SP. Structural Achilles tendon properties in athletes subjected to different exercise modes and in Achilles tendon rupture patients. *J Appl Physiol* 99: 1965–1971, 2005.
21. Korhonen MT, Cristea A, Alén M, Häkkinen K, Sipilä S, Mero A, Viitasalo JT, Larsson L, Suominen H. Aging, muscle fiber type, and contractile function in sprint-trained athletes. *J Appl Physiol* 101: 906 – 917, 2006.
22. Korhonen MT, Heinonen A, Siekkinen J, Isolehto J, Alén M, Kiviranta I, Suominen H. Bone density, structure and strength, and their determinants in aging sprint athletes. *Med Sci Sports Exerc* 44: 2340 – 2349, 2012.
23. Kubo K, Ikebukuro T, Yata H, Tomita M, Okada M. Morphological and mechanical properties of muscle and tendon in highly trained sprinters. *J Appl Biomech* 27: 336 –344, 2011.
24. Kulmala JP, Korhonen MT, Kuitunen S, Suominen H, Heinonen A, Mikkola A, Avela J. Which muscles compromise human locomotor performance with age? *J R Soc Interface* 11: 20140858, 2014.
25. Kunimasa Y, Sano K, Oda T, Nicol C, Komi PV, Locatelli E, Ito A, Ishikawa M. Specific muscle-tendon architecture in elite Kenyan distance runners. *Scand J Med Sci Sport* 24: 1–6, 2014.
26. Lee SS, Piazza SJ. Built for speed: musculoskeletal structure and sprinting ability. *J Exp Biol* 212: 3700 – 3707, 2009.
27. Lichtwark GA, Wilson AM. In vivo mechanical properties of the human Achilles tendon during one-legged hopping. *J Exp Biol* 208: 4715–4725, 2005.
28. Lieber RL, Friden J. Clinical significance of skeletal muscle architecture. *Clin Orthop Relat Res* 383: 140 –151, 2001.
29. Mademli L, Arampatzis A. Mechanical and morphological properties of the triceps surae muscle-tendon unit in old and young adults and their interaction with a submaximal fatiguing contraction. *J Electromyogr Kinesiol* 18: 89 –98, 2008.
30. Maganaris CN. Tendon conditioning: artefact or property? *Proc R Soc B Biol Sci* 270, Suppl: S39 –S42, 2003.

31. Magnusson SP, Beyer N, Abrahamsen H, Aagaard P, Neergaard K, Kjaer M. Increased cross-sectional area and reduced tensile stress of the Achilles tendon in elderly compared with young women. *J Gerontol A Biol Sci Med Sci* 58: 123–127, 2003.
32. Magnusson SP, Hansen P, Aagaard P, Brond J, Dyhre-Poulsen P, Bojsen-Moller J, Kjaer M. Differential strain patterns of the human gastrocnemius aponeurosis and free tendon, in vivo. *Acta Physiol Scand* 177: 185–195, 2003.
33. Magnusson SP, Kjaer M. Region-specific differences in Achilles tendon cross-sectional area in runners and non-runners. *Eur J Appl Physiol* 90: 549–553, 2003.
34. McPhee JS, Hogrel JY, Maier AB, Seppet E, Seynnes OR, Sipila S, Bottinelli R, Barnouin Y, Bijlsma AY, Gapeyeva H, Maden-Wilkinson TM, Meskers CG, Paasuke M, Sillanpaa E, Stenroth L, ButlerBrowne G, Narici MV, Jones DA. Physiological and functional evaluation of healthy young and older men and women: design of the European MyoAge study. *Biogerontology* 14: 325–337, 2013.
35. Mian OS, Thom JM, Ardigò LP, Narici MV, Minetti a. E. Metabolic cost, mechanical work, and efficiency during walking in young and older men. *Acta Physiol* 186: 127–139, 2006.
36. Morse CI, Thom JM, Birch KM, Narici MV. Changes in triceps surae muscle architecture with sarcopenia. *Acta Physiol Scand* 183: 291–298, 2005.
37. Narici MV, Maganaris CN, Reeves ND, Capodaglio P. Effect of aging on human muscle architecture. *J Appl Physiol* 95: 2229–2234, 2003.
38. Peltonen J, Cronin NJ, Avela J, Finni T. In vivo mechanical response of human Achilles tendon to a single bout of hopping exercise. *J Exp Biol* 213: 1259–1265, 2010.
39. Rantanen T, Masaki K, Foley D, Izmirlian G, White L, Guralnik JM. Grip strength changes over 27 yr in Japanese-American men. *J Appl Physiol* 85: 2047–2053, 1998.
40. Rantanen T, Guralnik JM, Foley D, Masaki K, Leveille S, Curb JD, White L. Midlife hand grip strength as a predictor of old age disability. *JAMA* 281: 558–560, 1999.
41. Reid KF, Doros G, Clark DJ, Patten C, Carabello RJ, Cloutier GJ, Phillips EM, Krivickas LS, Frontera WR, Fielding RA. Muscle power failure in mobility-limited older adults: preserved single fiber function

- despite lower whole muscle size, quality and rate of neuromuscular activation. *Eur J Appl Physiol* 112: 2289–2301, 2012.
42. Scholz MN, Bobbert MF, van Soest AJ, Clark JR, van Heerden J. Running biomechanics: shorter heels, better economy. *J Exp Biol* 211: 3266–3271, 2008.
43. Sipilä S, Suominen H. Quantitative ultrasonography of muscle: detection of adaptations to training in elderly women. *Arch Phys Med Rehabil* 77: 1173–1178, 1996.
44. Stenroth L, Peltonen J, Cronin NJ, Sipilä S, Finni T. Age-related differences in Achilles tendon properties and triceps surae muscle architecture in vivo. *J Appl Physiol* 113: 1537–1544, 2012.
45. Stenroth L, Sillanpää E, McPhee JS, Narici MV, Gapeyeva H, Pääsuke M, Barnouin Y, Hogrel JY, Butler-Browne G, Bijlsma A, Meskers CG, Maier AB, Finni T, Sipilä S. Plantarflexor muscle-tendon properties are associated with mobility in healthy older adults. *J Geront A Biol Sci Med Sci* 70: 996–1002, 2015.
46. Tanaka H, Seals DR. Endurance exercise performance in Masters athletes: age-associated changes and underlying physiological mechanisms. *J Physiol* 586: 55–63, 2008.
47. Thorpe CT, Udeze CP, Birch HL, Clegg PD, Screen HR. Capacity for sliding between tendon fascicles decreases with ageing in injury prone equine tendons: a possible mechanism for age-related tendinopathy? *Eur Cells Mater* 25: 48–60, 2012.
48. Wood LK, Arruda EM, Brooks SV. Regional stiffening with aging in tibialis anterior tendons of mice occurs independent of changes in collagen fibril morphology. *J Appl Physiol* 111: 999–1006, 2011.
49. Yataco AR, Busby-Whitehead J, Drinkwater DT, Katzel LI. Relationship of body composition and cardiovascular fitness to lipoprotein lipid profiles in master athletes and sedentary men. *Aging (Milano)* 9: 88–94, 1997.
50. Ying M, Yeung E, Li B, Li W, Lui M, Tsoi CW. Sonographic evaluation of the size of Achilles tendon: the effect of exercise and dominance of the ankle. *Ultrasound Med Biol* 29: 637–642, 2003.
51. Zajac FE. Muscle and tendon: properties, models, scaling, and application to biomechanics and motor control. *Crit Rev Biomed Eng* 17: 359–411, 1989.

52. Zampieri S, Pietrangelo L, Loeffler S, Fruhmahn H, Vogelauer M, Burggraf S, Pond A, Grim-Stieger M, Cvecka J, Sedliak M, Tirpakova V, Mayr W, Sarabon N, Rossini K, Barberi L, De Rossi M, Romanello V, Boncompagni S, Musaro A, Sandri M, Protasi F, Carraro U, Kern H, Tirpáková V, Mayr W, Sarabon N, Rossini K, Barberi L, De Rossi M, Romanello V, Boncompagni S, Musarò A, Sandri M, Protasi F, Carraro U, Kern H. Lifelong physical exercise delays age-associated skeletal muscle decline. *J Gerontol A Biol Sci Med Sci* 70: 163–173, 2015.