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1 **Manuscript**

2 **1. Introduction**

3 Anterior cruciate ligament (ACL) injury is a common and potentially traumatic sports related injury, presenting with substantial short- and long-term morbidities (Griffin et al., 2006). ACL tears tend to occur during activities including sudden acceleration and deceleration, rapid changes of directions, jumping and landing tasks; where rapid and unanticipated movement responses of the ACL and the medial and lateral hamstring muscles (act as synergistic to the ACL) are necessary to stabilize the knee joint and successfully counteract the extreme load forces generated (McLean et al., 2008; Smith et al., 2012).

4 It has therefore been postulated that the hamstrings’ reaction time is one of the most important primary risk factor associated with ACL tears (Hughes and Watkins, 2006). Specially, longer hamstrings’ reaction times may negatively influence the muscle’s ability to quickly stabilize the knee against the large external loads generated during sporting tasks and subsequently might increase the risk of tear (Besier et al., 2003; Blackburn et al., 2009; McLean et al., 2010). This reaction time is comprised of two critical phases: the pre-motor time and motor time (Botwinick and Thompson, 1966). The pre-motor time, defined as the time between the presentation of a stimulus and the first detectable muscle activity (Weiss, 1965), incorporating perception, decision making and information processing and transfer. The motor time is also called electromechanical delay and is defined as the time between the onset of muscle activity and the onset of force generation by that muscle’s contraction (Zhou et al., 1995). It is related to the rate of muscle force production and is also considered an indirect measure of muscle-tendon unit stiffness (Blackburn et al., 2009).

5 Consequently, some authors have stated that ACL injury screening and prevention efforts may ultimate benefit form the inclusion of hamstrings reaction times assessments (Hewett et al., 2005, 2006; McLean et al., 2010; Ristanis et al., 2009). However, before the hamstrings total
reaction time, pre-motor time and motor time can be used for legitimate research and to establish progress from training and/or rehabilitation practices, the inter-session reliability of these measurements must be determined. Surprisingly, when the body of literature is carefully scrutinised, it is shown that no studies (to the authors’ knowledge) have addressed the examination of their inter-session reliability of the hamstrings’ total reaction time, pre-motor time and motor time.

The incidence of non-contact ACL injury in women has been reported to be 6-8 times greater than in men competing in the same sports (Griffin et al., 2006). Apart from the obvious anatomical and hormonal differences between men and women, it is possible that sex specific hamstrings’ reaction times profile may play a role in the higher incidence of ACL injuries in women. In some studies (Bell and Jacobs, 1986; Blackburn et al., 2004; Granata et al., 2002; Winter and Brookes, 1991; Zhou et al., 1995), although not all (Blackburn et al., 2009; Moore et al., 2002), the motor time (measured under isometric and concentric muscle actions) has been found to be longer in women than men. However, among the aforementioned studies, only Blackburn et al. (2009) reported data for the hamstrings during isometric muscle actions and they showed that the motor time scores did not differ significantly across sex. In addition, to the author’s knowledge, no studies have examined sex-related differences in hamstrings total reaction time and pre-motor time. This knowledge would provide insight into the understanding of the factor associated with the sex-related differences in the ratio of ACL injuries.

Therefore, the aims of this investigation were twofold: (a) to ascertain the inter-session reliability of hamstrings total reaction time, pre-motor time and motor time; and (b) to examine sex-related differences in the hamstrings reaction times profile in recreational athletes.

2. Methods

2.1 Participants
Twenty-four men (age = 20.7 ±2.8 y; stature = 174.3 ±7.9 cm; body mass = 74.2 ±9.7 kg) and 24 women (age = 20.1 ±2.1 y; stature = 162.9 ±7.9 cm; body mass = 61.1 ±6.7 kg) who were recreationally active adults (engaging in 2-5 hours of moderate physical activity 3-5 days per week) completed this study. Although all participants reported engaging in recreational sports performed at the intramural or competitive university level, none of them were involved in a systematic and specific strength-training programme. Participants were instructed to avoid their regular training throughout the experimental period and refrain from vigorous physical activity 48 hours before each testing day.

Other exclusion criteria were: (a) histories of orthopaedic problems, such as episodes of hamstrings injury, fractures, surgery or pain in the knee or hamstring muscles over the past six months; (b) missing one testing session during the data collection phase; and (c) presence of delayed onset muscle soreness at any testing session to avoid the effects of muscle soreness on muscle lengthening and force production. The women were not in the ovulation phase (self-reported, days 10-14) of their menstrual cycle during testing as fluctuating concentrations of oestrogen throughout the menstrual cycle affect musculotendinous stiffness (Bell et al., 2009; Eiling et al., 2007) and joint laxity (Romani et al. 2003). The participants were verbally informed about the study procedures before testing and provided written informed consent. This study was approved by the University of Gloucestershire Research Ethics Committee (United Kingdom).

2.2 Research design

A repeated measures design was carried out to determine the inter-session reliability of hamstrings total reaction time, pre-motor time and motor time. A week before the testing sessions commenced, the participants were familiarized with the testing procedure by performing several sub-maximal and maximal isokinetic eccentric knee flexion movements.
simulating the testing conditions that were carried out during the experimental sessions. In addition, in order to ascertain the players’ dominant limb, during this familiarization session all the participants were required to undertake three tests: 1) jumping on one leg; 2) kicking a ball; and 3) climbing onto a stool with one leg according to the methodology described by Wang et al. (1993). The limb used to do at least 2 of the 3 tests was considered the dominant one.

After the familiarization protocol was completed, each participant undertook the testing procedure on three different occasions, with a 72-96 hours rest interval between testing sessions. The choice of a 72-96 hours interval period between testing sessions in our study is based on the fact that a minimum of 36-48 hours rest interval appears to be necessary to restore the optimal muscle function after a light bout of strength training (Bompa, 2000). Therefore, we used a 72-96 hours interval period between testing sessions to ensure no carry over effects between testing sessions.

An experienced clinician carried out each of the three testing sessions at the same time of the day under the same environmental conditions (room temperature at 25 ºC) to avoid inter-tester variability and to reduce the influence of individual circadian rhythm on test data. The clinician was blinded to the purpose of the study and test results from previous testing sessions.

Before hamstrings total reaction time, pre-motor time and motor time testing was carried out, participants warmed-up by performing 5 minutes of general warm-up (cycle at 50 W and 60–70 rpm), 4 sub-maximal (self-perceived 50% effort) and 2 maximal eccentric knee flexion actions to reduce the variability and standard error of measurements by minimizing the effect of different body temperature on muscle strength performance (Bishop, 2003). There was a 2-minute rest between the warm-up and the hamstrings total reaction time, pre-motor time and motor time testing.

2.3 Testing procedure
The assessments of the hamstrings total reaction time, pre-motor time and motor time of the dominant limb were performed using a Biodex System-3 isokinetic dynamometer (Biodex Corp., Shirley, NY, USA) and a wireless 8-channel Delsys electromyography telemetry system (Delsys Myomonitor III, Delsys Inc., Boston, MA, USA). The dynamometer and EMG data were interfaced by feeding the analogue data directly from the dynamometer in to the Universal Input Unit via a trigger box and were displayed online on a computer using dedicated software (Delsys, Boston, MA). This system allowed for the dynamometer data to be converted to a digital signal in parallel with the EMG signal; consequently both data sets were collected in synchrony before processing by the EMG software (EMG Works 2, Delsys, Boston, MA). Therefore, this method allowed that the data from the EMG and dynamometer were completely time aligned making it possible to determine the onset of surface EMG activity in relation to the onset of torque production. Before and after the testing procedure commenced, the dynamometer and the EMG device were calibrated according to their respective manufacturer’s instructions to assure that no change occurred in the sensitivity.

2.4 Participant and dynamometer orientation

Participants were secured in a prone position on the dynamometer with the hip passively flexed at 10-20º and the head maintained erect. The prone position (10-20º hip flexion) was selected instead of a seated position (80-110º hip flexion) for two main reasons: (a) the prone position is more representative of the hip position during running/sprinting in contrast with a seated position; and (b) a prone position replicates the knee flexor and extensor muscle length-tension relationships which occurs in the late phase and the early contact phase of sprinting, and when landing or pivoting, which is when the ACL is loaded (Worrell et al., 1989, 1990). Although the standing position appears to be the most ecologic valid testing position, it was not used because of technical issues (the bench of the dynamometer could not adopt this position).
The axis of rotation of the dynamometer lever arm was aligned with the lateral epicondyle of the knee. The force pad was placed approximately 3 cm superior to the medial malleolus with the foot in a relaxed position. Adjustable strapping across the pelvis, posterior thigh proximal to the knee and foot localised the action of the musculature involved. The range of movement was set from $90^\circ$ knee flexion (initial position) to $0^\circ$ ($0^\circ$ was determined as maximal voluntary knee extension for each participant). All settings, including seat height, seat length, dynamometer height and lever arm length, were noted during the practice session so that they were identical throughout experimental trials.

### 2.5 Surface electromyography

Surface electromyography was obtained from medial and lateral hamstring muscles of the dominant limb represented by semitendinosus and biceps femoris using bipolar and preamplified electrodes with a fixed interelectrode spacing of 10 mm (DE-02, Delsys, Bagnoli-Boston, MA). The electrodes were attached parallel to the muscle fibers and over the dorsomedial muscle bulge at two thirds of the proximodistal thigh length for the semitendinosus, and at the dorsolateral side of the thigh at one half of the proximodistal thigh length for the biceps femoris (Merletti and Parker, 2004). The visually largest area of muscle belly was selected using a contraction against manual resistance. The ground electrode was placed on the lateral malleolus of the ankle. Each electrode placement was marked with semi-permanent ink during the familiarisation session and re-marked at the end of each testing session to ensure consistent placement on subsequent testing days. Electrodes and cables were secured with surgical tape to avoid movement artifacts. Before the placement of the electrodes, the hair of the area was shaved, and the skin was cleaned using alcohol swabs and abraded lightly with sandpaper to reduce impedance below $5 \, \text{k}\Omega$.

### 2.6 Data acquisition
Before the assessment of the hamstrings reaction time, pre-motor time and motor time, all participants performed a “zero offset” function to establish a zero baseline from each of the EMG channels during 10 s of stationary lying. The EMG and dynamometer data were acquired at a sampling rate of 1000 Hz. The dynamometer data were lowpass filtered at 10 Hz (4th order, zero phase lag, Butterworth), and the root-mean-square amplitude for each muscle activity was calculated as follows: the raw EMG signals were measured in a band of 20 to 450 Hz, full-wave rectified, high-pass filtered (4th order, zero phase lag, Butterworth) to remove movement artefacts with a cut-off frequency of 20 Hz, and smoothed with a 100-millisecond RMS algorithm.

After this baseline calculation process, participants were instructed to resist as hard and quickly as possible the knee extension movement generated by the arm of the dynamometer by eccentric action of the hamstrings throughout the full range of motion immediately after receipt of a simultaneous auditory (dynamometer) and visual (trigger box) signal. Both signals, which were given randomly within 1-4 s, and defined the beginning of data acquisition. Participants were also instructed to relax and not exert force on the level arm prior to the auditory and visual signals in order to avoid pre-action of the muscle.

Functional multi joint testing procedures seem to be more ecologically valid than a single joint isokinetic testing procedure, but due to the necessity of qualified technicians, longer and more practice sessions to accustom participants to the task required (learning effect) and highly sophisticated instruments, the use of these complex lab-based techniques may be limited in clinic and sports contexts. Therefore, in an attempt to be more realistic with the clinic and sports contexts, we decided using a isokinetic knee flexion testing procedure.

Six maximal voluntary eccentric knee flexion muscle actions were performed with 30 s rest between each contraction. After each eccentric muscle action, the clinician passively returned the tested limb to the initial position.
The biceps femoris and semitendinosus total reaction time, pre-motor time and motor time were calculated under eccentric muscle actions because it more appropriately simulates the pattern of movements that usually occur during the mechanisms of noncontact ACL injury (Hughes and Watkins, 2006). Six maximal eccentric knee flexion muscle actions were chosen because in a pilot study with 10 participants of similar age and training status, they subjectively indicated that 6 eccentric muscle actions were the maximum number of repetitions that they were able to undertake without feeling musculoskeletal fatigue and hence, bias the results. Therefore, to reduce the likelihood of fatigue throughout the testing procedure, the current study used 6 eccentric knee flexion muscle actions.

The speed of the isokinetic level arm throughout each repetition was preset at 240º/s so that the onset of torque was developed during the acceleration phase in order to replicate better the high speeds underlying in the mechanism of non-contact knee injury (Boden et al., 2000). The 240º/s angular velocity was chosen because in the pilot study, participants subjectively indicated that 240º/s was the maximum velocity that they were able to perform comfortably during the test. The reaction time was defined as the time interval from the application of the auditory and visual stimulus to the torque development (9.6 Nm torque) (Winter and Brookes, 1991). The pre-motor time was determined as the time between the initial auditory and visual stimulus and the associated muscle activation onset defined by the EMG activity (change from the EMG mean baseline level to ±15μV deviation) (Zhou et al., 1995). Visual inspection of the EMG signal was also used to be confident that there was no EMG activity prior to movement of the lever arm. The motor time was calculated as the time interval between the onset of EMG activity and torque development (time taken [milliseconds] to generate 9.6 Nm torque) (Zhou et al., 1995). The 2 trials with the highest and lowest total reaction time, pre-motor time and motor time values for each participant were discarded, and mean values for each neuromechanical variable were calculated across the remaining four trials. In addition, reliability studies have
reported better consistency of a measure when they used the mean value from several trials
(two or more) rather than the single highest or lowest value (Sole et al., 2007).

2.7 Statistical analysis

The distributions of raw data sets were checked using the Kolomogorov-Smirnov test and
demonstrated that all data had a normal distribution (p > 0.05). Descriptive statistics including
means and standard deviations were calculated for hamstrings total reaction time, pre-motor
time and motor time variables for both men and women separately. A paired t-test was
performed to compare hamstrings total reaction time, pre-motor time and motor time variables
(the average value among the three testing sessions) between men and women.

The inter-session reliability for each hamstrings reaction time measure was calculated to
average the reliability for the consecutive pairs of trials (2-1, 3-2) (Hopkins, 2000). In addition,
in line with current consensus regarding establishment of between day reproducibility in human
performance based studies (Atkinson and Nevill, 1998; Hopkins, 2000; Wier, 2005), the
following three aspects were explored:

1) Assessment of the bias between scores obtained in consecutive pairs of trials (2-1, 3-2).

Thus, 3 separate 3-way repeated measures analysis of variance (RMANOVAs; time [testing
session 1, 2 and 3] x muscle [biceps femoris and semitendinosus] x sex [men and women])
were used to identify the change in the mean (CM) (systematic bias), the 90% confidence
limits (CL) and the standard deviation of the difference between consecutive pairs of trial
for each variable (using Bonferroni post hoc test). Mauchly’s test was used to check the
sphericity of the data. The differences are reported as percent changes between pairs of
consecutive trials and their respective 90% CL using logarithmic values (Hopkins, 2000).
The 90% CL calculations also utilized t-distribution values corresponding to the appropriate
degrees of freedom in each sample.
2) The precision of measurement was determined. This was done using the typical percentage error (within-subjects variation in %) (Hopkins, 2000). The typical percentage error (as a coefficient of variation [CV_{TE}]) and its 90% CL was calculated using the log-transformed data via the following formula: 100 (e^s - 1), where s is the typical error (standard deviation of the difference between consecutive pairs of trial / \sqrt{2}). Logarithmic transformations of the data were performed and used to reduce the possible heteroscedasticity (when the difference scores demonstrate a trend toward larger values for participants at one end of the plot) of the raw data (Atkinson and Nevill, 1998). To interpret the CV_{TE} values, the current study used the arbitrary value suggested by Vincent (Vincent, 1994) with an analytical goal of ≈ 10% or below.

3) Assessment of the relative reproducibility. This was achieved using intraclass correlations (ICC) and was chosen for generalization purposes (Wier, 2005). ICCs for the sample were calculated from the analysis of variance via the formula: \( (F - 1) / (F + k - 1) \), where F is the F-ratio for the subject term and k (= 3) is the number of testing sessions. Magnitudes of correlations were assessed using the following scale of thresholds: <0.80 low, 0.80-0.90 moderate, and >0.90 high (Hopkins, 2000).

Statistical analyses were performed using the Statistical Package for Social Sciences (SPSS, v. 16.0 for Windows; SPSS Inc, Chicago) and Microsoft Excel 2003. The level of significance was set at \( \alpha = .05 \).

3. Results

Descriptive statistics (mean values for each testing session \([k = 3]\) ± standard deviation) for each variable are displayed in table 1 and table 2 for men and women respectively. Paired \( t \)-test analysis reported no significant differences between men and women for biceps femoris and semitendinosus total reaction time (\( p = 0.06 \)), pre-motor time (\( p = 0.18 \)) and motor time (\( p = 0.09 \)). Mauchly’s test of sphericity was not significant (\( p > 0.05 \)) for all variables. The
RMANOVA analysis indicated no significant interaction effect among trials for each variable for both men (table 1) and women (table 2), demonstrating that no systematic bias were present. Men and women reliability statistics (CM, CV$_{TE}$ and ICC) for biceps femoris and semitendinosus total reaction time, pre-motor time and motor time values are also presented in table 1 and table 2 respectively. The CV$_{TE}$ for all variables ranged from 4.3% (women semitendinosus total reaction time) to 10.8% (women biceps femoris pre-motor time) with ICC scores higher than 0.65. The total reaction time demonstrated the lowest inter-session variability in both men (CV$_{TE} =$ 4.5%) and women (CV$_{TE} =$ 6.0%).

***Table 1 and table 2 near here***

4. Discussion

There is a growing body of literature that has proposed the use of preseason screening of the dynamic knee stabilizers reaction time (mainly from the hamstring muscles) to identify athletes at increased risk of incurring ACL injuries (Hewett et al., 2005, 2006; McLean et al. 2010) and to assess the impact of therapeutic interventions or the effects of physical training (Hewett et al., 1999). However, before these data can be used for clinical and training goals, values must be defined so as to provide guidance in deciding whether an observed change on reassessment is within the boundaries of assessment error or whether there has been a true change (Hopkins, 2000). Therefore, one of the purposes of the current study was to determine the inter-session reliability of hamstrings total reaction time, pre-motor time and motor time in recreational athletes.

In this regard, the first aspect of reproducibility explored was the assessment of systematic error, the presence of which has been implicated to potentially occur in total reaction time, pre-motor time and motor time testing to due to learning effects or insufficient recovery time (Hopkins, 2000). It is clearly evident from the results obtained in the current investigation that the utilized familiarization session was sufficient in eliminating possible systematic error. This
may be partly attributed the fact that the participants in the study were generally accustomed to
physical activity performance and because the testing procedure was simple enough that just a
familiarization session was necessary to successfully avoid learning effects.

Another aspect of reliability explored is the precision of measurements. The typical percentage
error (CV\textsubscript{TE}) and the 95% Limits of Agreement (95% LoA) are the most widely used reliability
statistics to determine the precision of a measurement or testing procedure. However, the
current study selected the CV\textsubscript{TE} as an indicator of precision of measurement instead the 95%
LoA because it has been argued that the 95% LoA values may be too severe for assessing true
change in participant status (Hopkins, 2000). Thus, the findings of the present study indicated
that in both men and women, biceps femoris and semitendinosus total reaction time, pre-motor
time and motor time measures have a good precision (using the standard thresholds of precision
previously suggested) when measured during eccentric muscle actions of the hamstrings (CV\textsubscript{TE}
\approx 6\%). Unfortunately, we are not able to compare the precision results for total reaction time,
pre-motor time and motor time obtained in the current research with other studies because to
our knowledge, no studies have examined the inter-session reliability of hamstrings total
reaction time, pre-motor time and motor time during either concentric or eccentric muscle
actions.

After calculation of the minimal amount of change necessary to reflect a real improvement
(typical percentage error), clinicians and practitioners should make a judgment on the
implication of the typical error on the real application of the measurement (Atkinson and Nevill,
1998; Hopkins, 2000). Admittedly, the clinical decision regarding the exact reference value is
challenging, especially since there are no clear guidelines for reference value establishment, as
well as the potential need to evaluate multiple factors (training status, sex, age) to reach a
knowledgeable decision. However, a possible way of arriving at an acceptable percentage of
error may be to decide whether the variability associated with a particular measurement is small
enough to allow the detection of the expected changes with training interventions. In this sense, Minshull et al. (2009) using a repeated measures design and a testing procedure similar to that reported in the current study, although using concentric muscle actions; observed that the participant’s biceps femoris and semitendinosus motor time was increased by 20% after performing a standardised fatigue task in contrast with the control condition. Consequently, it would be appear that the errors associated with biceps femoris (8%) and semitendinosus (9%) motor time may be narrow enough to detect the expected changes after acute interventions. However, it is unclear whether the precision of motor time is satisfactory to monitor changes with neuromuscular training because to our knowledge no studies have examined the effects of a long lasting training intervention on hamstring motor time. Furthermore, for the biceps femoris and semitendinosus total reaction time and pre-motor time, it is unclear whether the precision of measurements (5.5% and 5.6% respectively) is satisfactory, mainly because there is a lack of information regarding changes in performance as a result of interventions (acute, chronic and surgical).

The last aspect assessed concerns relative reproducibility, which was quantified using ICC. The results of the current study reported moderate relative reliability scores for all the variables assessed in both men and women (ICC ranged from 0.65 to 0.91).

The findings of the current study indicated that there were no significant differences between hamstrings reaction times values of men and women. These results are in agreement with the only other study (to the author’s knowledge) that has compared hamstring motor time (measured during isometric contractions) between men and women (Blackburn et al., 2009). However, it should be highlighted that, although not significant, women reported consistently longer total reaction time (22.7 ms and 24.2 ms for biceps femoris and semitendinosus), pre-motor time (10.4 ms and 15.1 ms for biceps femoris and semitendinosus) and motor time (8.9 ms and 6.1 ms biceps femoris and semitendinosus) than men. Furthermore, considering that
injury occurs within a very narrow time frame (e.g., 73 milliseconds for medial collateral ligament injury [Pope et al., 1979]), the differences in neuromechanical function of the hamstrings that we found in our study, although small may be clinically significant and potentially large enough to play a role in ACL injury risk. Blackburn et al. (2009) have theoretically suggested that a delay in posterior tibial shear force provided by hamstring contraction may increase the risk of ACL injury by allowing a greater amount of anterior tibial translation to occur before the hamstrings are able to produce the critical level of force necessary to stabilize the joint. While the magnitude of the critical force required for stability differs based on the external demands placed on the system and the anthropometric characteristics of the individual (Blackburn et al. 2009), the data presented in the current study suggest that women may require a greater amount of time to reach a specified percentage of maximal force. However, future studies are necessary to determine whether this sex difference in hamstring reaction times has a real appreciable effect on dynamic joint stability and injury risk.

Interestingly, the results of this study did not found differences between biceps femoris and semitendinosus reaction times values in both men and women. A possible explanation for this result is that the biceps femoris works synergistically with the semitendinosus during knee flexion to provide functional balance to the knee. Direct comparison of our reported raw values to previous literature is not possible because, to the author’s knowledge, this is the first investigation which has evaluated the reaction times of the hamstrings during eccentric actions. One of the potential limitations of the current study is the population used. The age distribution of participants was relatively narrow and the generalizability to the broader population cannot be ascertained. Similarly, whether the tests would be as reliable in a population of injured participants must also be considered although pre-season screening is generally performed in healthy, uninjured populations. In addition, the current study explored the reliability of the
hamstrings total reaction time, pre-motor time and motor time during eccentric isokinetic knee flexion movements adopting a prone position because it may simulate better the mechanics of ACL injury. Whether the reliability of these parameters during concentric isokinetic knee flexion movements and/or in seated and/or standing position produces different reliability results was not explored. Since the EMG and dynamometer data were treated differently, different timing offsets might be present so future comparisons should be made with that in mind. Finally, the non-ovulation phase of the menstrual cycle in each participant was not verified with an ovulation test but was self reported. This may have potentially influenced our findings as the menstrual cycle is not always consistent between and within women (Bell et al., 2009).

It is recommended that physiotherapists undertaking pre-season screening of athletes consider the use of the test methodologies described here, as standardised testing protocols enable comparisons to be made across different clubs and sports. Future studies should examine possible strategies designed to increase the reliability of hamstrings total reaction time, pre-motor time and motor time such as different approaches to determine the onset of EMG activity and force production (2 times the baseline standard deviation, 2 times the baseline noise level) and with different devices (i.e. force plates and EMG). Furthermore, studies examining the reliability in different populations are needed to ascertain the clinical application of hamstrings total reaction time, pre-motor time and motor time.

5. Conclusions

The current study provides clinicians and practitioners with important information regarding the reliability threshold for the hamstrings total reaction time, pre-motor time and motor time and can serve as a guide for establishing whether an observer change between testing sessions is real or simply a product of typical error. Thus, an observer change larger than 5%, 9%, 8.0%, for total reaction time, pre-motor time and motor time respectively from baseline scores after
performing acute/chronic fatigue tasks or neuromuscular training would indicate that a real change was likely.

In addition, the results of this investigation indicate that, although not significant, women reported consistently longer hamstrings total reaction time (23.5 ms), pre-motor time (12.7 ms) and motor time (7.5 ms) values than men. These differences may play a role in the greater incidence of ACL injuries in women. However, future studies should address this issue.

6. References


25. Ristanis S, Tsepis E, Giotis D, Stergiou N, Cerulli G, Georgoulis AD. Electromechanical delay of the knee flexor muscles is impaired after harvesting hamstring tendons for anterior


Figure 1: A typical time plot of a single trial on the presentation of the stimulus (sound and visual signals) to the onset of the electromyography (EMG) signal (biceps femoris) and force generation (torque). The onset of torque development is defined as a 9.6 Nm deviation above the baseline level and the onset of EMG signal as ±15 μV deviation above the baseline.